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Hybrid cellular Potts modeling of cell-ECM interactions

Roeland Merks

and: Bente Hilde Bakker, Sonja Boas, Joao Carvalho, Josephine Daub, Babette de Jong, Martijn de Jong, Koen Keijzer, René van Oers, Margriet Palm, Lisanne Rens, Koen Schakenraad, Leonie van Steijn, Erika Tsingos, Tessa Vergroesen, Vincent Vermeulen, and experimental collaborators (and many others)

Mathematical Institute & Institute of Biology Leiden
Leiden University, The Netherlands

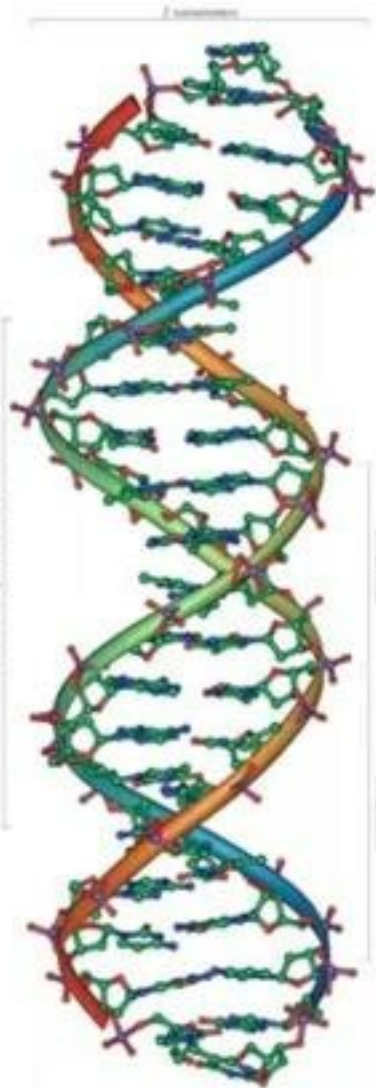
**Institute of Fundamental Technological
Research of the Polish Academy of Sciences**

March 27, 2023, online

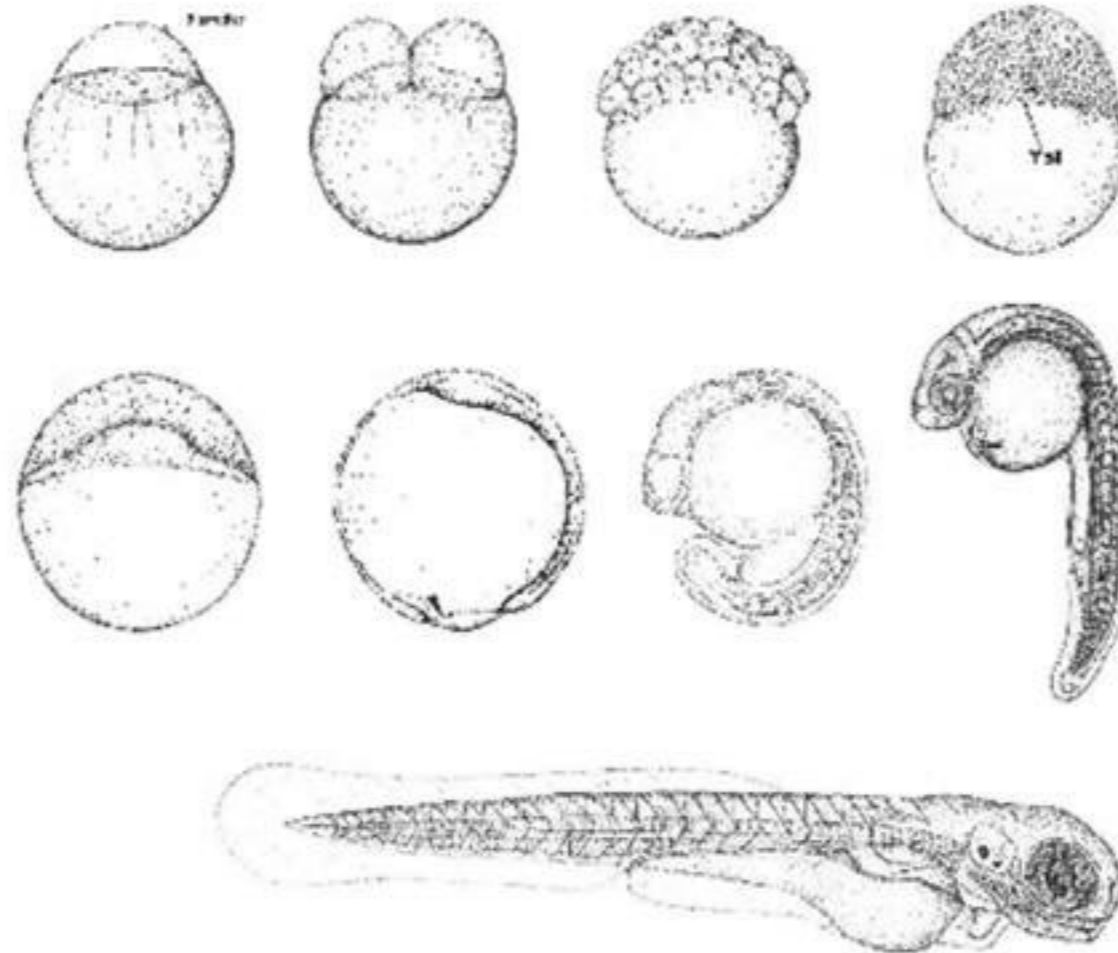
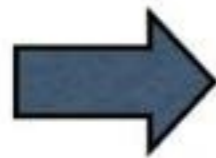


Morphogenesis

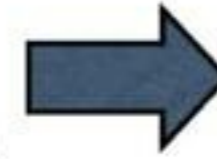
How is the **linear** information in the DNA translated into the **three-dimensional** shape of organisms?



DNA



Morphogenesis

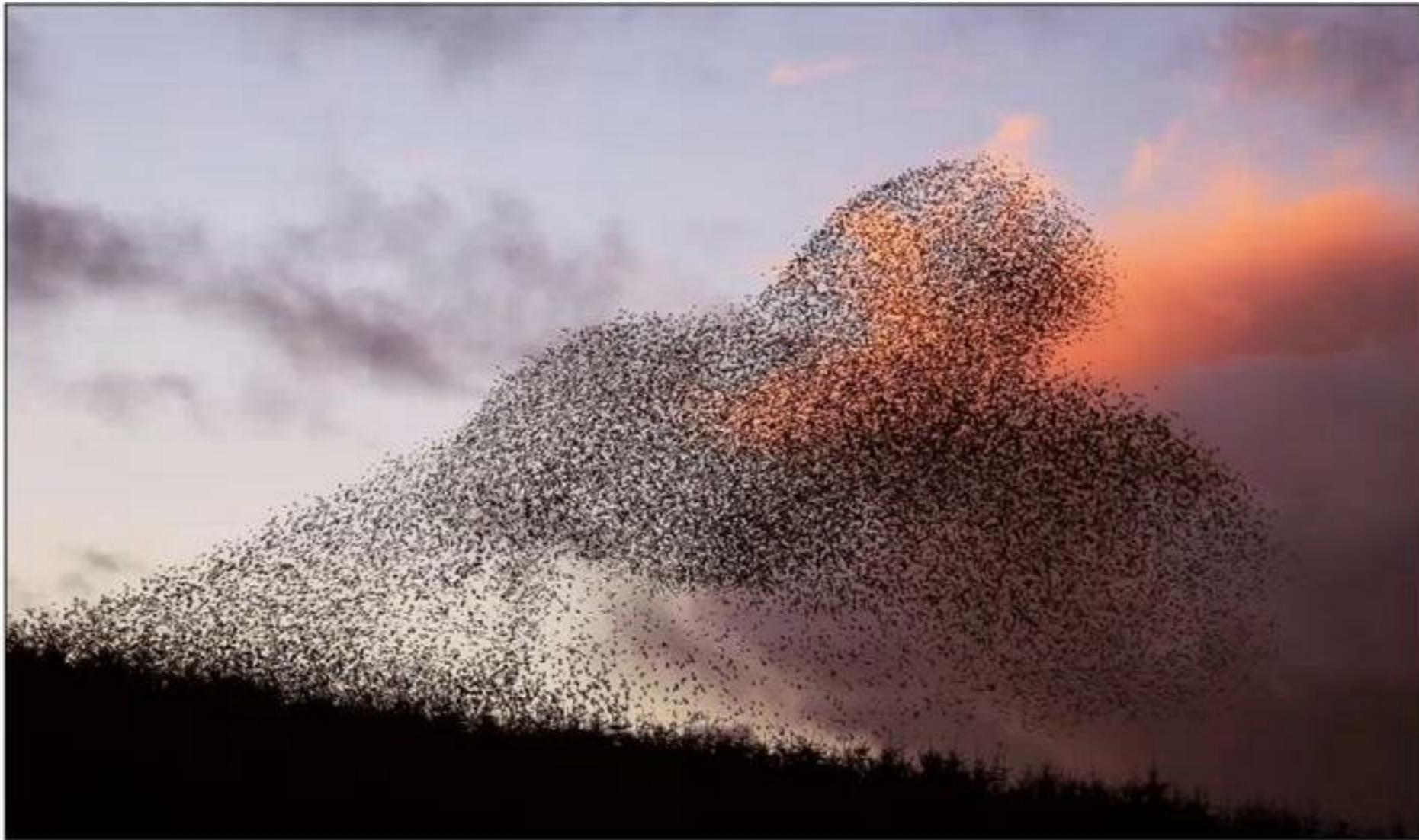


Adult



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Morphogenesis = Collective behavior



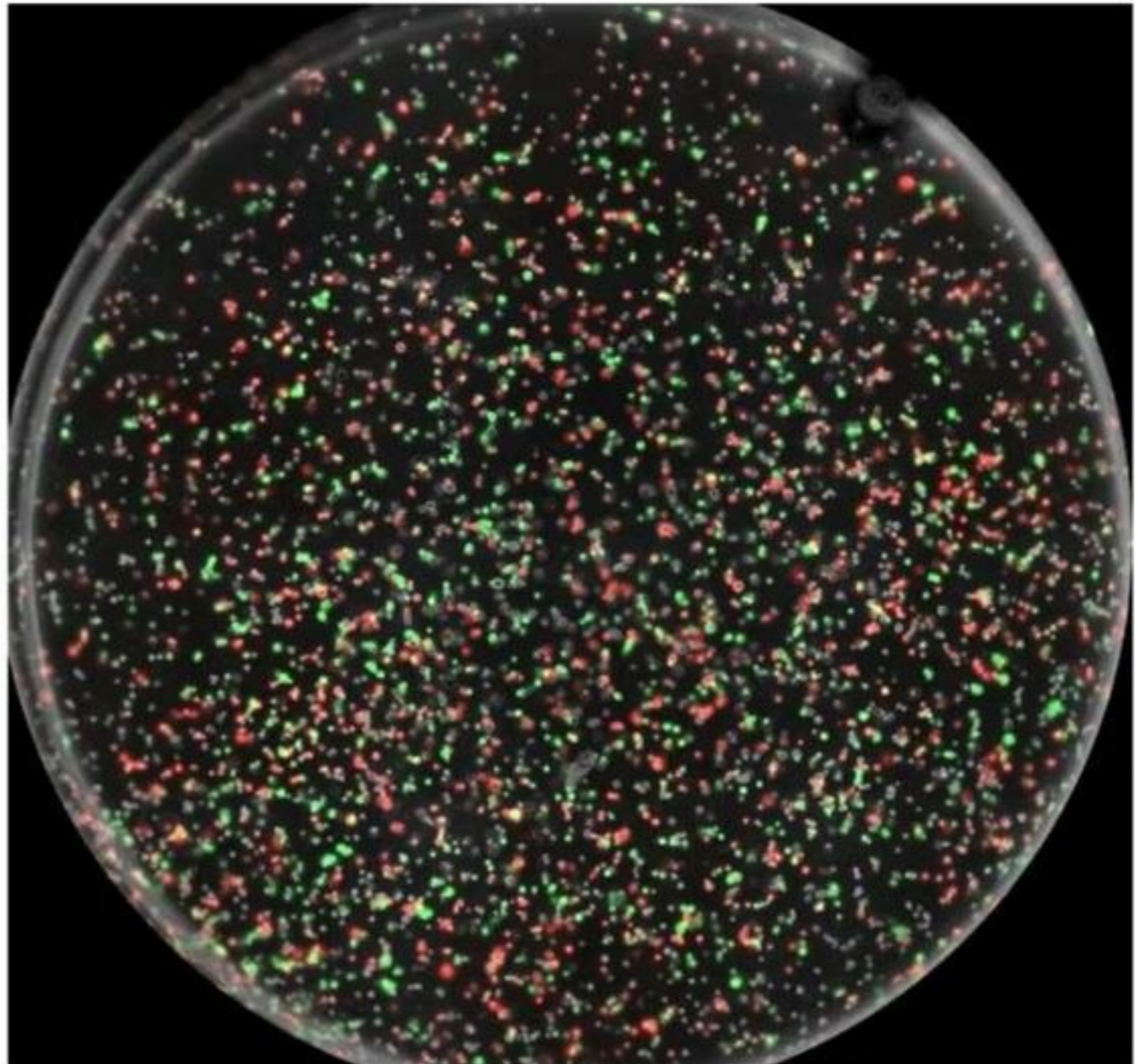
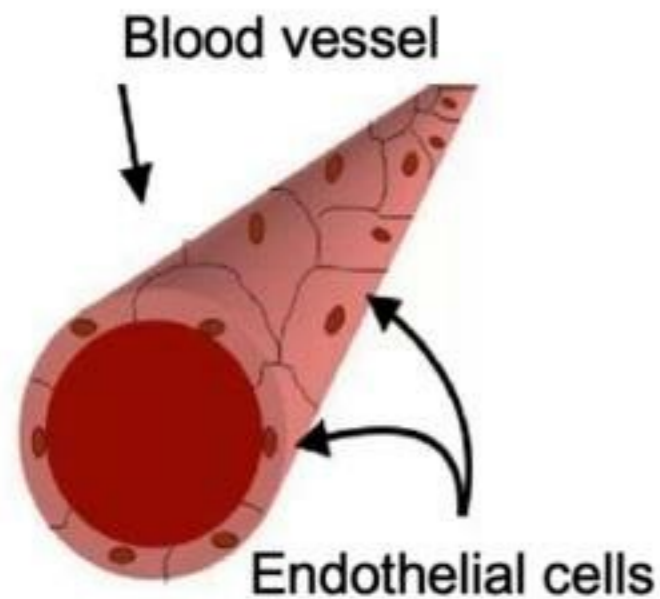
Multicellular organism: a 'flock' of cells

- Position in 'flock' may feed back on cell behaviour
- Study interaction of collective behavior and intracellular dynamics
- **Multiscale mathematical biology**



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Our favorite problem: Cell-ECM interactions driving angiogenesis

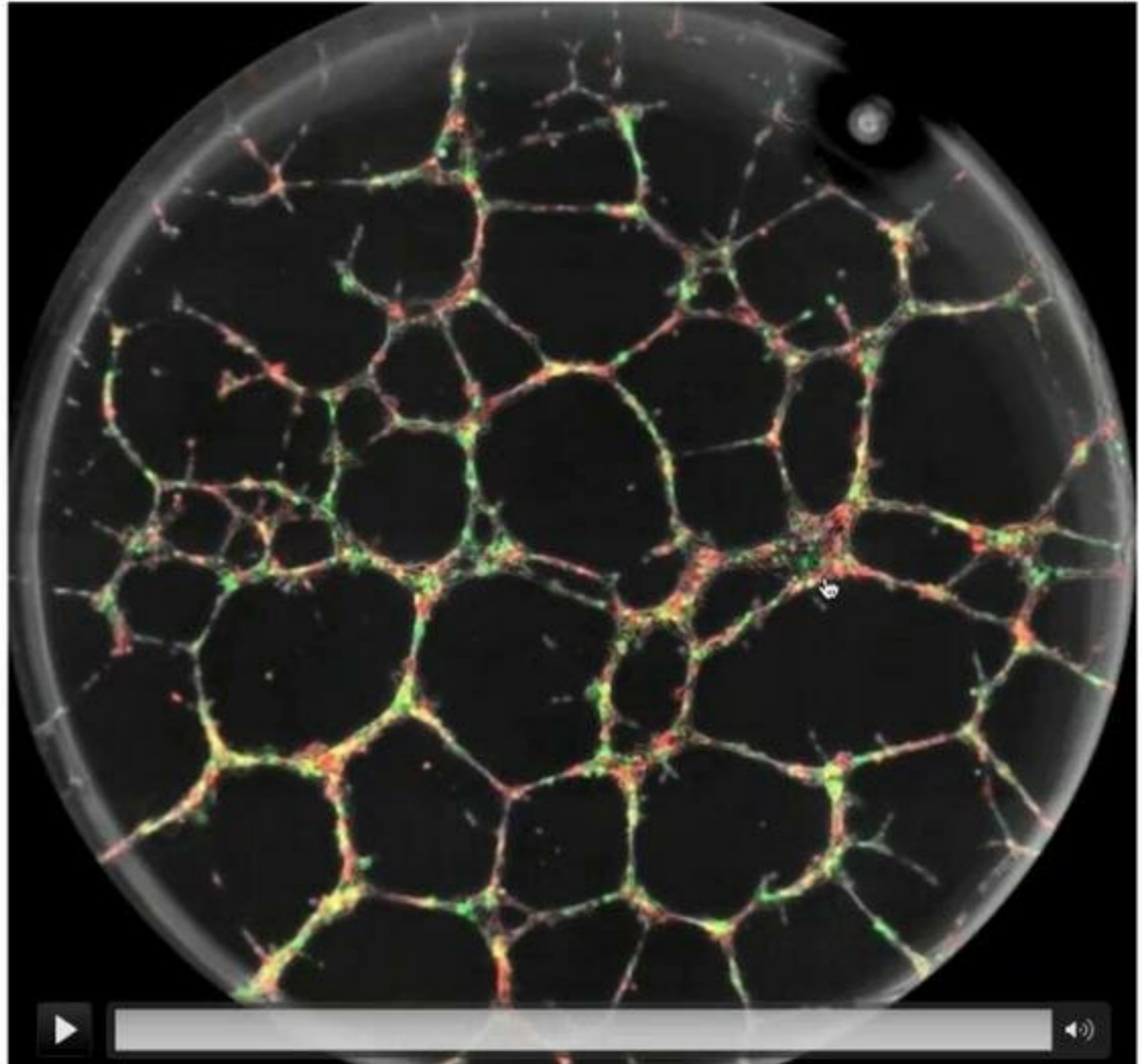
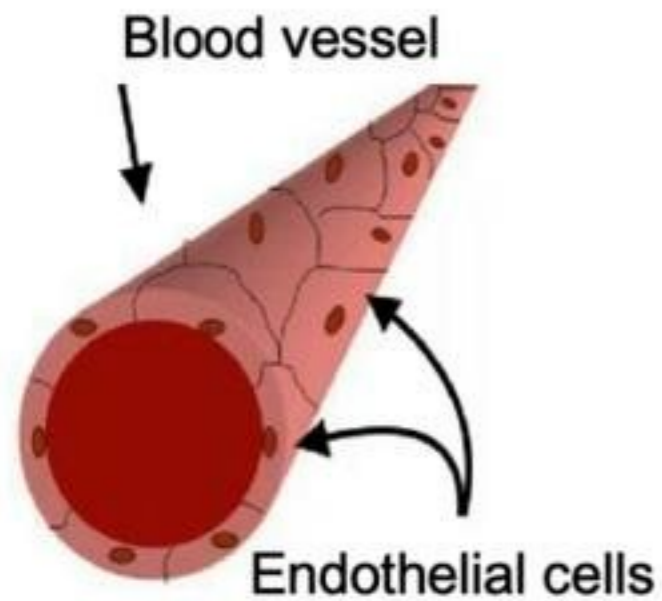


HMEC-1 in Matrigel; Tessa Vergroesen



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Our favorite problem: Cell-ECM interactions driving angiogenesis

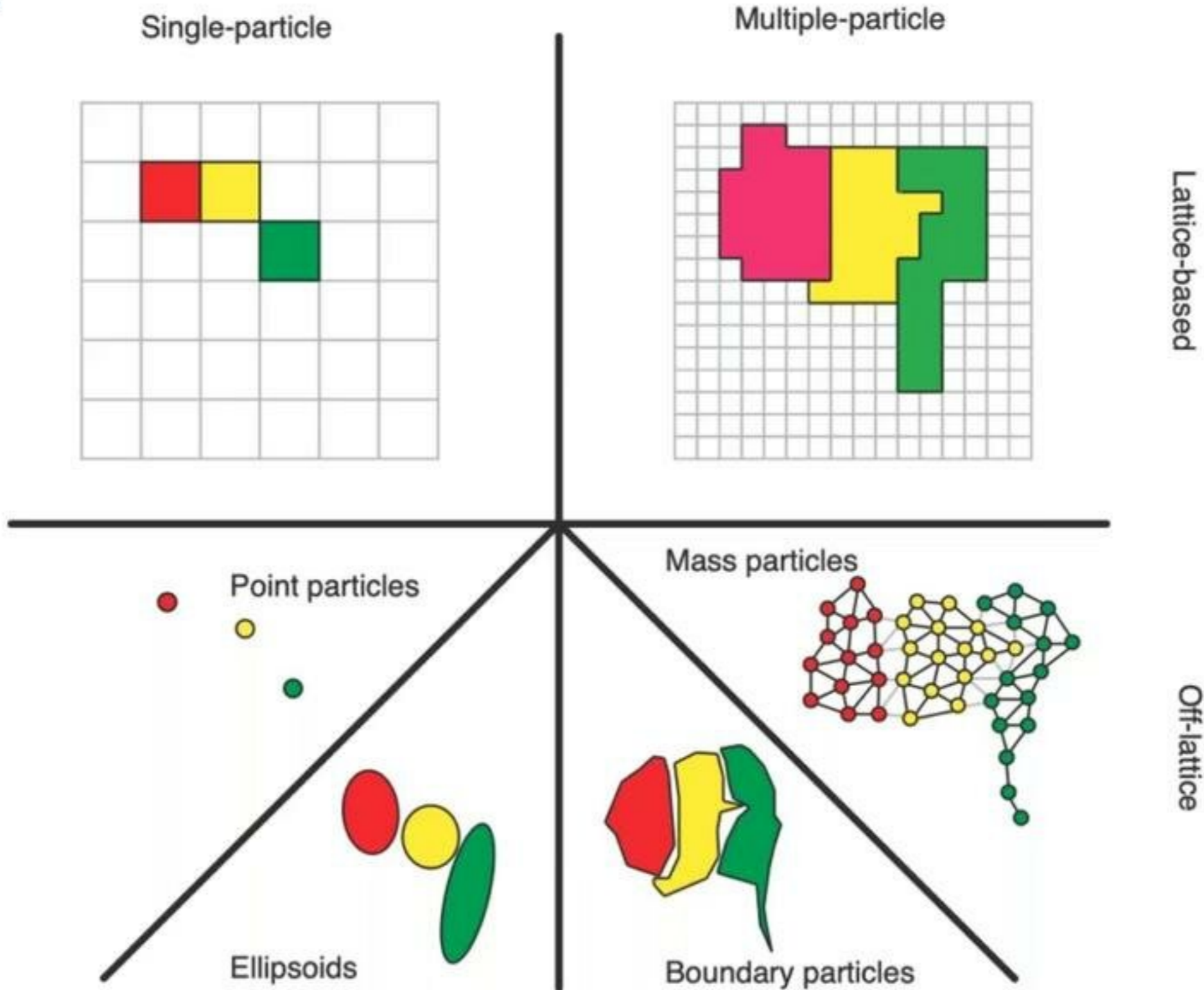


HMEC-1 in Matrigel; Tessa Vergroesen



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Cell-based models and the CPM



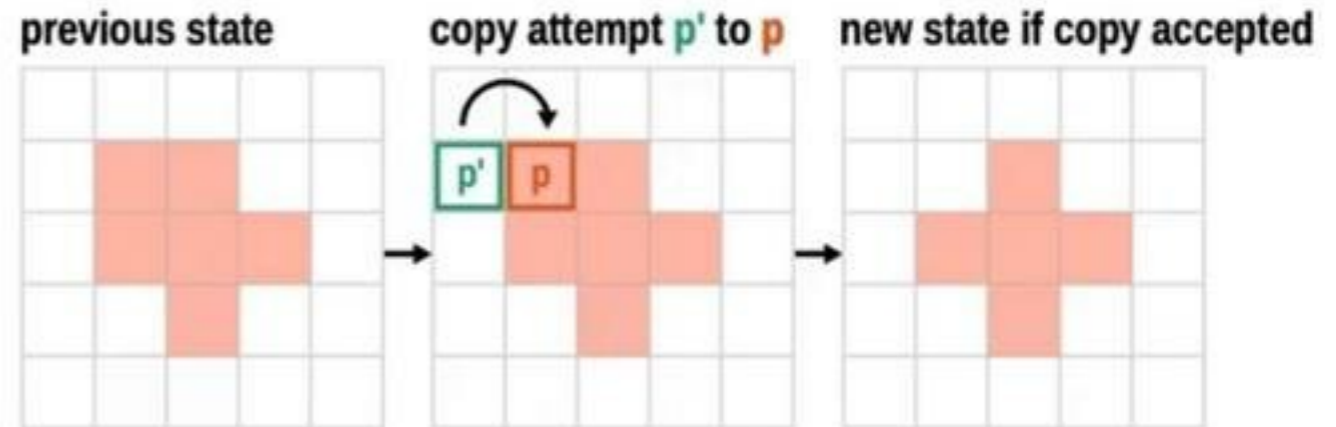


Cellular Potts Model (Graner & Glazier, 1992)



- Describes **random** cell motility
- Cells live on a grid
- One cell covers multiple grid points
- Cells move due to balance between active and reactive **cellular forces**:
 - **Reactive**: e.g, drag forces, adhesion to cells and matrix, strains in matrix based on Hamiltonian
 - **Active**: e.g., random extension/retraction of pseudopods, interaction with **external fields**
- Forces given by system energy, e.g.,:

$$H = \sum_{(\vec{x}, \vec{x}')} J(\sigma_{\vec{x}}, \sigma_{\vec{x}'}) \mathbb{1}_{\sigma_{\vec{x}} \neq \sigma_{\vec{x}'}} + \lambda_A \sum_{\sigma} (A_T(\sigma) - a(\sigma))^2$$



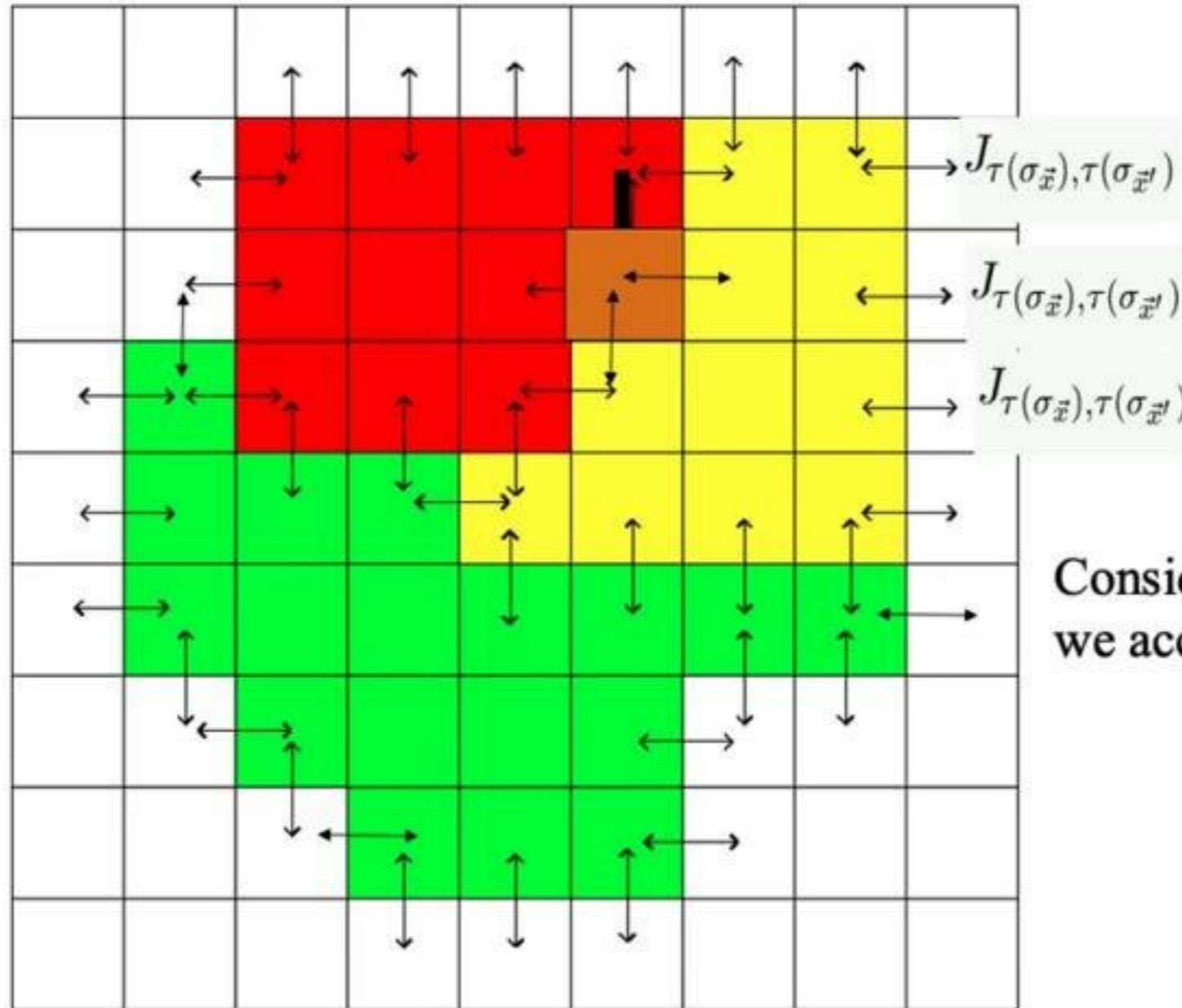
- Monitor energy change ΔH resulting from attempted copy
- Copy with probability:

$$P_{\text{copy}} = \begin{cases} 1 & \Delta H < 0 \\ \exp(-\Delta H/\mu) & \Delta H \geq 0 \end{cases}$$

μ “Cellular temperature”
Or: “Motility parameter”



Cellular Potts Model



Consider energy change ΔH if we accepted this copying

$$H = \sum_{(\vec{x}, \vec{x}')} J(\tau(\sigma_{\vec{x}}), \tau(\sigma_{\vec{x}'})) \mathbb{1}_{\sigma_{\vec{x}} \neq \sigma_{\vec{x}'}} + \lambda_A \sum_{\sigma} (A_T(\sigma) - a(\sigma))^2$$

Cell adhesion

Volume conservation

Plus additional constraints, e.g. cell shape constraint: $+\lambda_L (L_T - l(\sigma))^2$



Coupling with external fields

- Hybrid CPM-PDE model

- Example: cell secrete a growth factor that diffuses and is degraded.

$$\frac{\partial c(\vec{x}, t)}{\partial t} = \underbrace{D\nabla^2 c(\vec{x}, t)}_{\text{Diffusion}} - \underbrace{\varepsilon c(\vec{x}, t)}_{\text{Degradation}} + \underbrace{\mathbb{1}_{\sigma(\vec{x}) > 0} s}_{\text{Secretion by cells}}$$

- Chemotactic force along chemical gradients

$$\Delta H_{\text{work}} = -\chi_{\tau, i} (c_i(\vec{x}) - c_i(\vec{x}'))$$

Note, ΔH describes **work**:

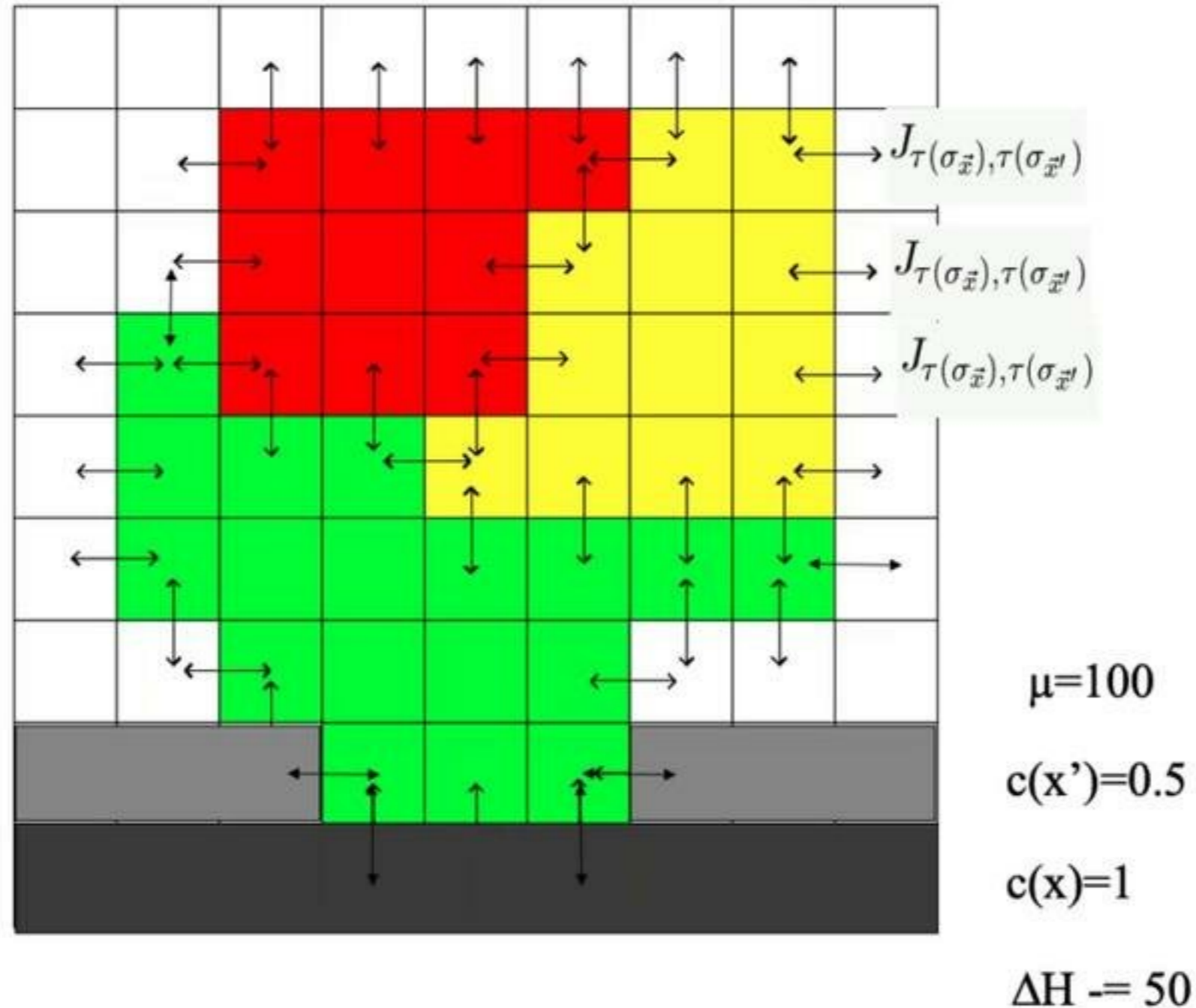
- Force over Distance = Work = Energy

$$P_{\text{copy}} = \begin{cases} 1 & \Delta H + H_{\text{work}} < 0 \\ \exp(-(\Delta H + H_{\text{work}})/\mu) & \Delta H + H_{\text{work}} \geq 0 \end{cases}$$



Coupling with extracellular fields

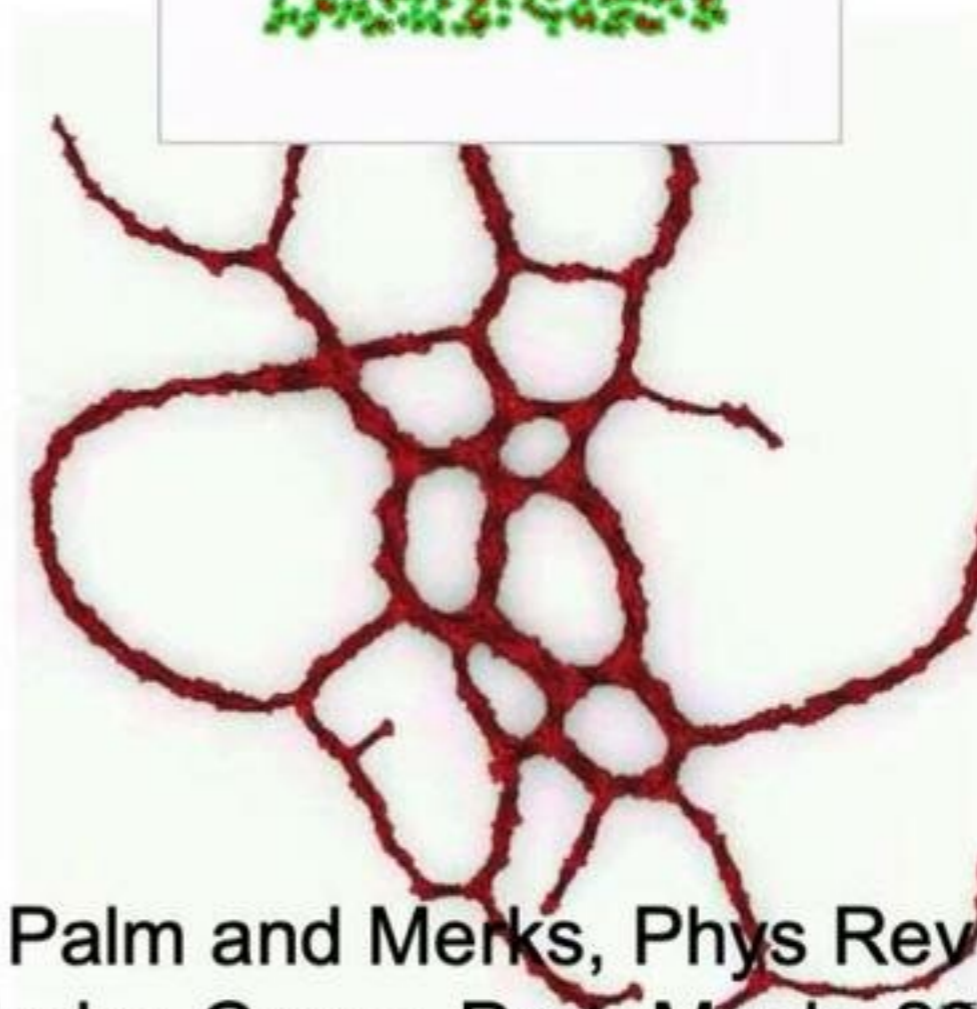
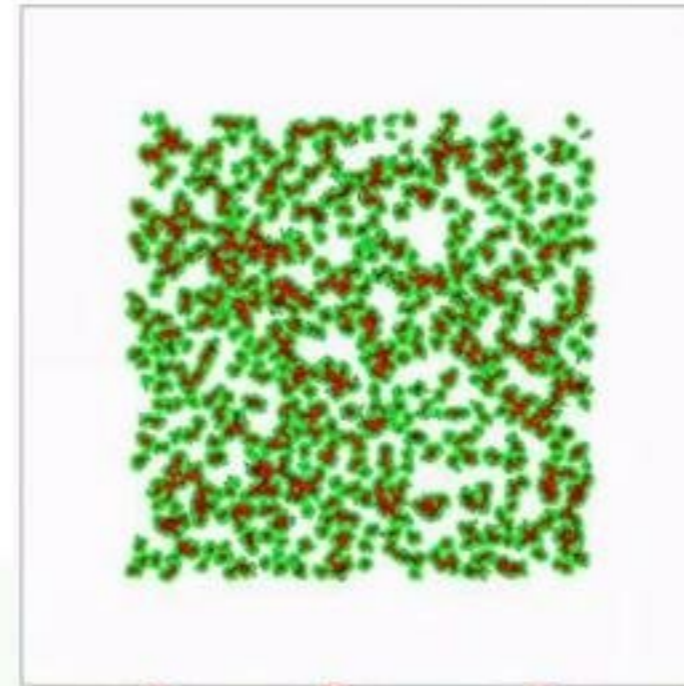
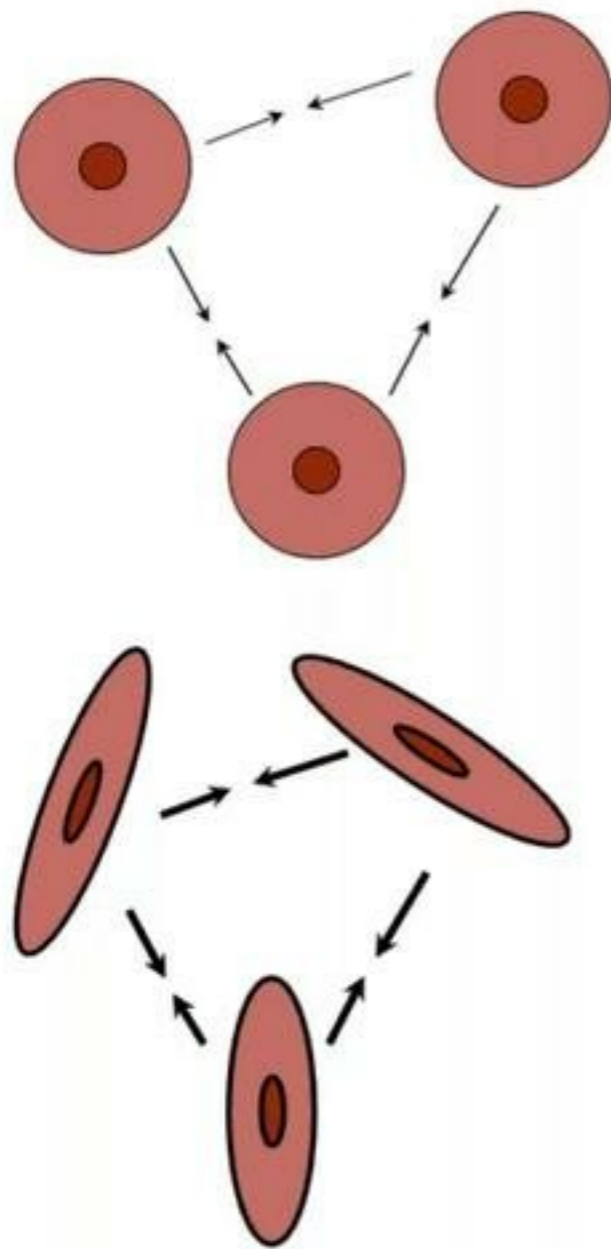
Pseudopods extend and retract more likely up chemical gradients





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Example: mutual attraction of elongated cells

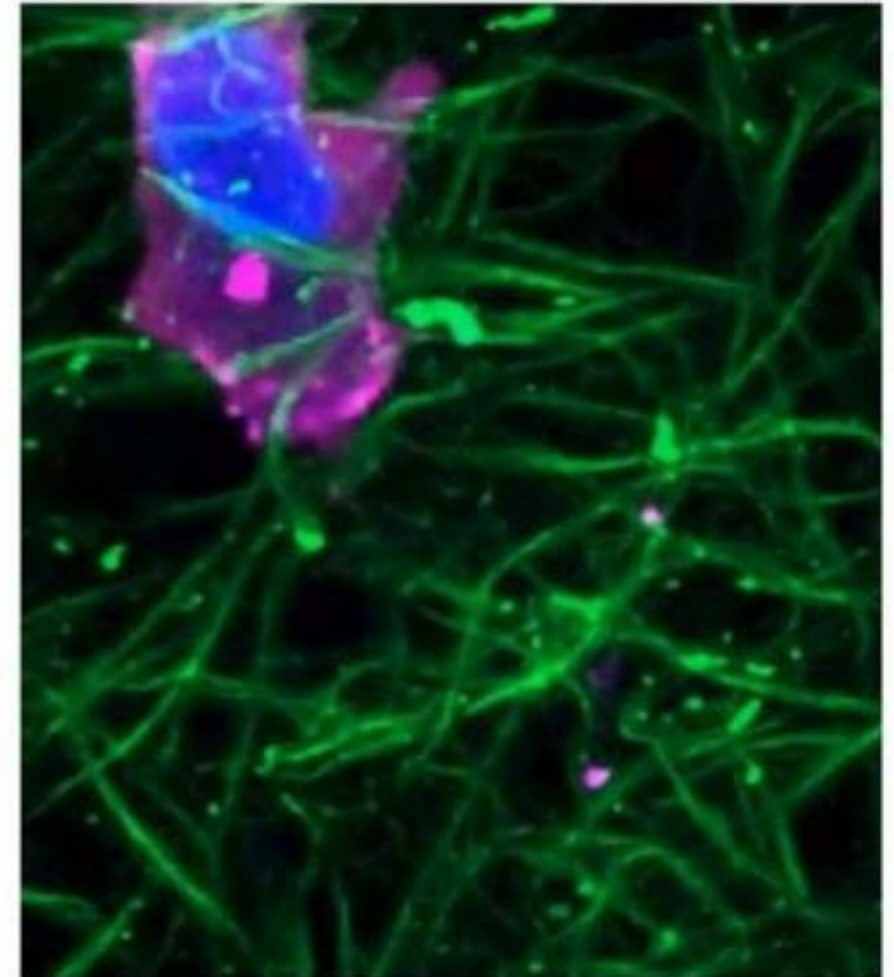


Merks et al. Dev Biol 2006; Palm and Merks, Phys Rev E 2013;
Palachanis, Szabó, Merks. Comp. Part. Mech. 2015



Extracellular matrix (ECM) in morphogenesis

- Extracellular matrix: network of materials that cells produce, for:
 - Mechanical support
 - Signaling
- Signals in ECM can be long-lived and long-distance
 - ECM binds chemical signals
 - Cells respond to strains in ECM
- Thus: ECM is key to tissue morphogenesis

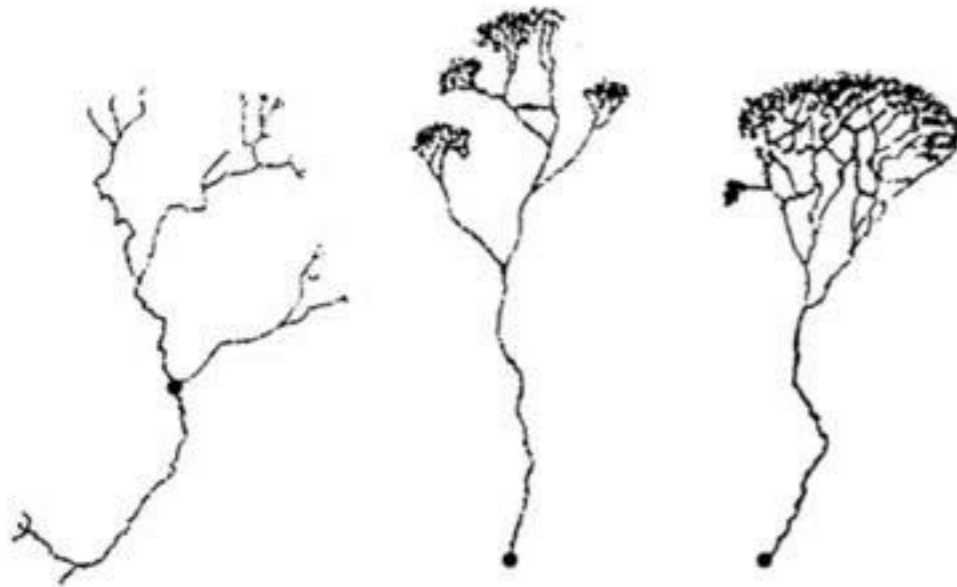


Doyle et al (2021) *Developmental Cell*



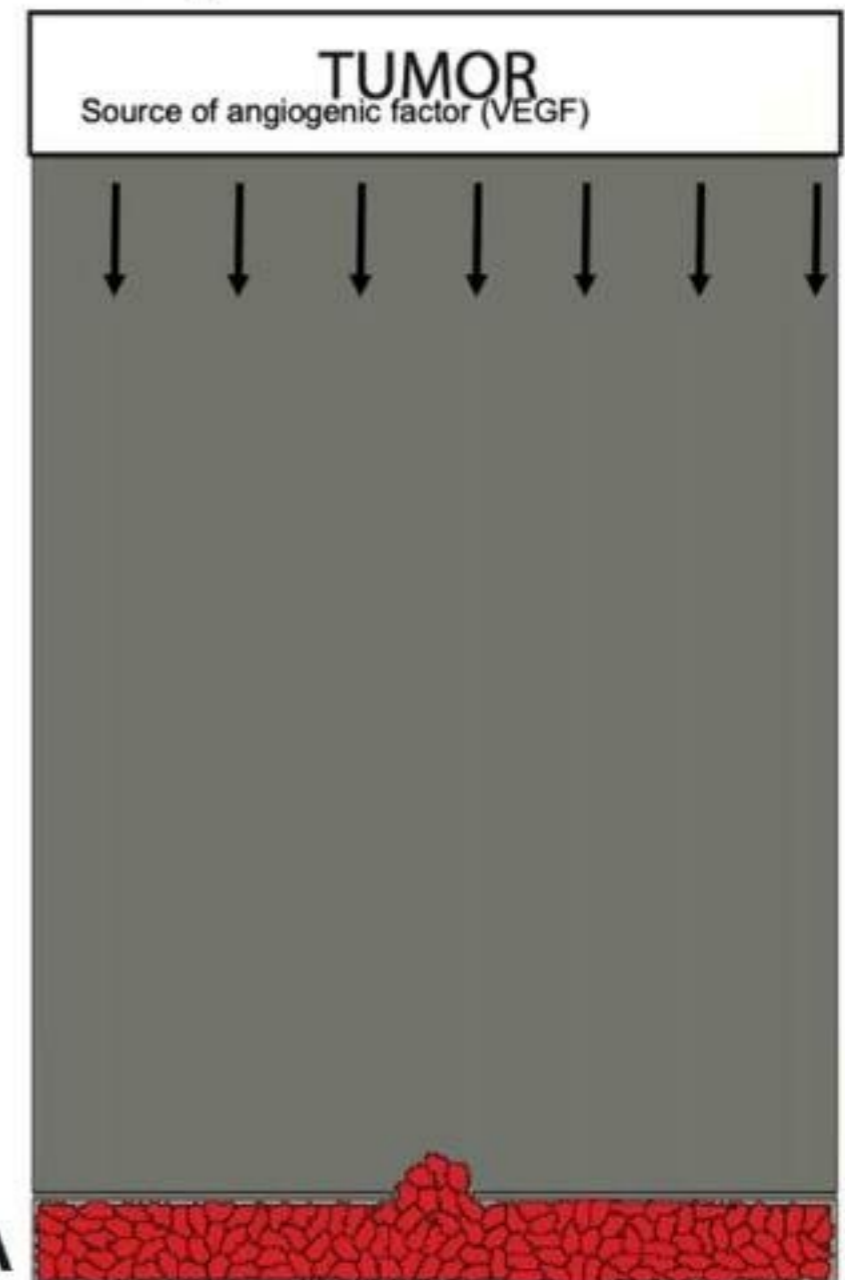
Extracellular matrix (ECM) coordinates angiogenesis

- ECM coordinates cells
 - ECM acts as “stigmergic” signal
 - *cf.* Pheromones in ant trail formation



Deneubourg et al. J. Insect Behav., 1989

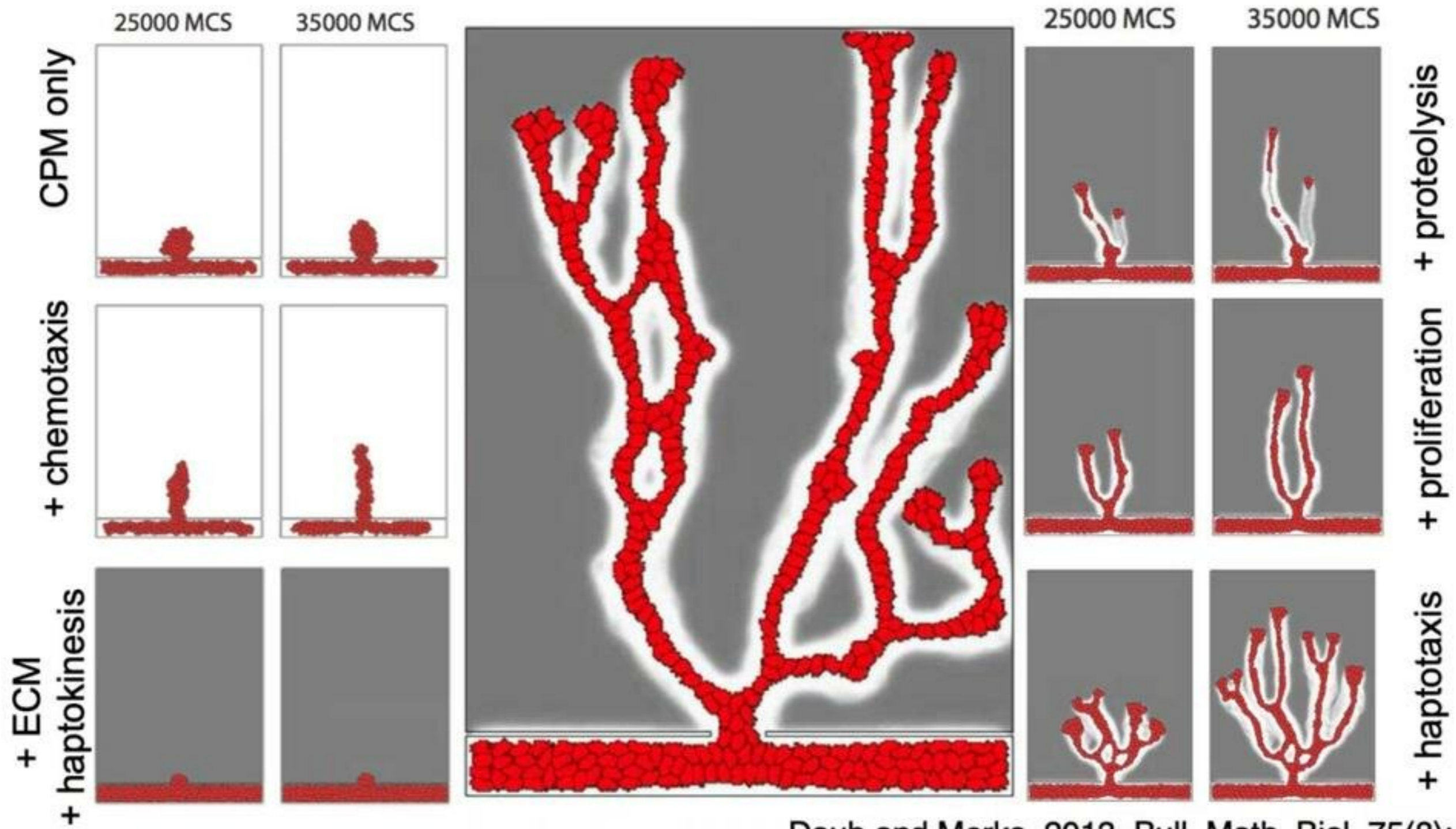
Explorative model:





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ECM as **chemical** signal: coordination of cell behavior during angiogenesis



Daub and Merks, 2013. Bull. Math. Biol. 75(8): 1377

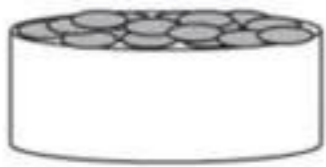
To build this model by yourself: Daub and Merks, *Methods in Molecular Cell Biology*, 2015



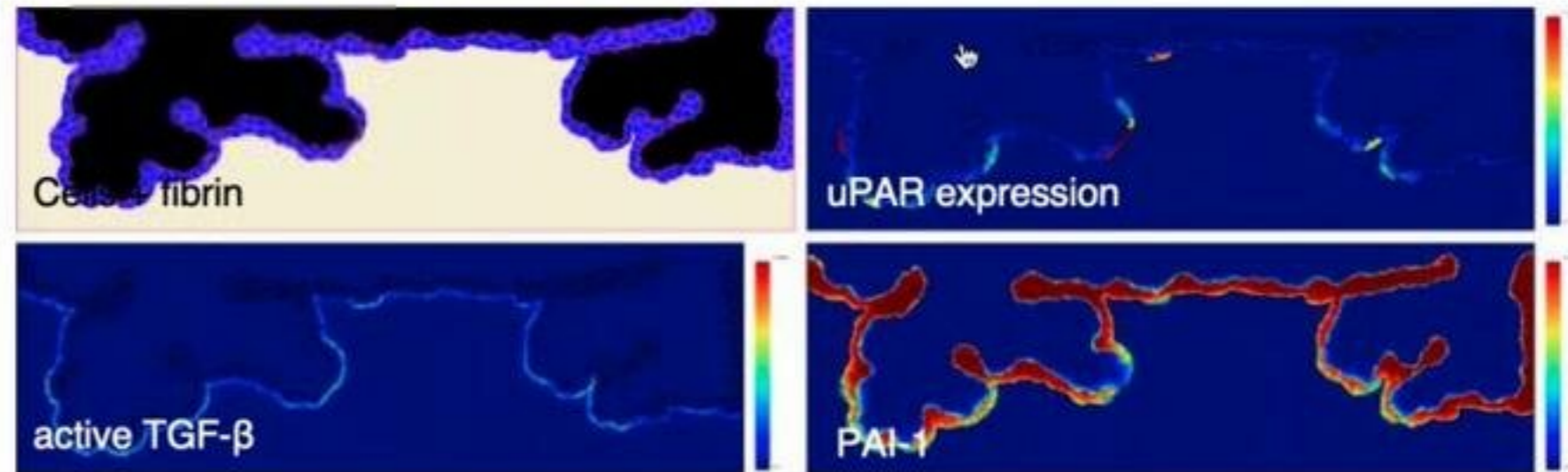
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ECM as cell-cell signal in human cell cultures *fibrin-hMVEC assay*

Monolayer of human microvascular endothelial cells on fibrin



Koolwijk *et al.* 1996

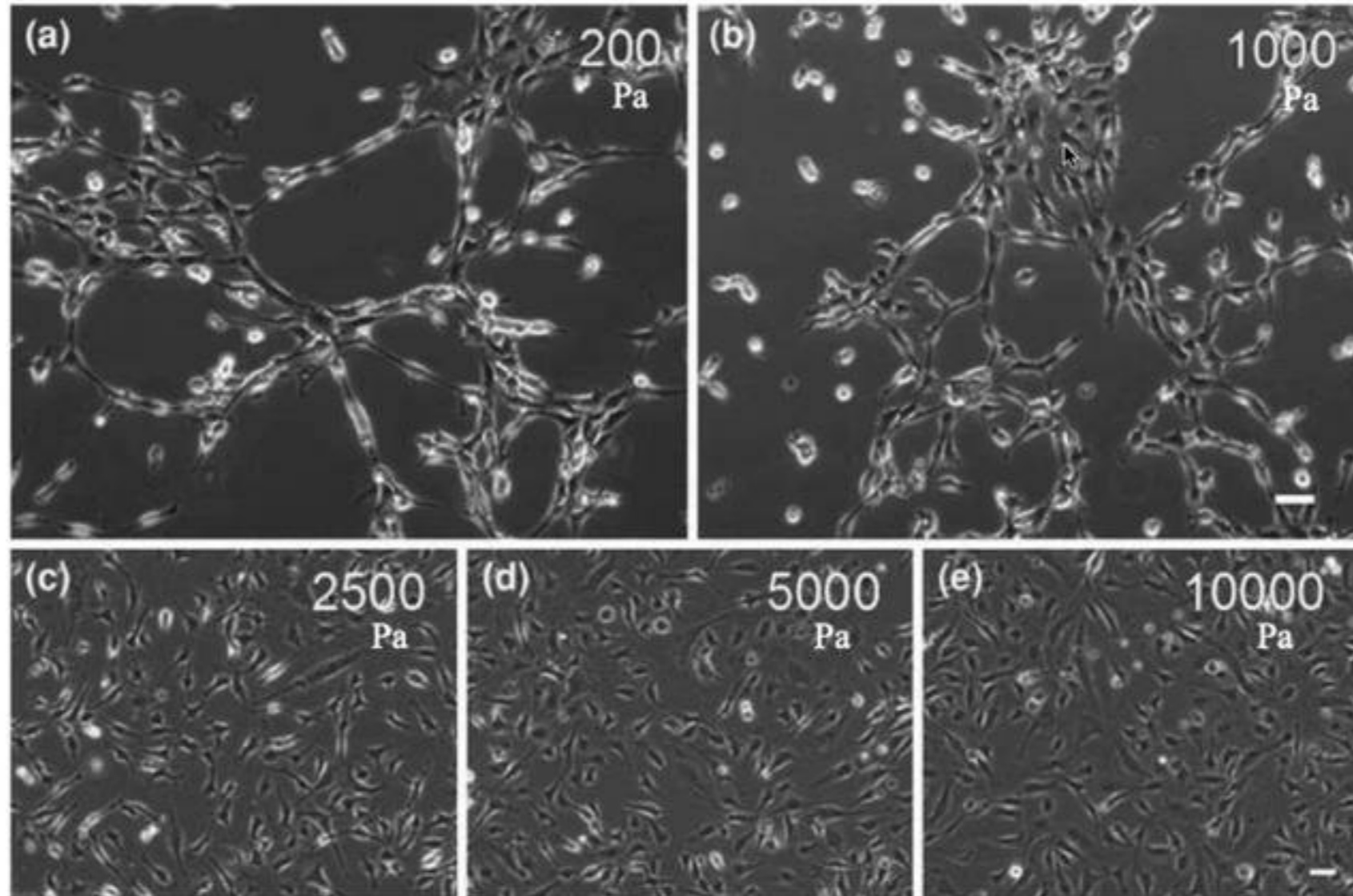


Boas *et al.* PLOS Computational Biology 2018



Stiffness of ECM affects vascular patterning

Soft matrix



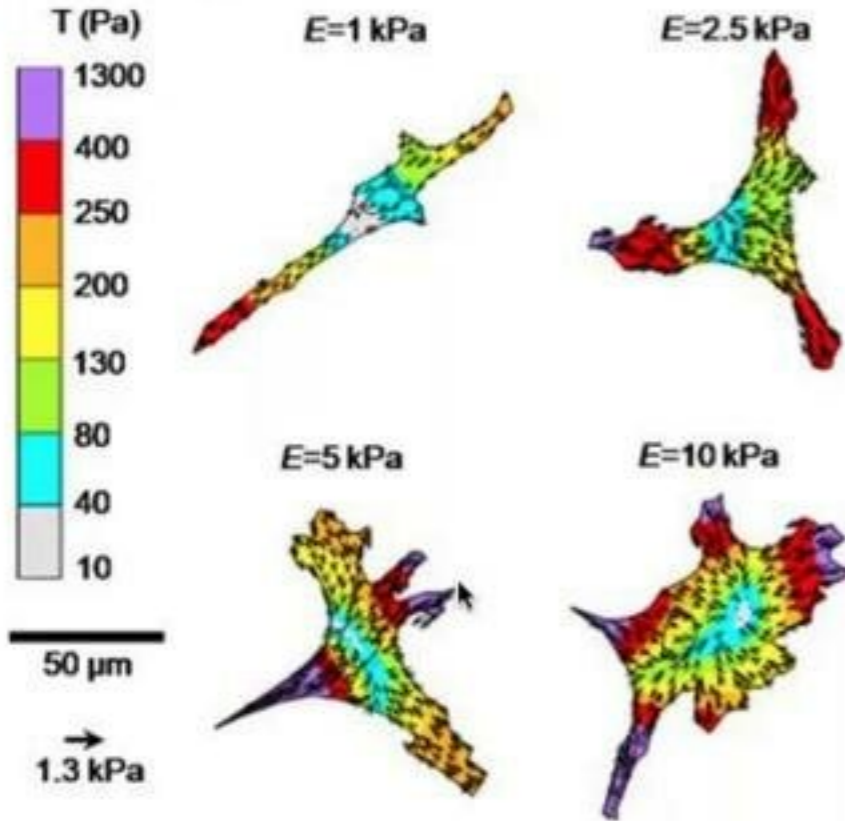
Califano and Reinhart-King, 2008

- **So: models must include substrate mechanics**

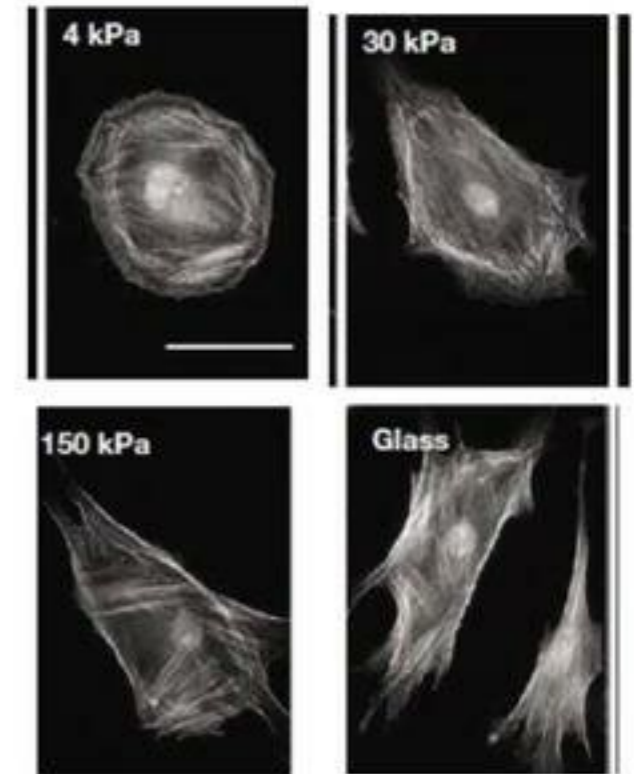
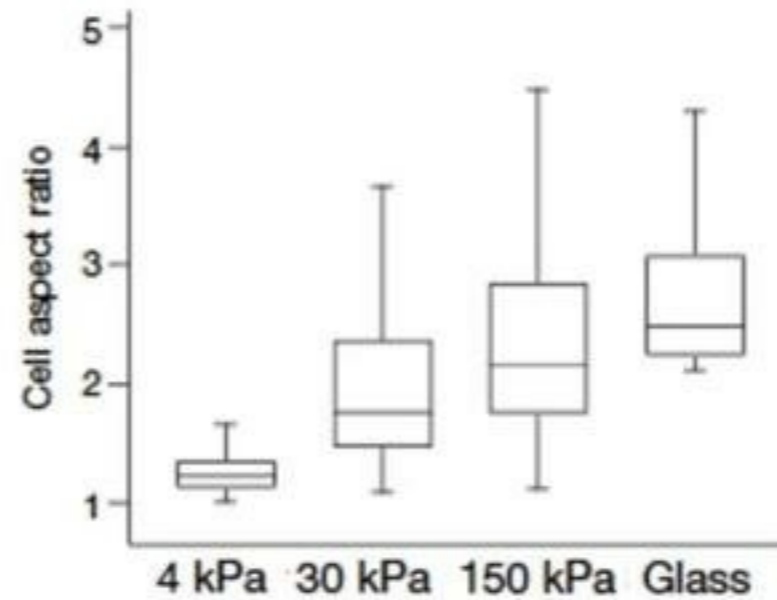


ECM stiffness affects cell shape

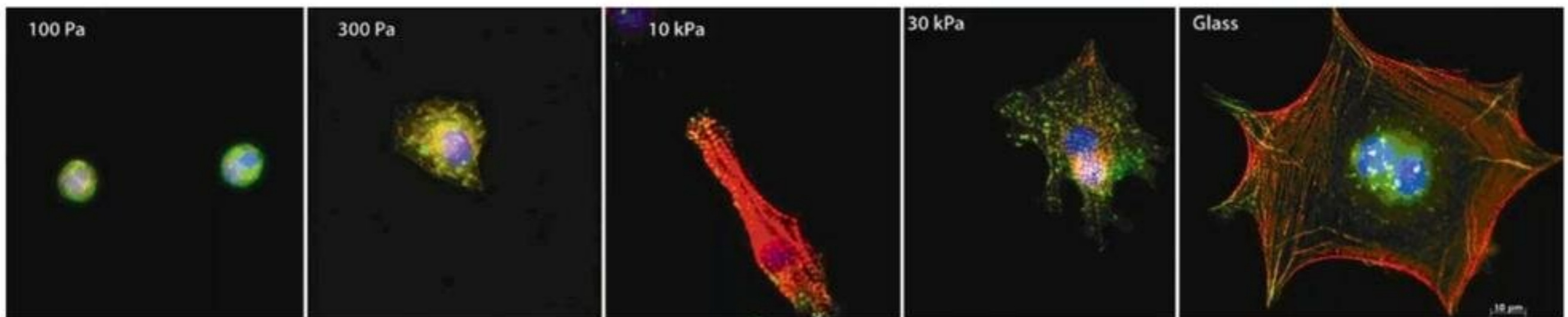
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Endothelial cells: Califano & Reinhart-King
Cell and Molecular Bioengineering 2010



Fibroblasts: Prager-Khoutorsky et al.
Nature Cell Biology 2011 (n=50)

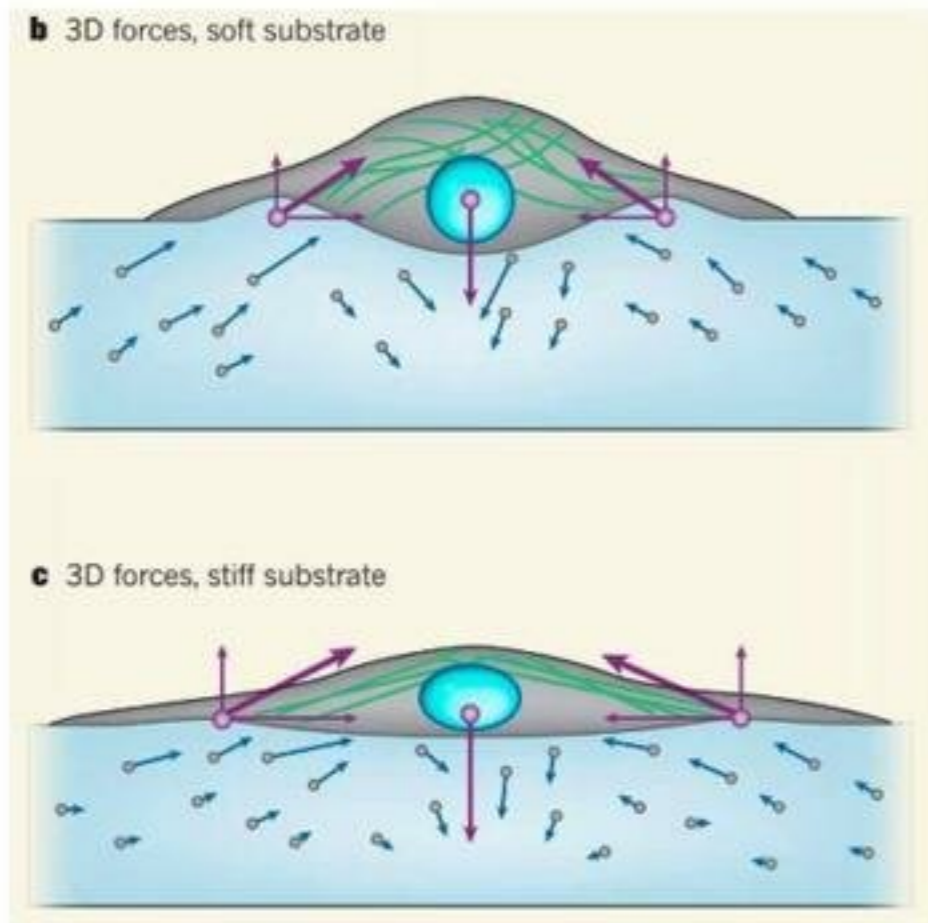


Cardiomyocytes: Winer et al. , in: Wagoner et al.
(eds.), 2011

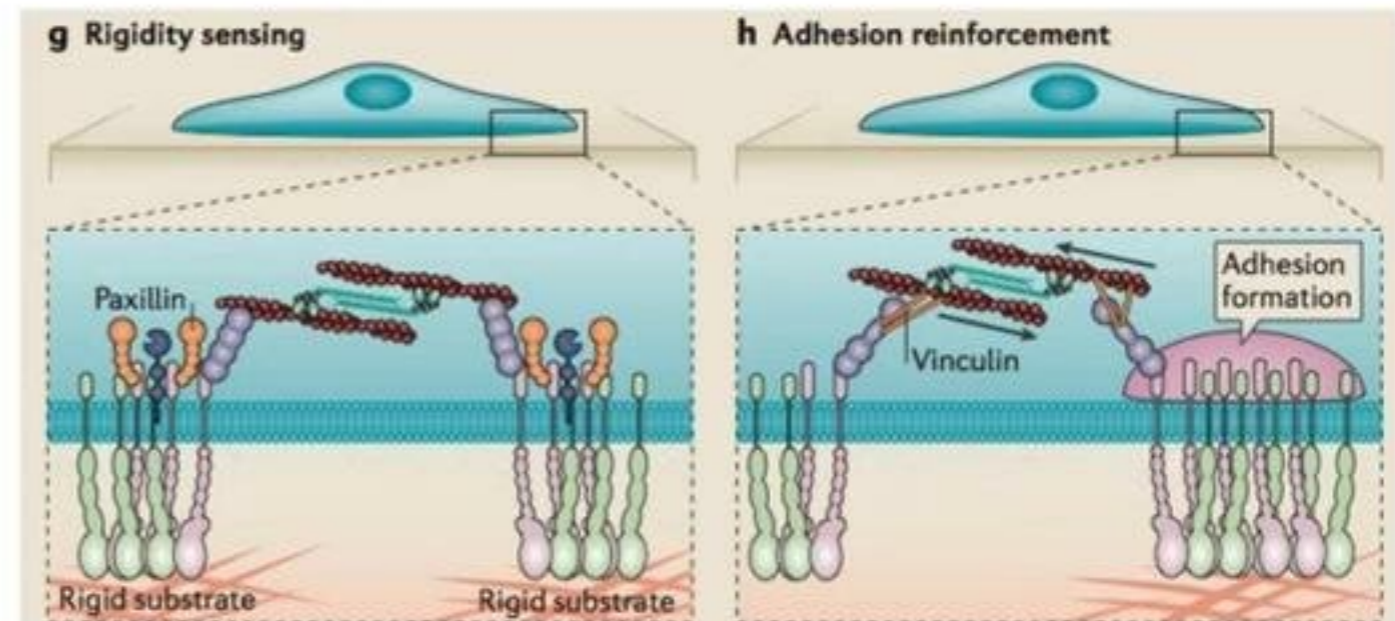


Mechanism: Mechanical reciprocity between cells and substrate

- (1) Cells pull on substrate
- (2) Cell-substrate connections stabilize on strained substrate



Hersen & Ladoux, Nature (2011)



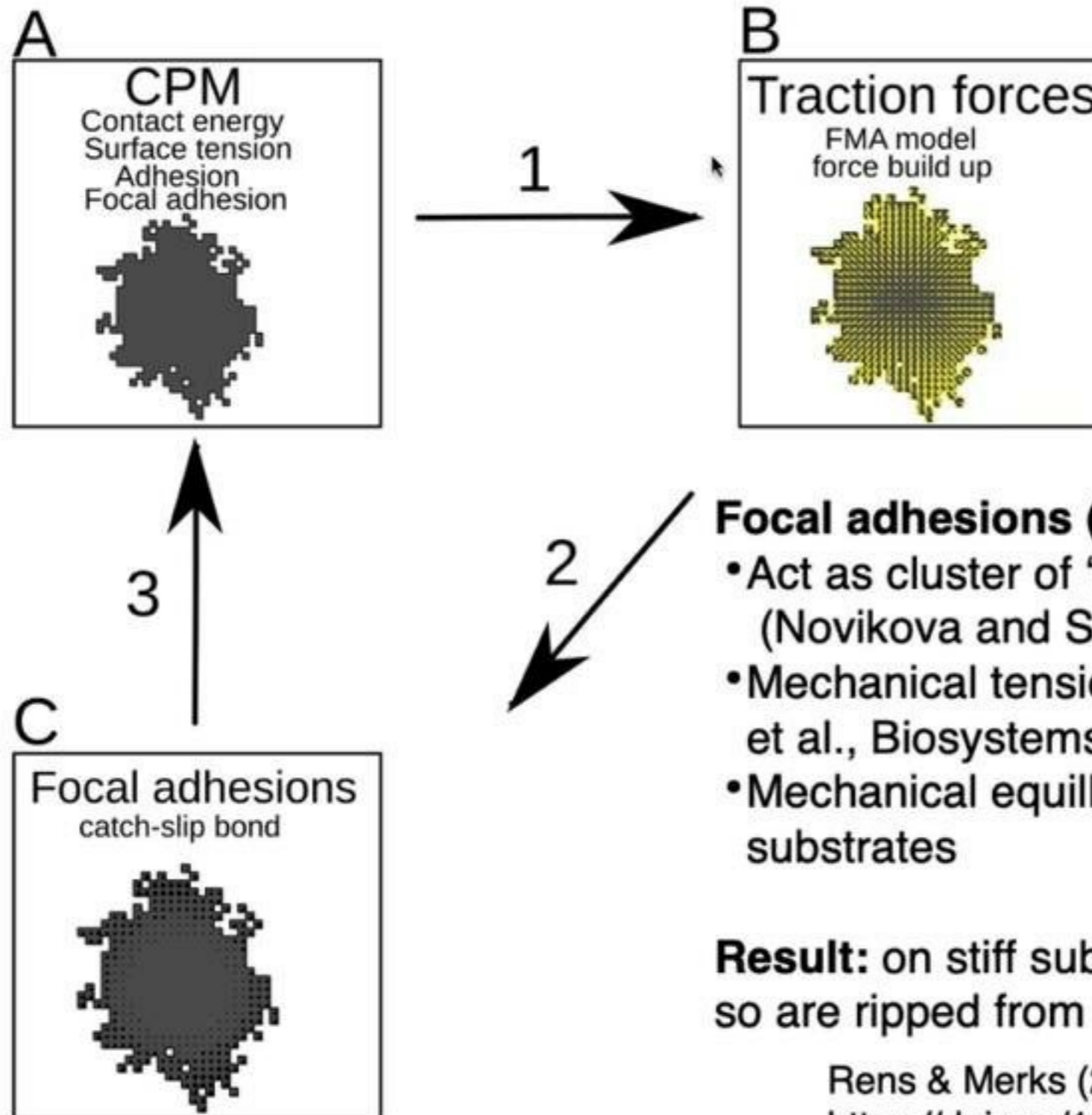
Iskratsch et al. Nat. Rev. Mol. Cell. Biol. (2014)



Mechanical reciprocity: Focal adhesions mature under force



Lisanne Rens



Focal adhesions (FAs):

- Act as cluster of 'catch-slip bonds' (Novikova and Storm, Biophys J 2014)
- Mechanical tension builds up over time (Schwarz et al., Biosystems 2006)
- Mechanical equilibrium reached faster on stiff substrates

Result: on stiff substrates FAs grow stronger, so are ripped from substrate less easily

Rens & Merks (2020) *iScience* 9: 101488
<https://doi.org/10.1016/j.isci.2020.101488>



Each focal adhesion (FA) is described by an ODE model

- Each FA of size $N_e(t)$ is a cluster of catch-slip bonds
(Novikova and Storm, *Biophys. J.* 2013: continuous assembly/disassembly)

$$\frac{dN_e(t)}{dt} = g(N_e(t) - N_t) - b(\phi_e(t))N_e(t)$$

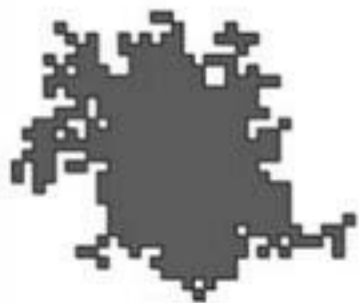
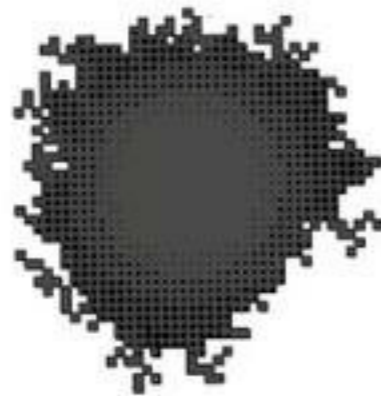
- Mechanical tension **inhibits** degradation of FAs
- Tension builds up **over time**, as (Schwarz et al. *Biosyst.* 2006),

$$\phi_e(t) = \left| F_s \left(1 - e^{-t/t_k} \right) \right|$$

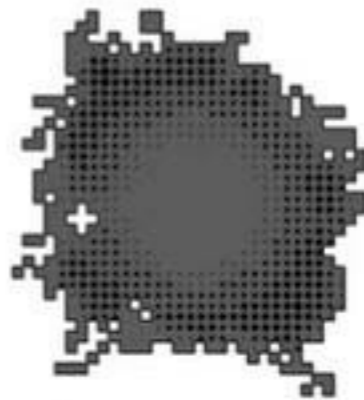
- with $t_k = F_s / v_0 K$; function of stall force F_s , contraction velocity of actomyosin cables v_0 and K , matrix stiffness
- Within a fixed time interval, FAs experience **less tension on soft matrices** than on stiff matrices



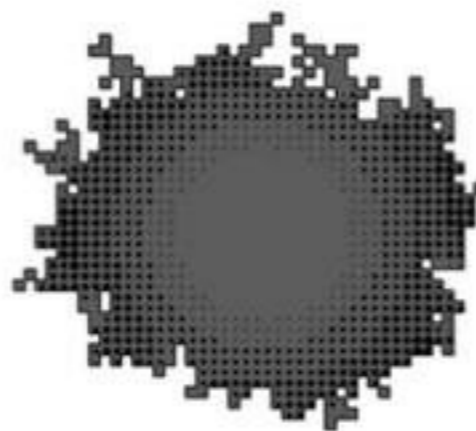
Detailed model explains cell spreading, but not elongation



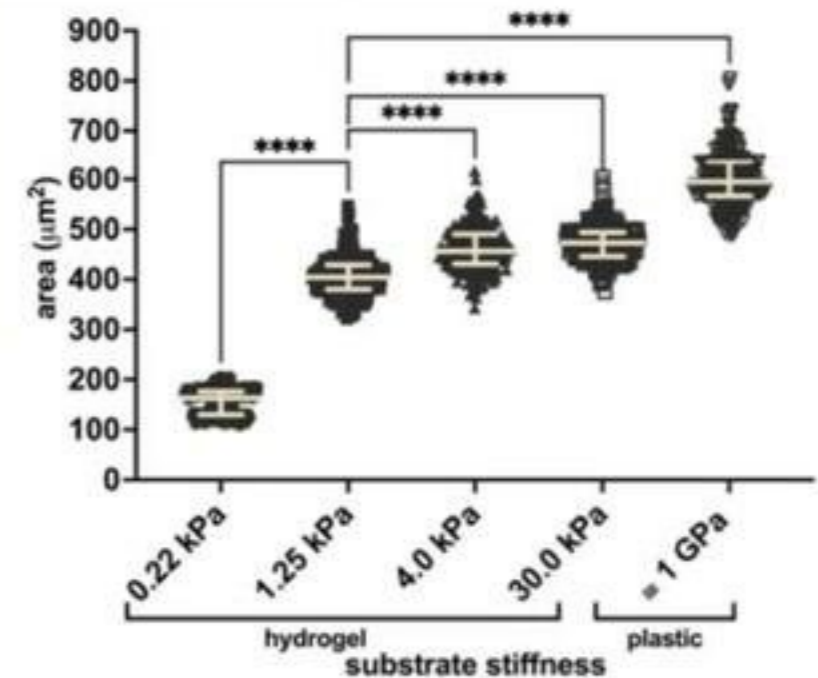
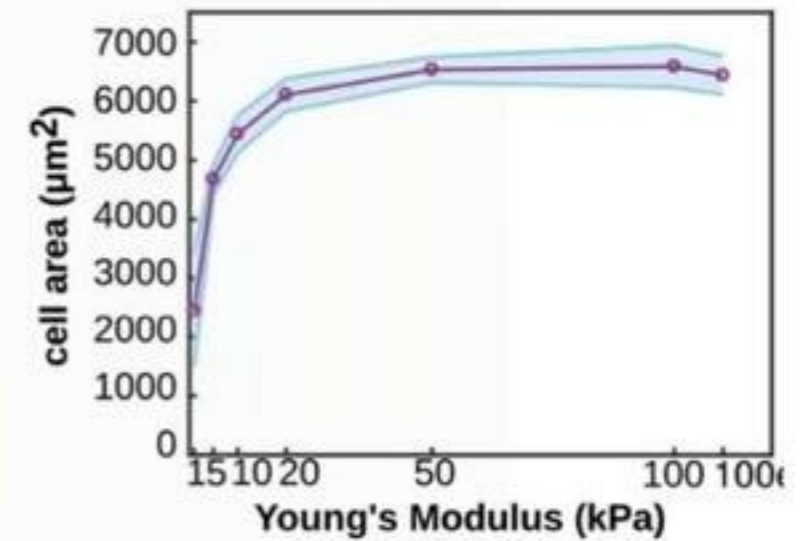
1kPa



5kPa

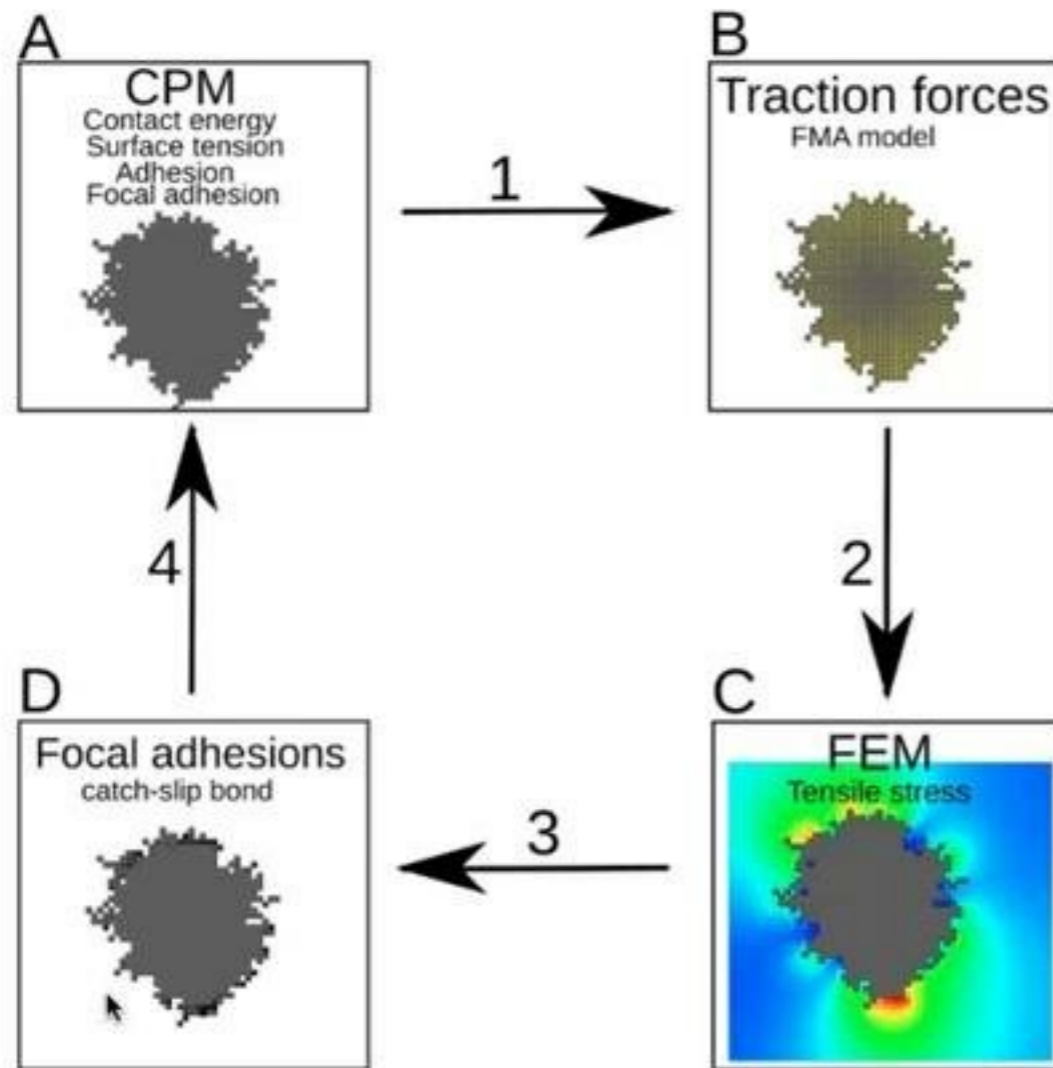


50kPa

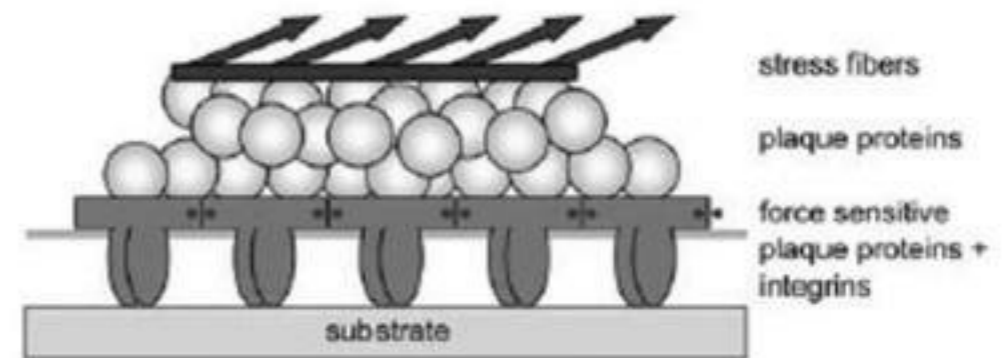




Feedback from ECM-deformation required for cell elongation



Planar substrate stress strengthens adhesions



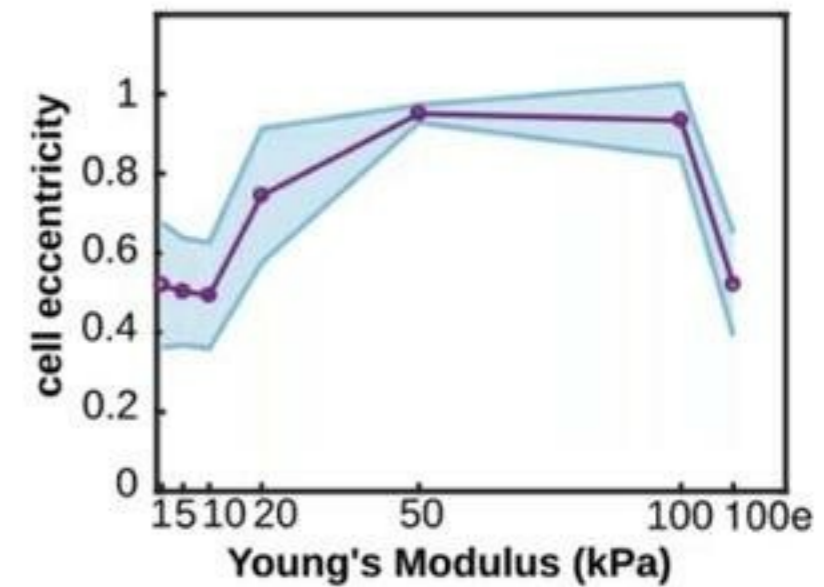
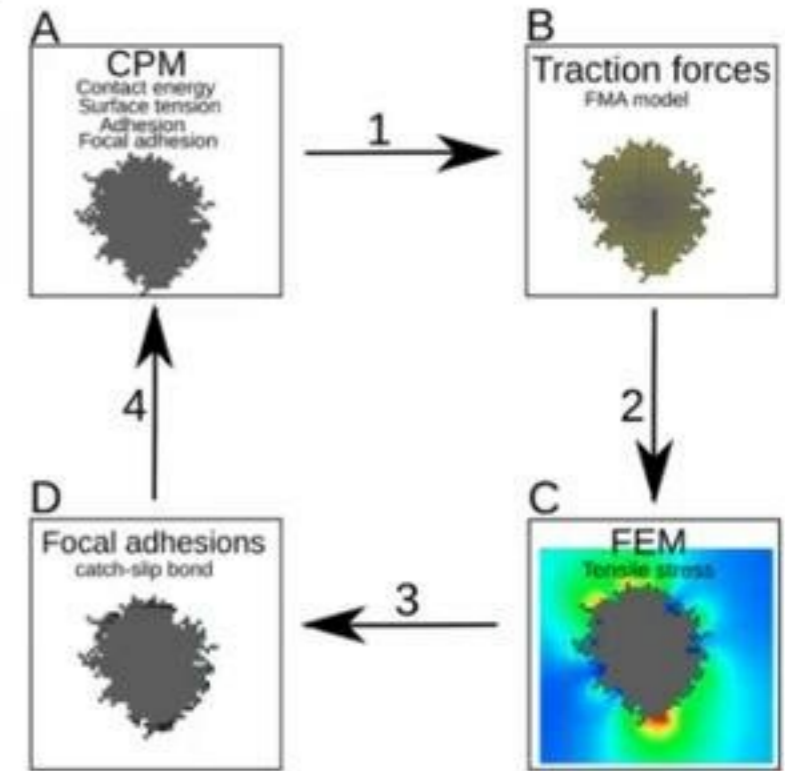
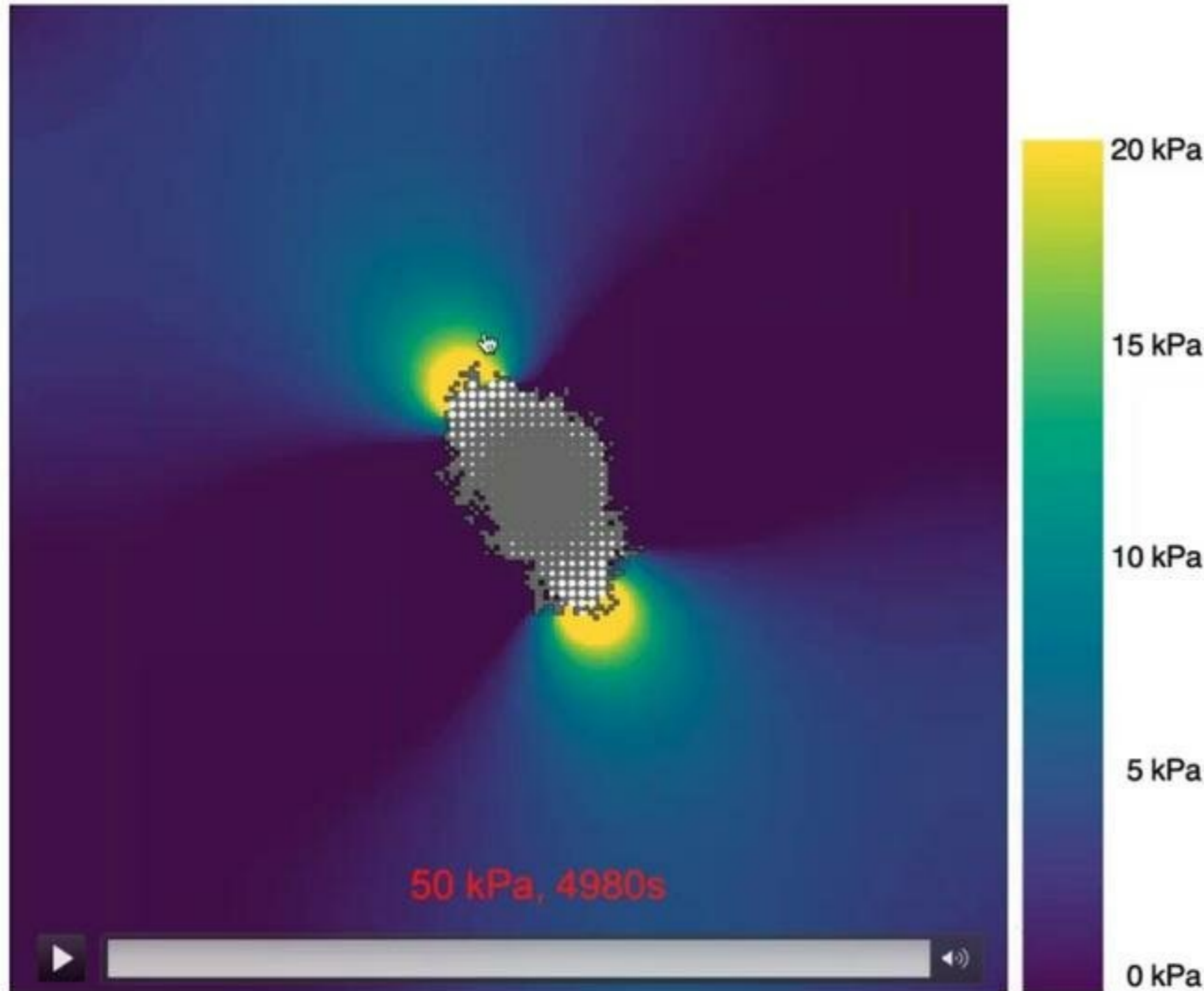
Besser et al. 2006

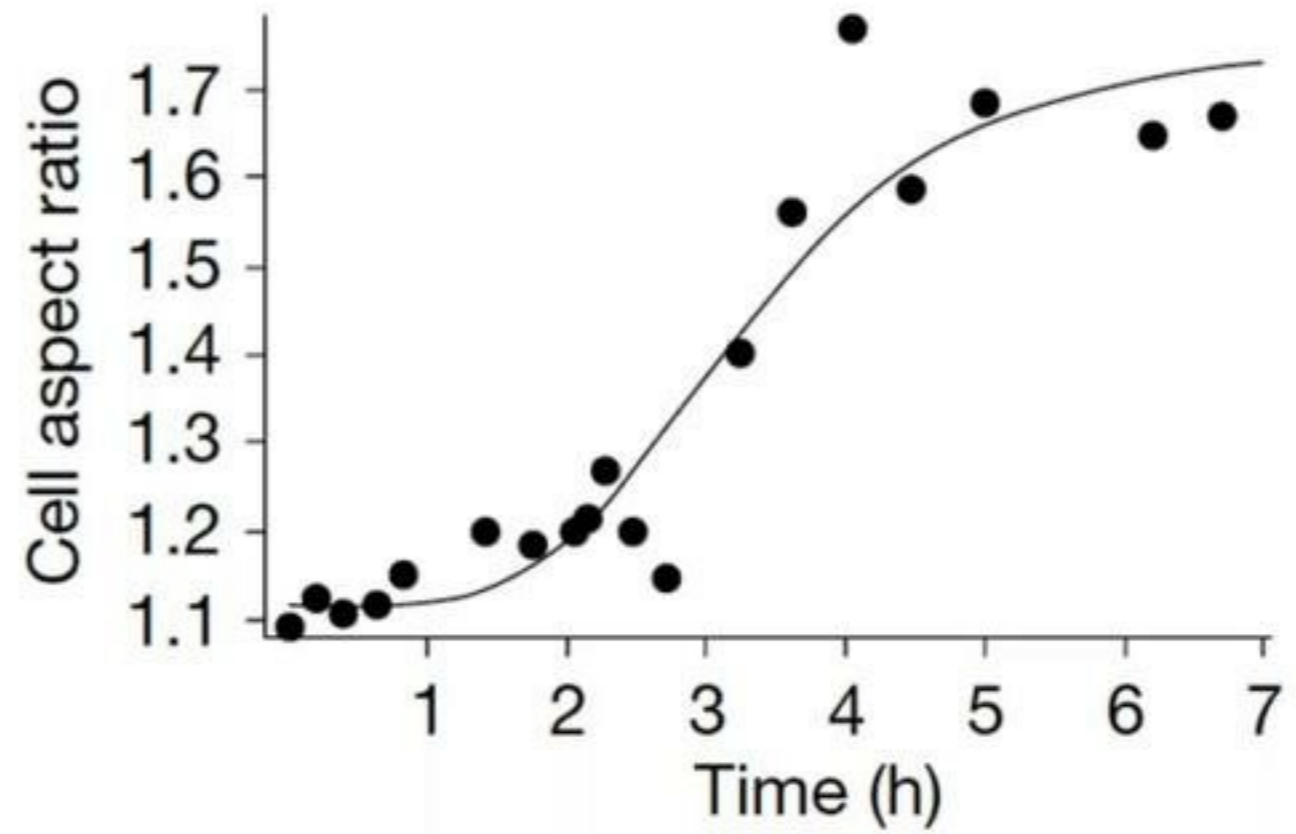
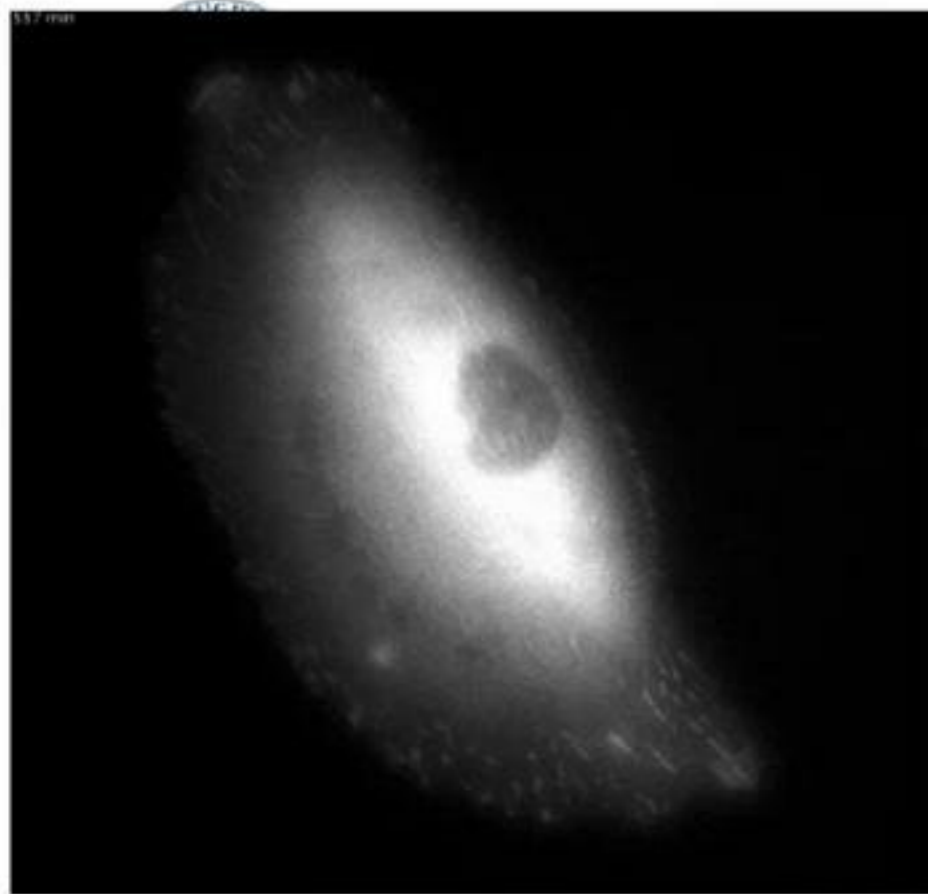
$$\Delta H_{\text{work}} = \lambda_N \frac{N(\vec{x})}{N_h + N(\vec{x})} \left(1 + p \frac{h(s(\vec{x}))}{s_o + h(s(\vec{x}))} \right)$$

with $h(s(\vec{x})) = \frac{1}{2}(s_{xx} + s_{yy})$ the hydrostatic stress of the substrate

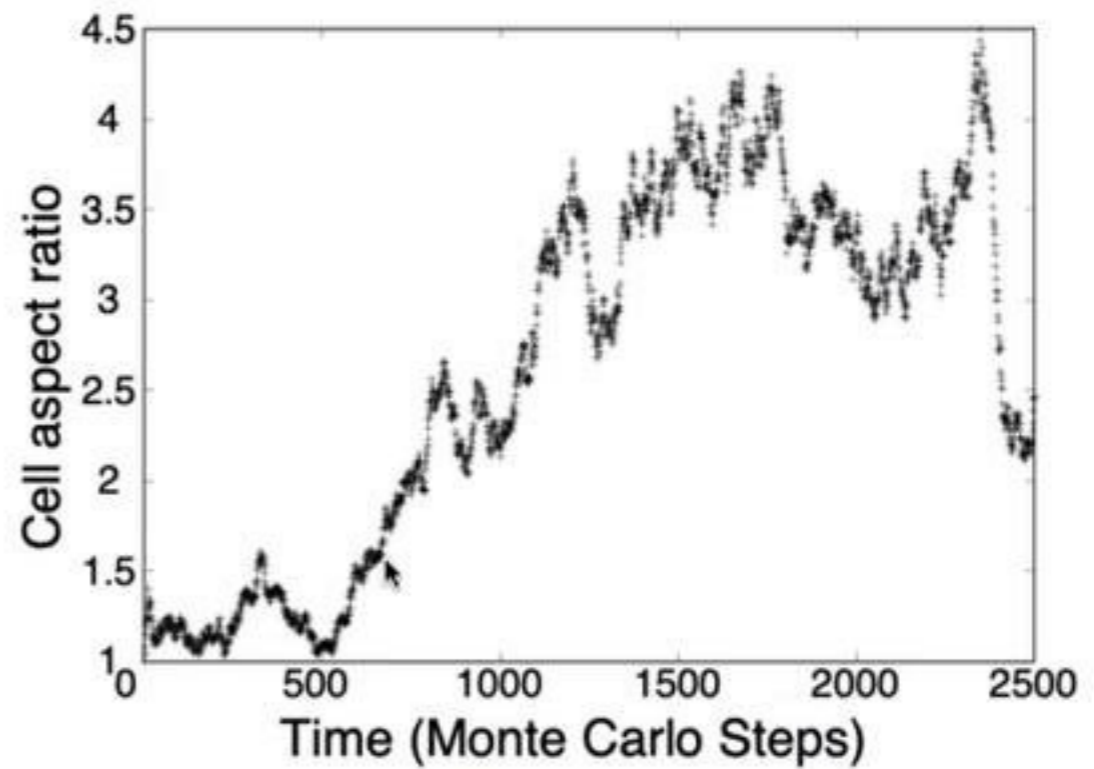
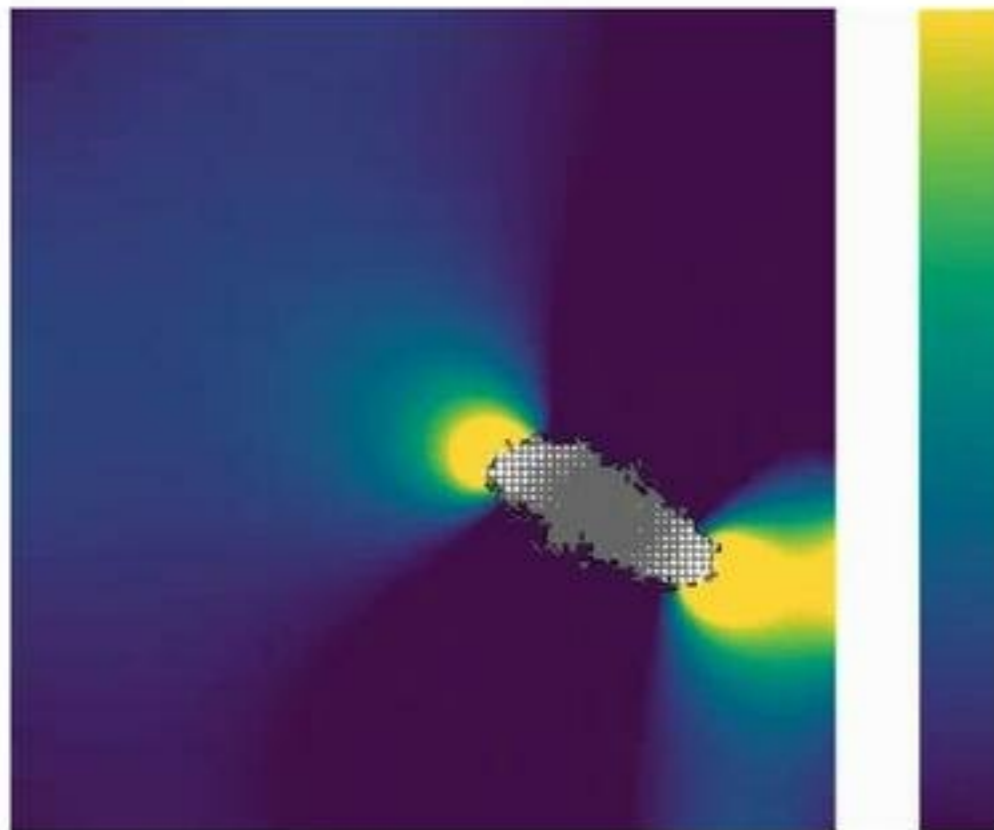


Cells elongate with substrate reciprocity





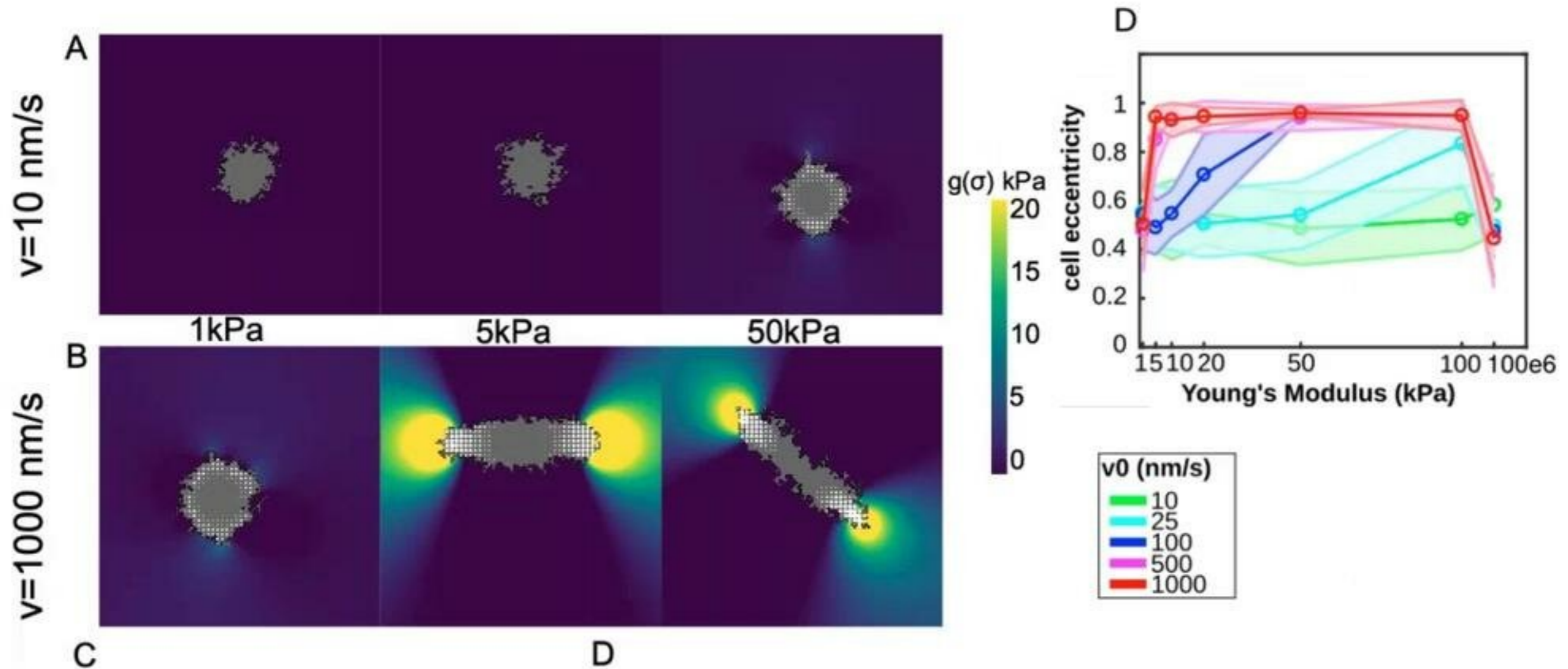
Fibroblast on 2 MPa substrate; Prager-Khoutrosky ... Bershadsky, Nature Cell Biology 2011



Simulated cell on 'stiff' substrate (qualitative!)



Speed of actomyosin contraction determines at what stiffness cells elongate

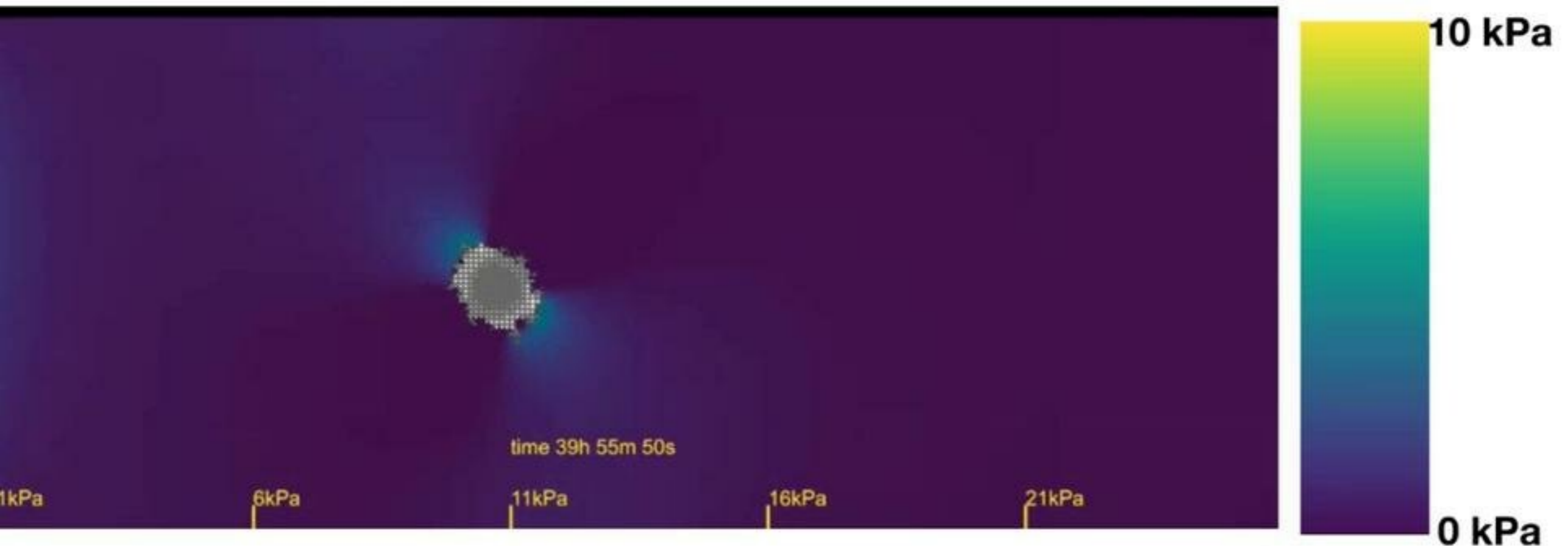




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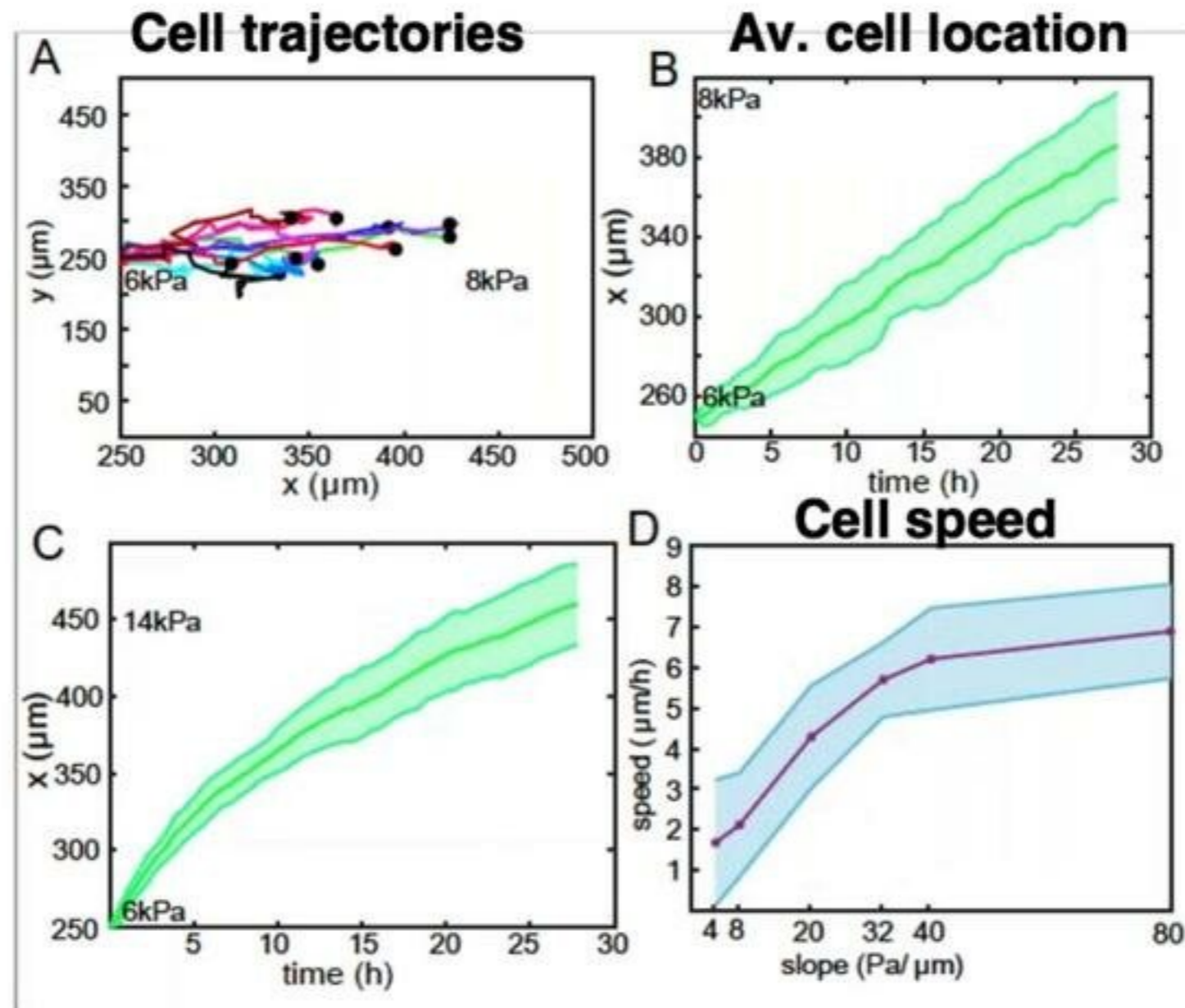
Durotaxis

Cells move to higher stiffness





Durotaxis: Faster movement on steeper slopes



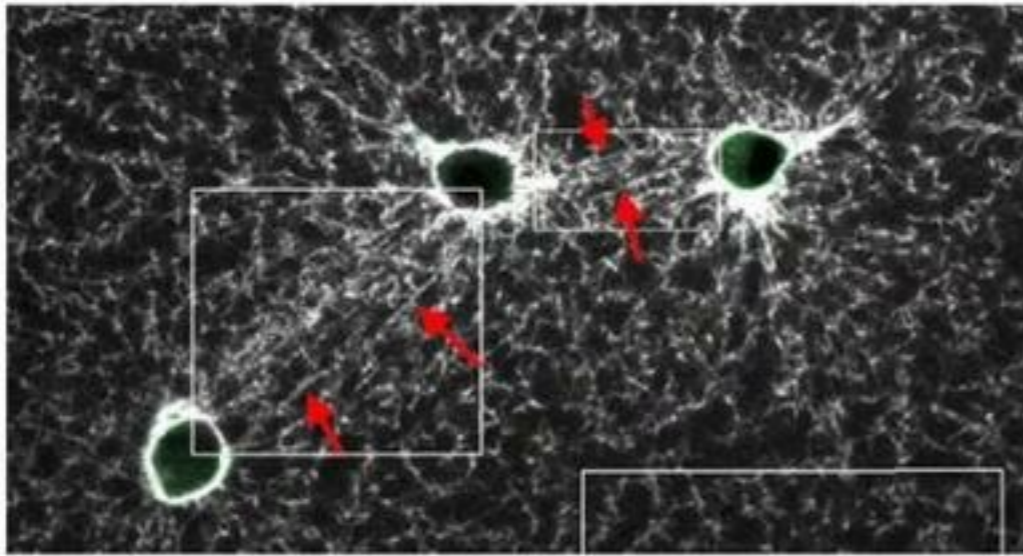


From **isotropic** ECMs to **fibrous** ECMs

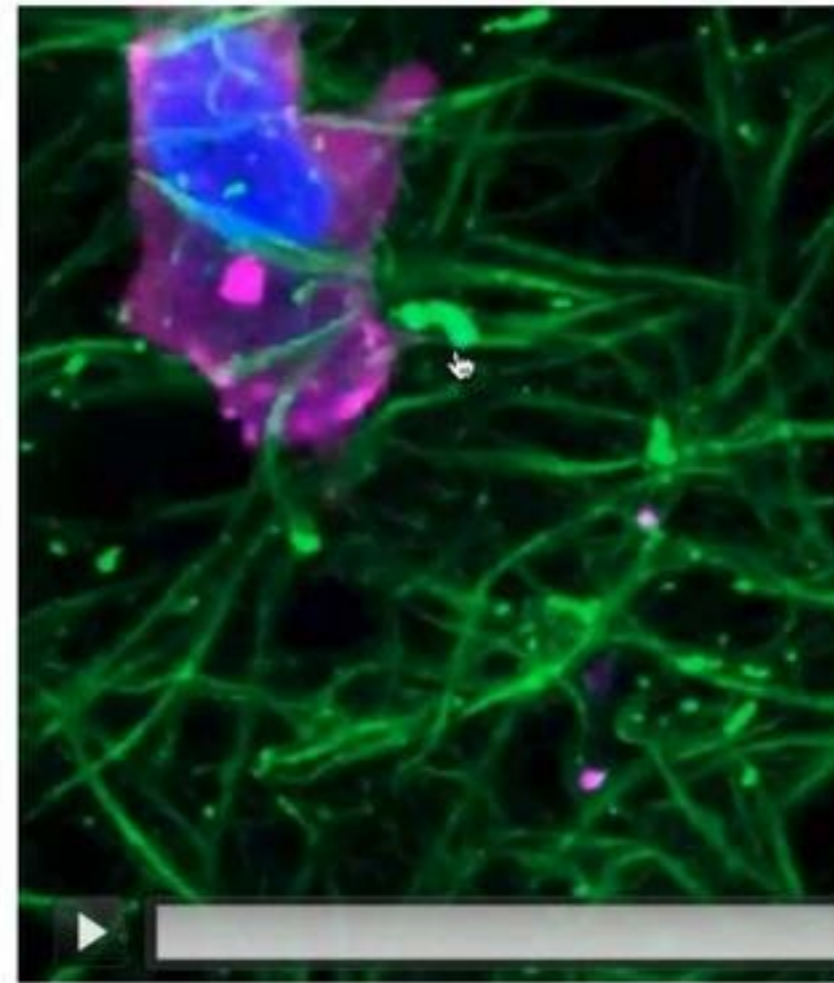
Is it correct to model the ECM as an isotropic material?



Was it correct to model ECMs as an isotropic material?

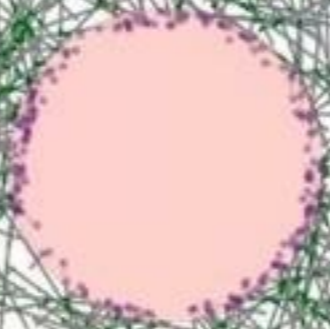


Mann et al. (2019) *Journal of the Royal Society Interface*



Doyle et al (2021) *Developmental Cell*

CPM with fibrous ECM





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CPM with fibrous ECM



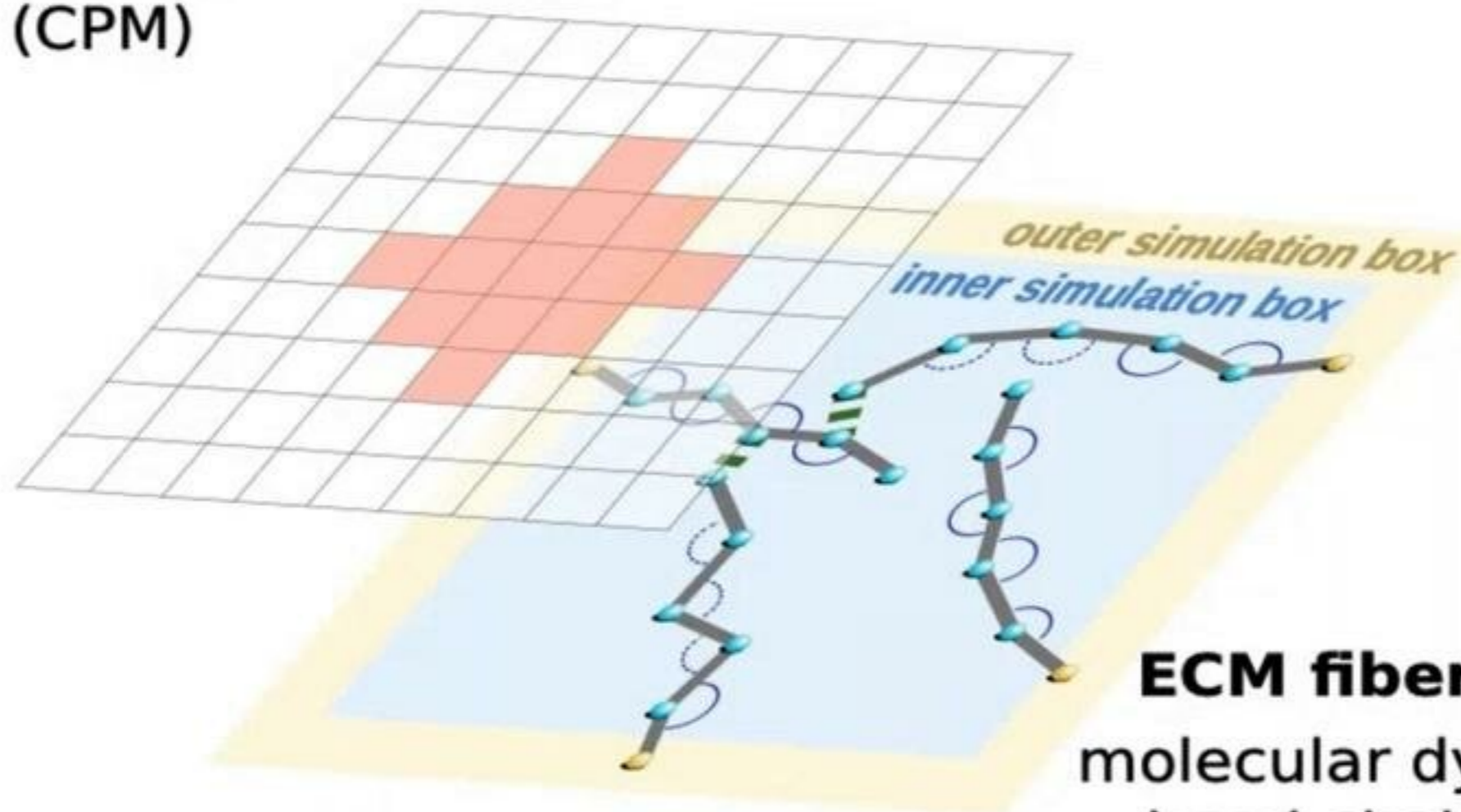
Bente Hilde Bakker



Erika Tsingos

cell model

cellular Potts model
(CPM)



ECM fiber model

molecular dynamics
bead-chain model



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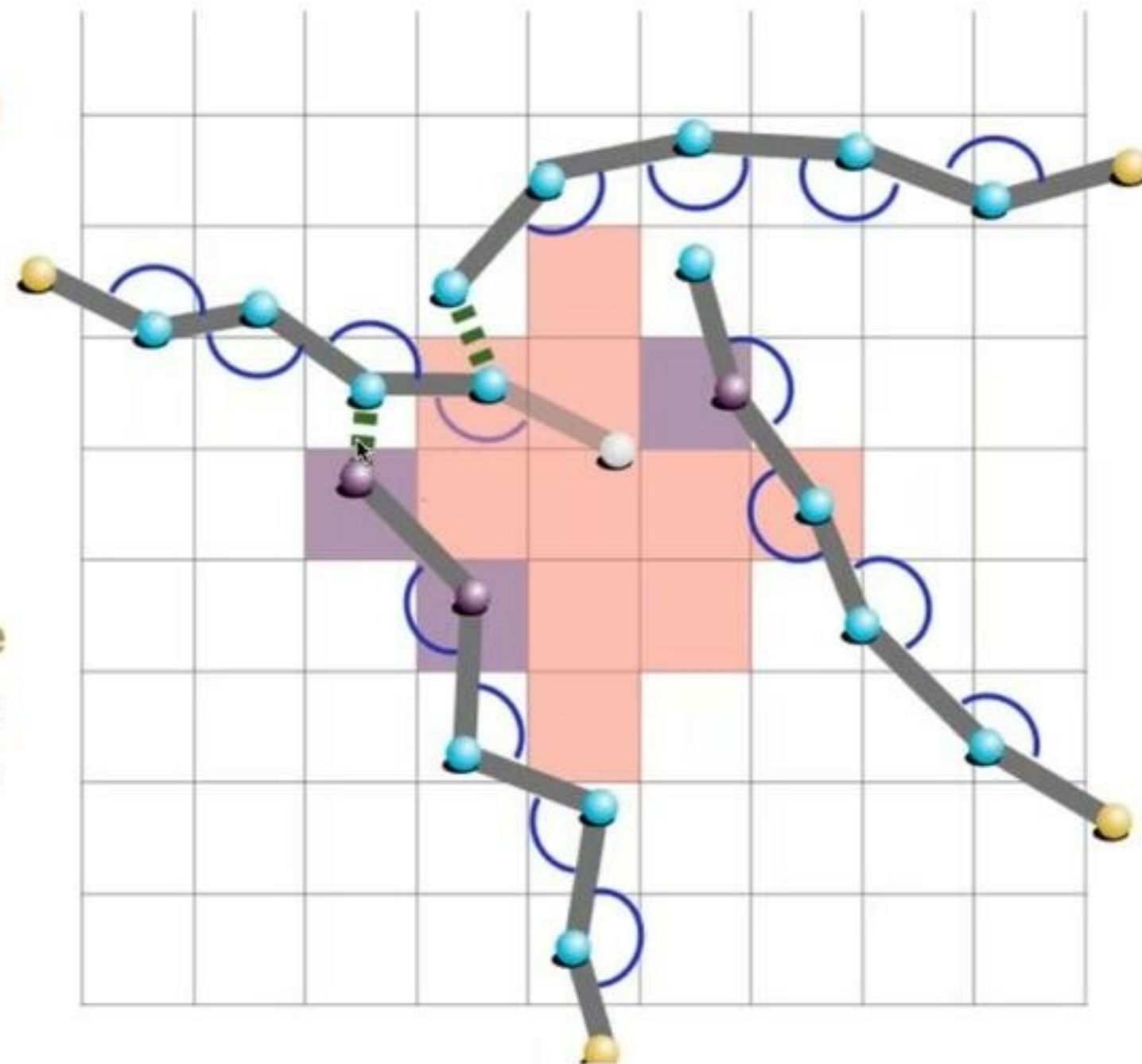
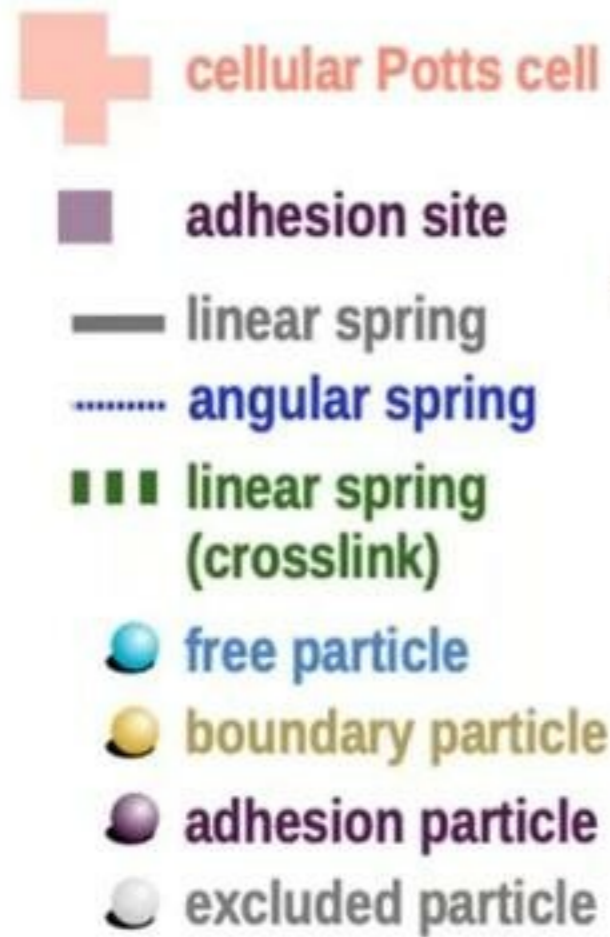
CPM with fibrous ECM



Bente Hilde Bakker



Erika Tsingos





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CPM with fibrous ECM

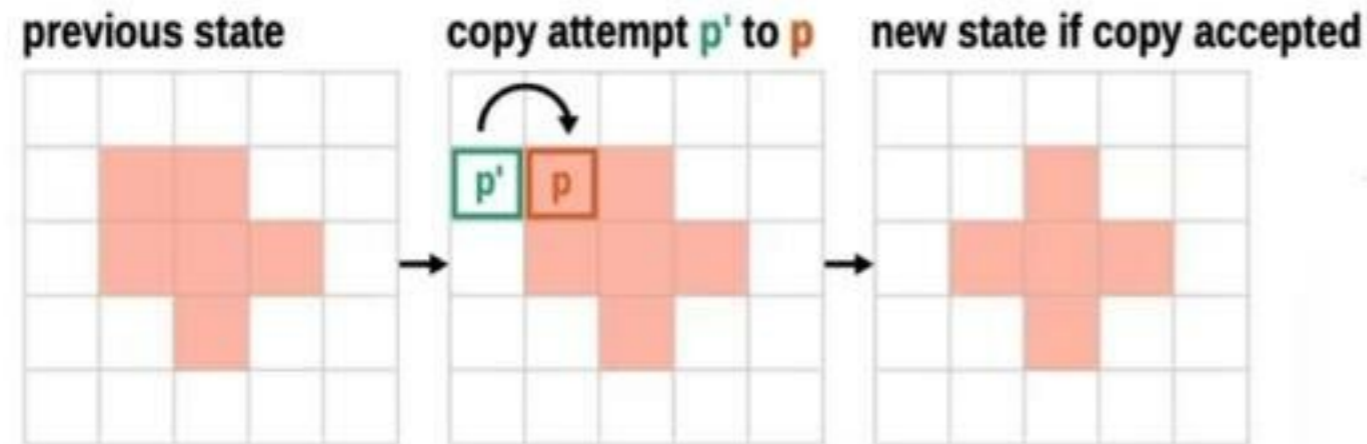


Bente Hilde Bakker

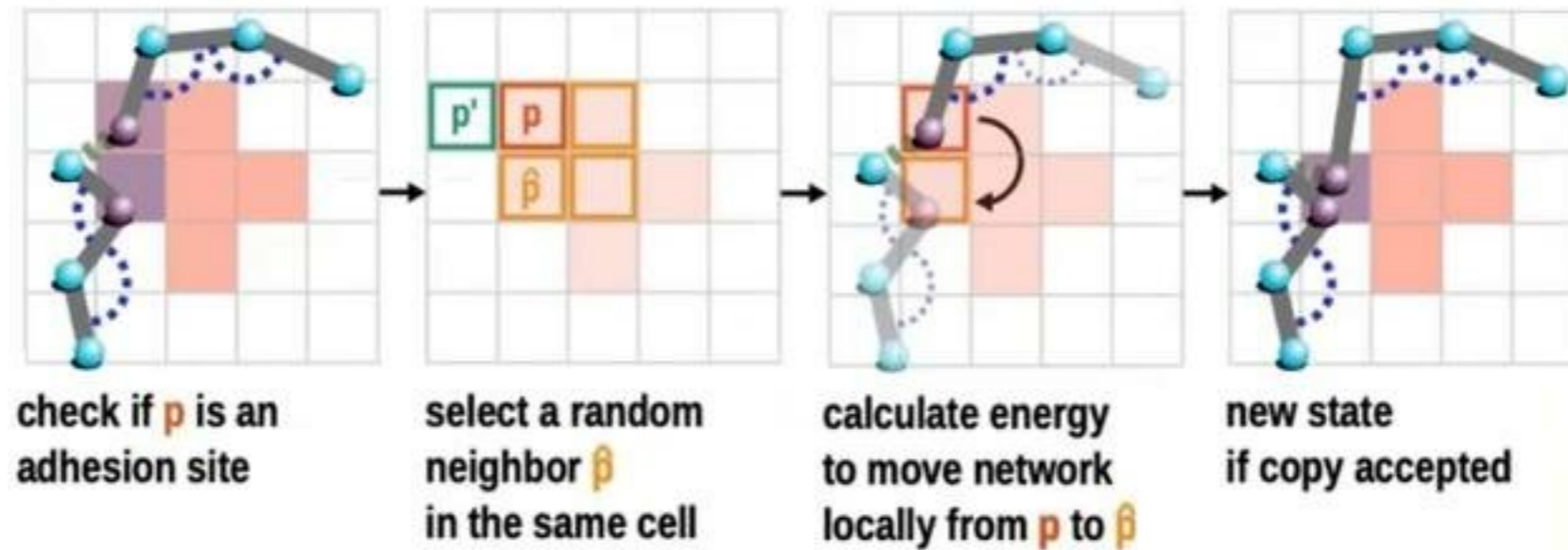


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standard CPM



with ECM bead-chain model





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CPM with fibrous ECM



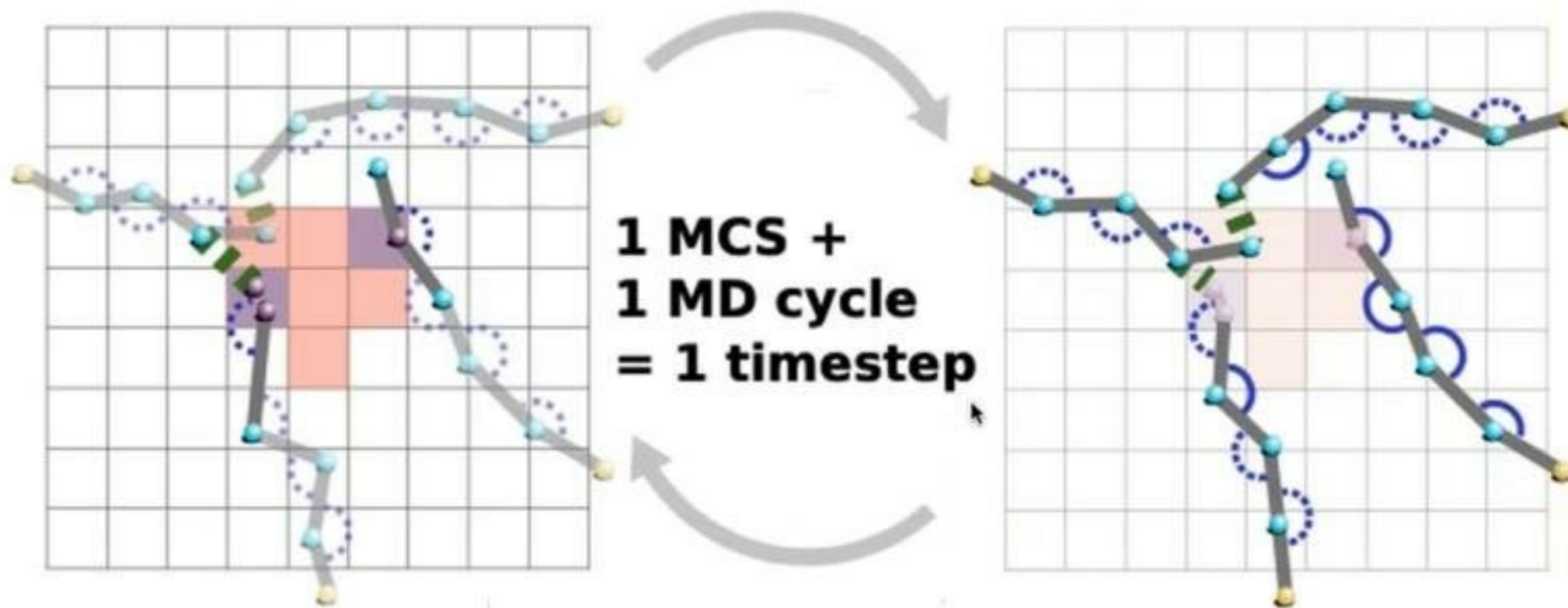
Bente Hilde Bakker



Erika Tsingos

1 MCS

- Assume network quasi-steady state
- Compute CPM Hamiltonian



1 MD cycle



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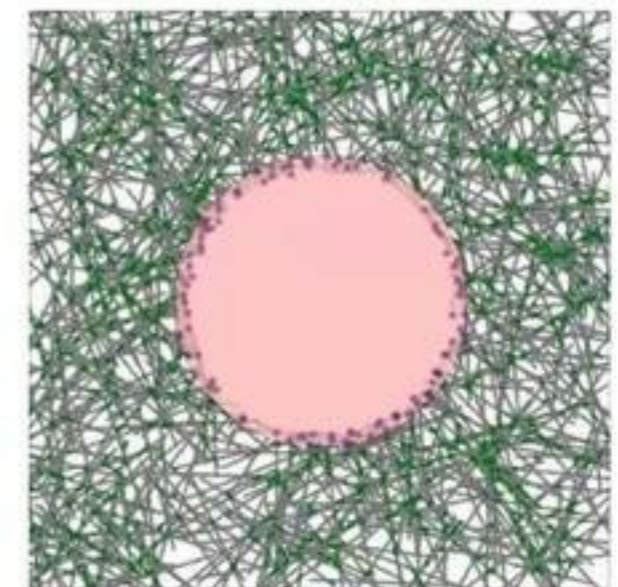
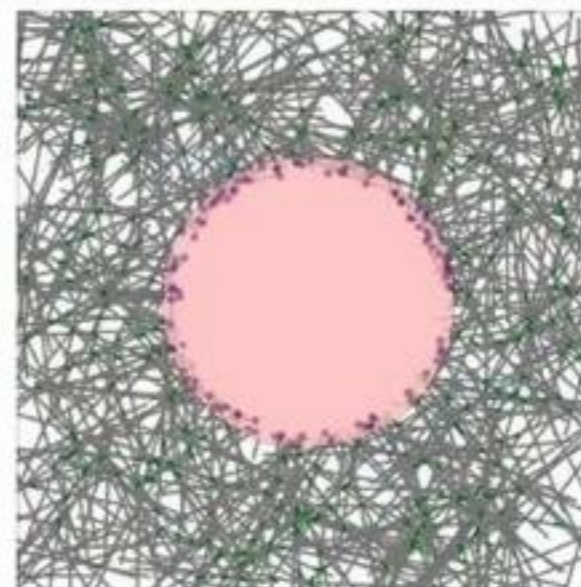
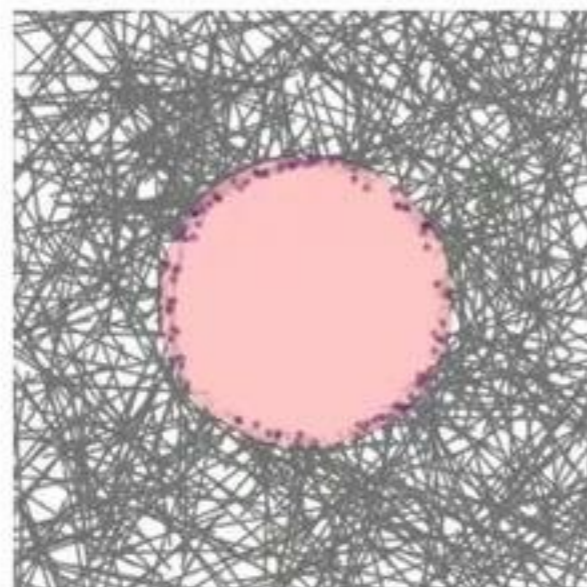
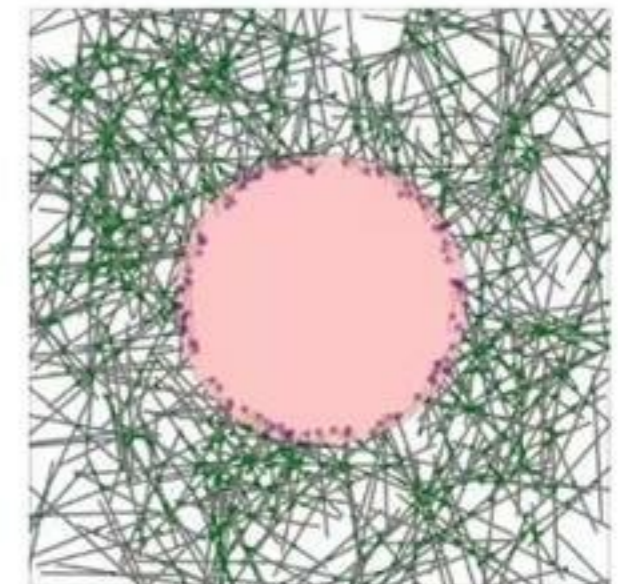
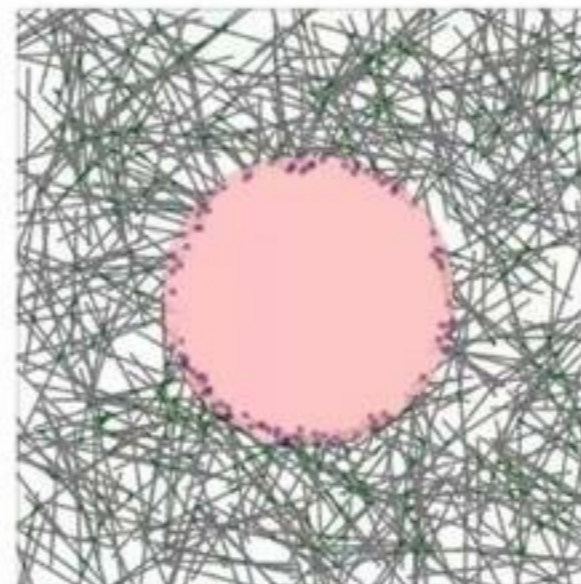
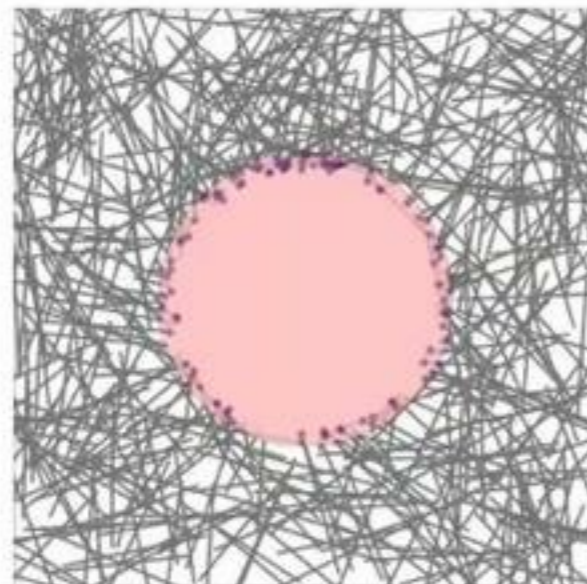
Effect of fiber density and cross-linker density

Cross-linker density

0 per μm^2

0.2 per μm^2

0.8 per μm^2



Fiber density:

~9.4 % v/v
~1.0 mg/ml
collagen [1]

~14.1 % v/v
~2.0 mg/ml
collagen [1]

Assuming fiber diameter of $0.25 \mu\text{m}$ and length of $12.5 \mu\text{m}$; domain height = $1 \mu\text{m}$. [1] Kreger et al. Biopolymers 93.8 (2010): 690-707.



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Effect of fiber density and cross-linker density

Cross-linker density

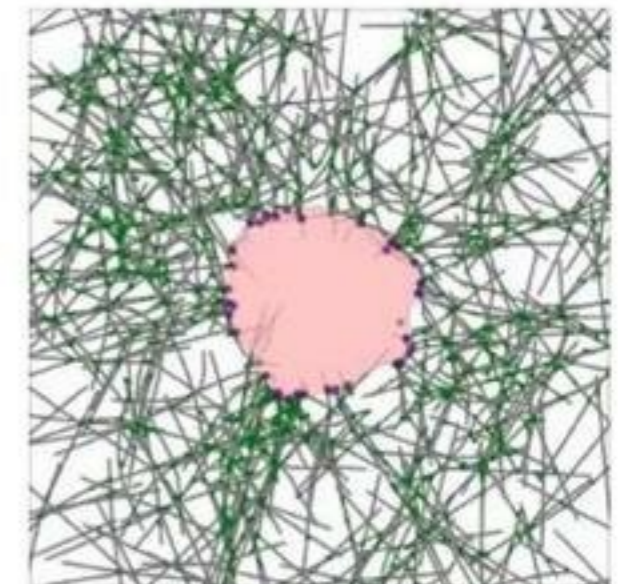
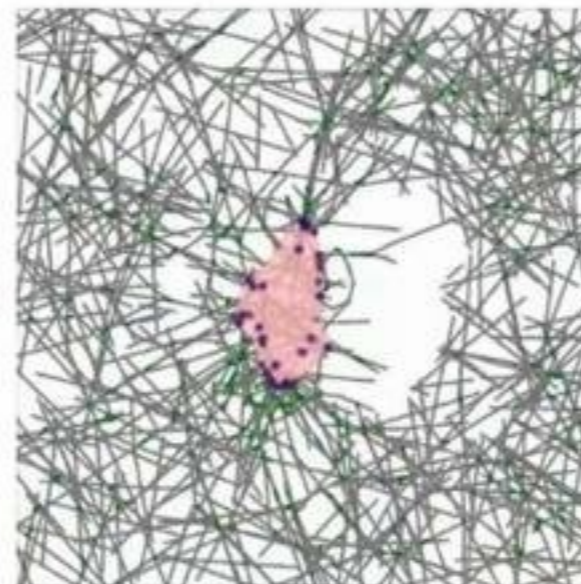
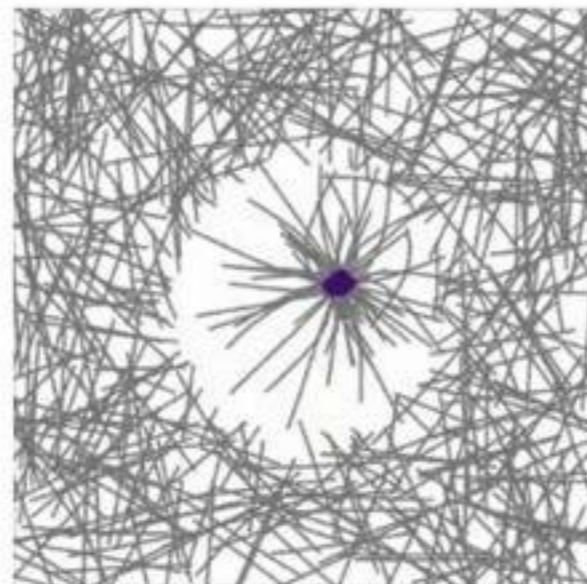
0 per μm^2

0.2 per μm^2

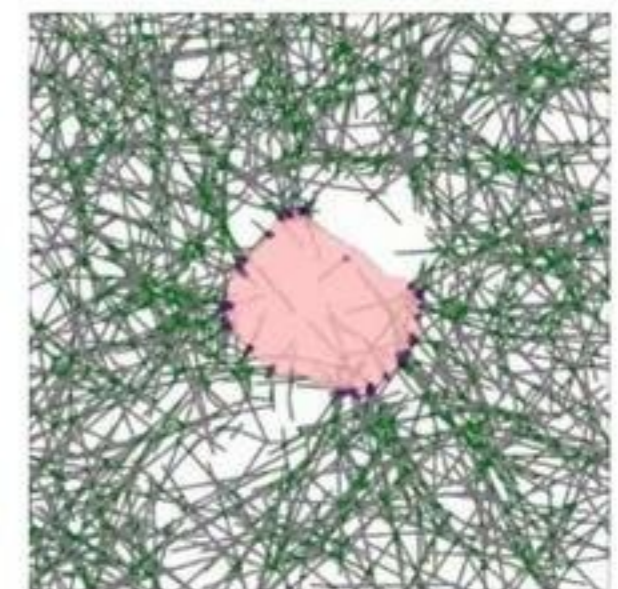
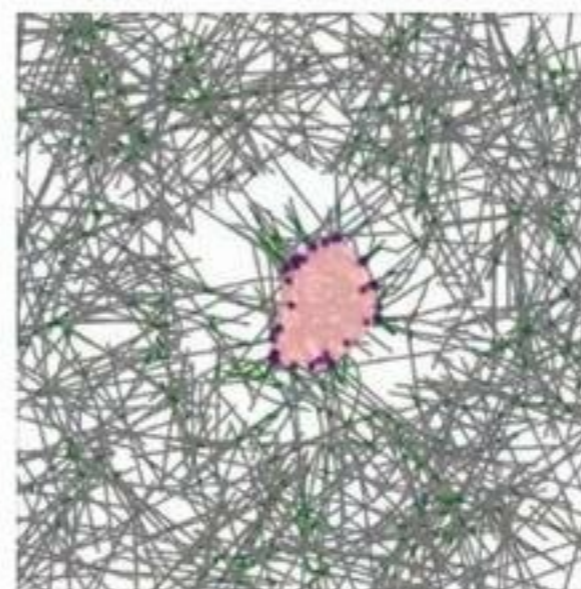
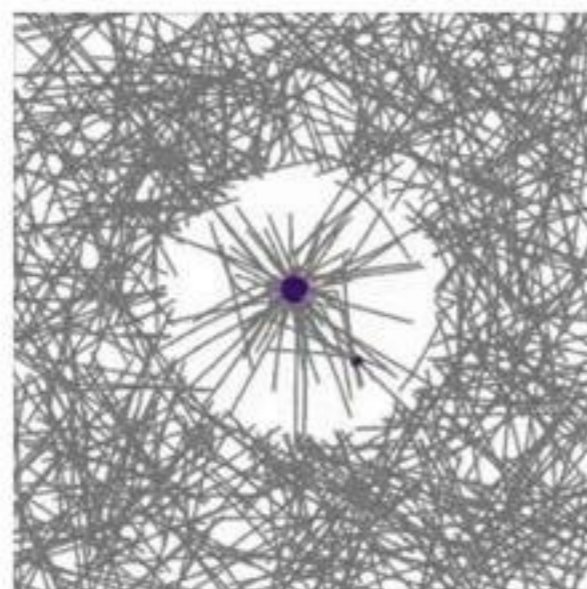
0.8 per μm^2

Fiber density:

~9.4 % v/v
~1.0 mg/ml
collagen [1]



~14.1 % v/v
~2.0 mg/ml
collagen [1]



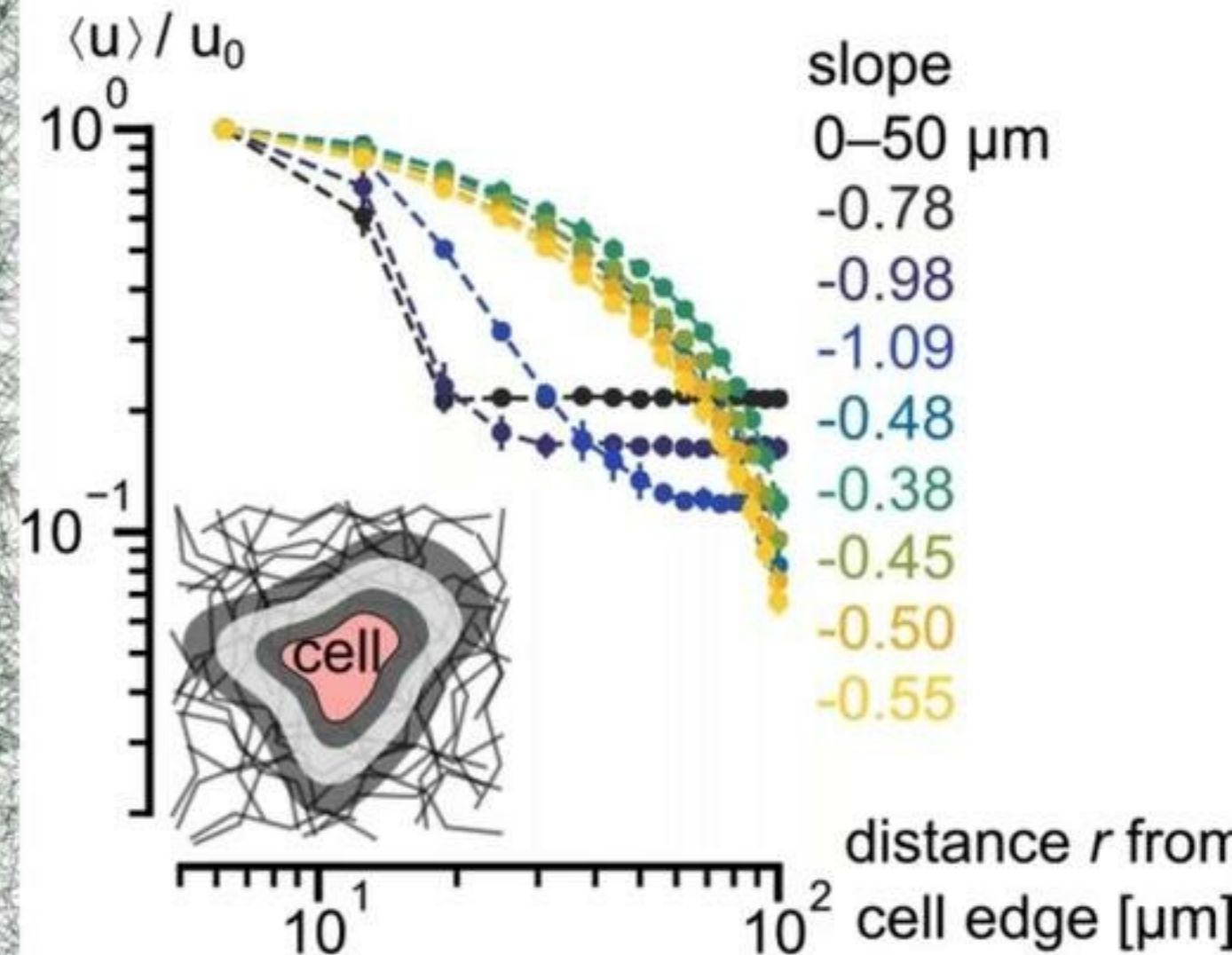
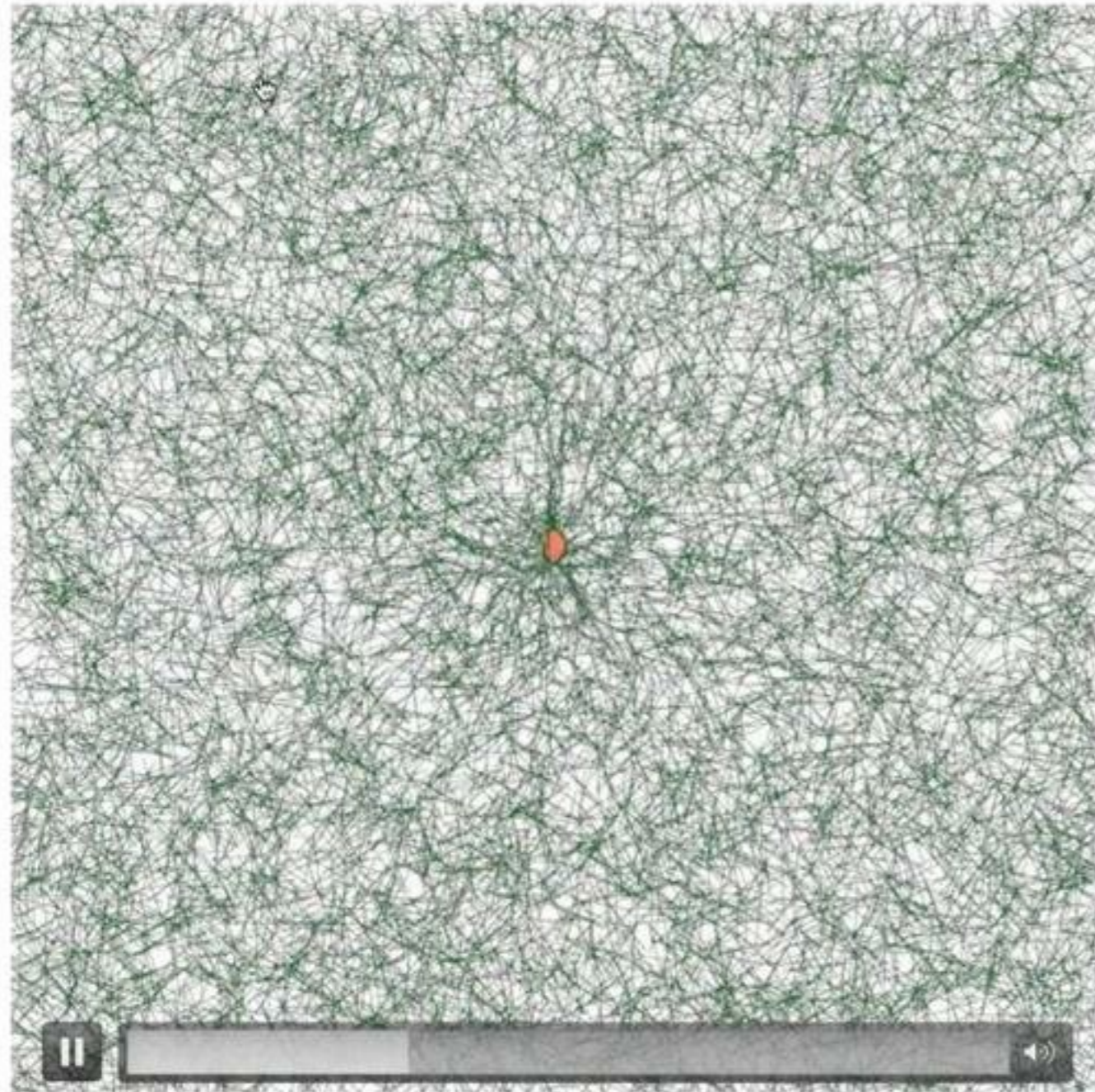
Assuming fiber diameter of $0.25 \mu\text{m}$ and length of $12.5 \mu\text{m}$; domain height = $1 \mu\text{m}$. [1] Kreger et al. Biopolymers 93.8 (2010): 690-707.

Erika Tsingos, Bente Hilde Bakker, Koen Keijzer, HJ Hupkes, RM, in revision, *bioRxiv*, 2022



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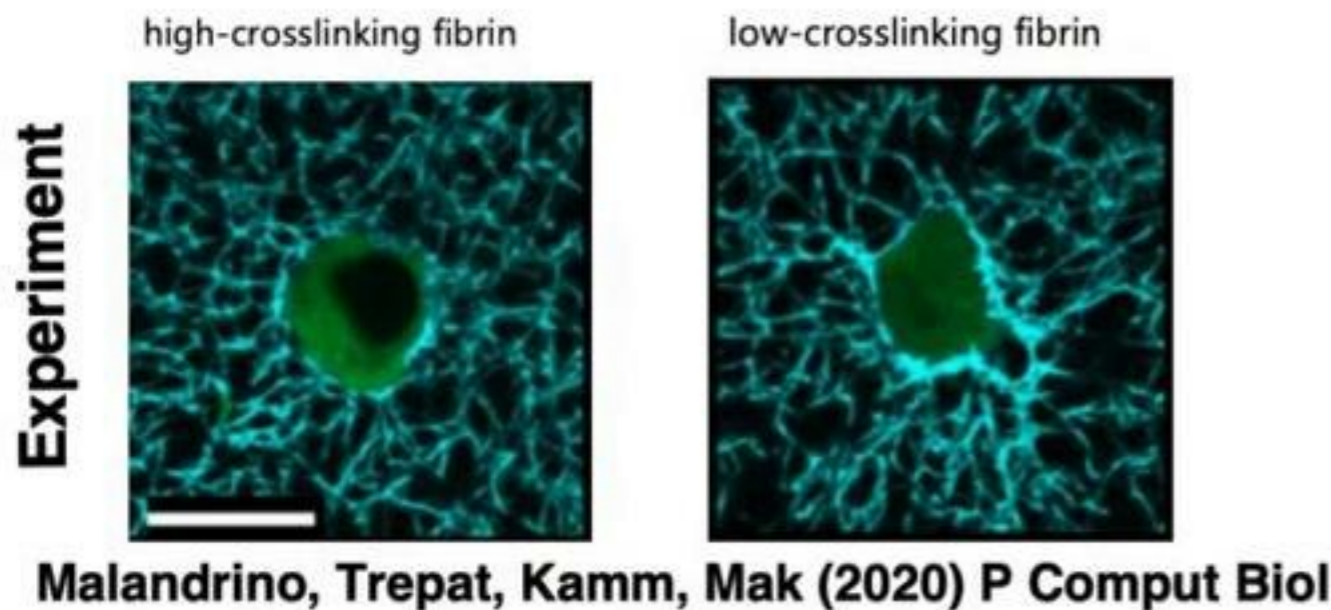
Cells remodel matrix up to 4 cell diameters away





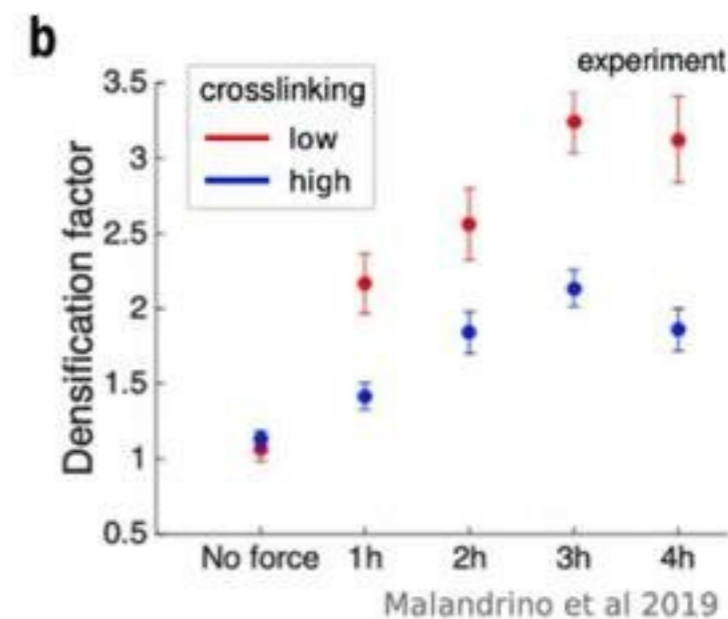
Contractile cells in fibrous extracellular matrices

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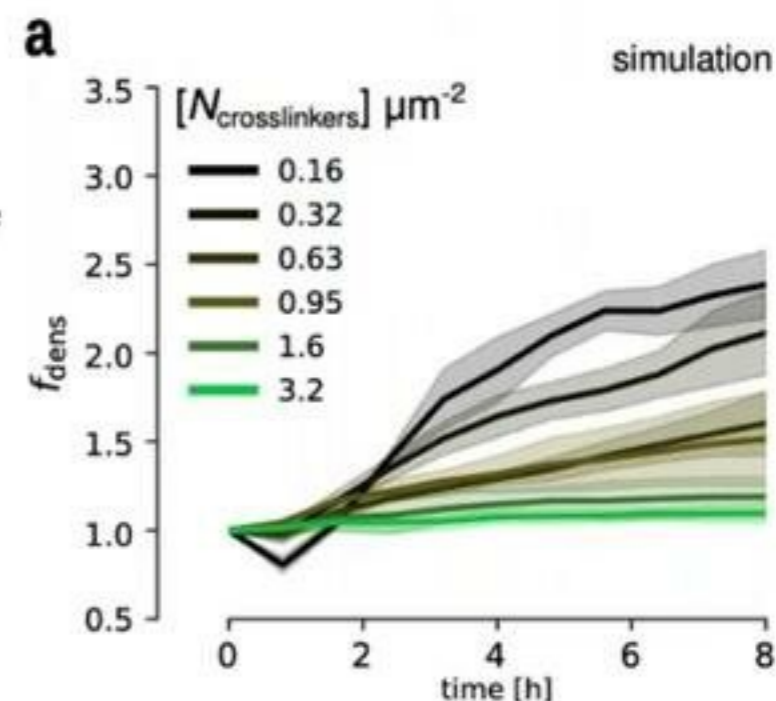
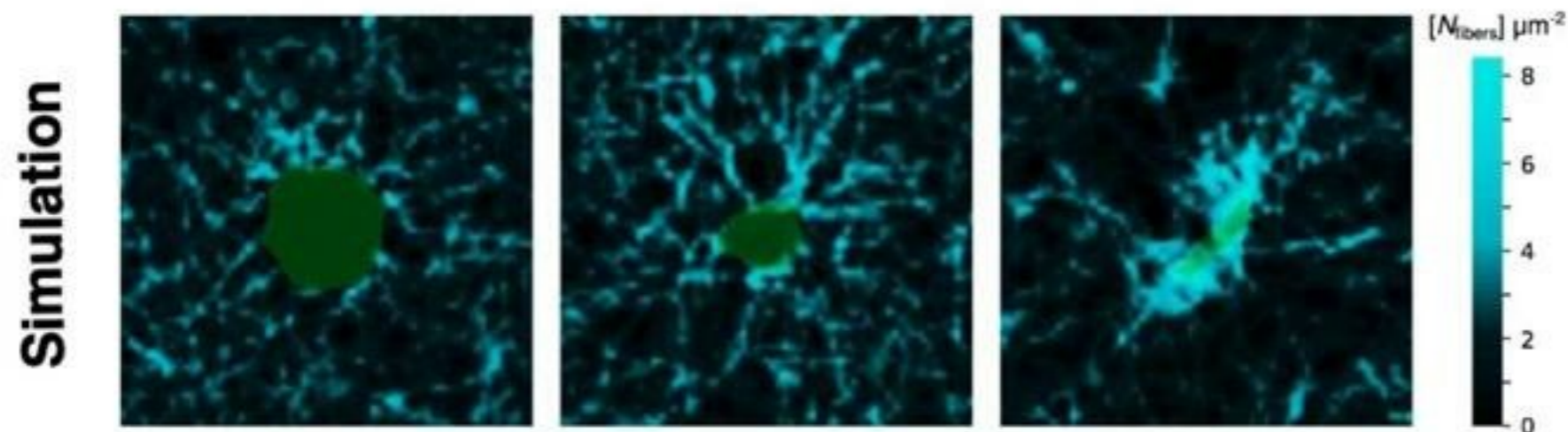


fiber densification:

$$f_{\text{dens}} = \frac{\langle \rho_{\text{near}} \rangle}{\langle \rho_{\text{far}} \rangle}$$



Time-averaged fiber density after ~8h simulated time

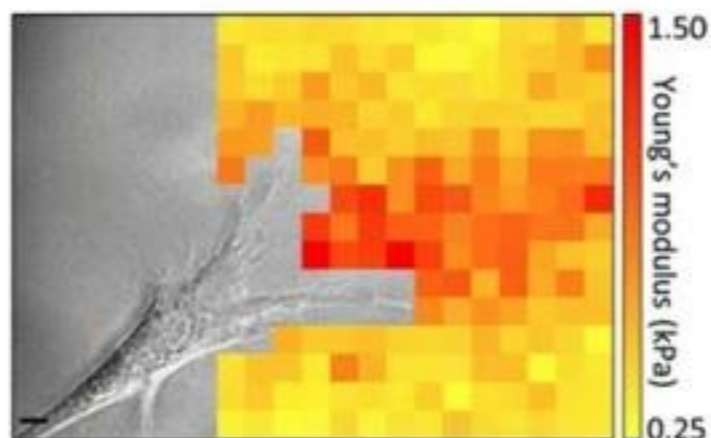
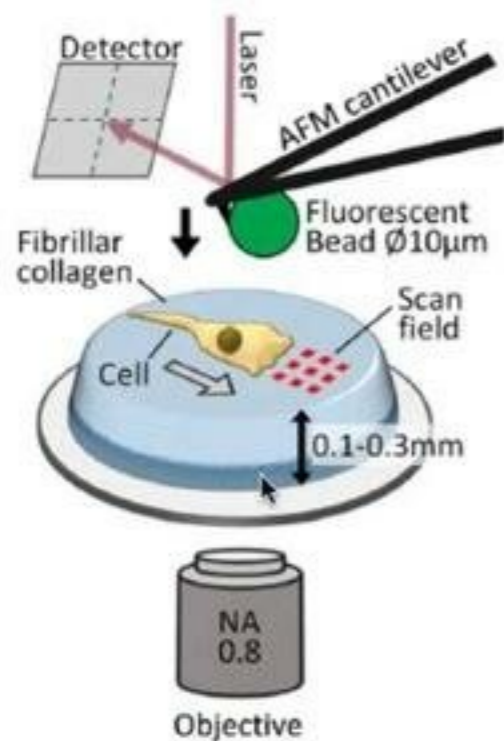




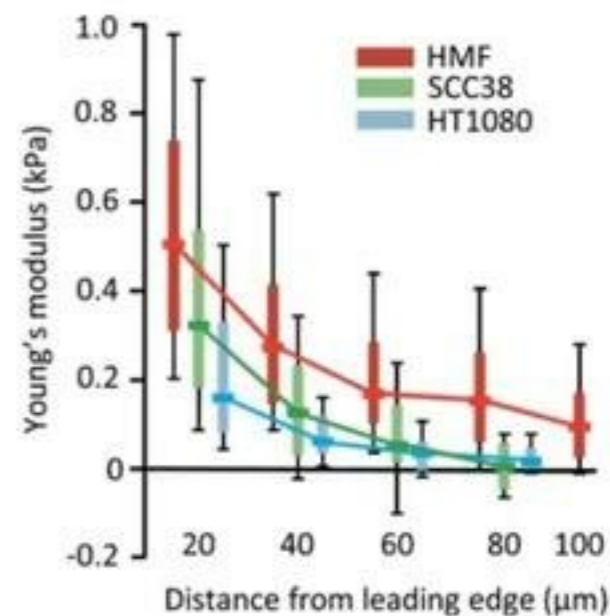
In silico atomic force microscopy

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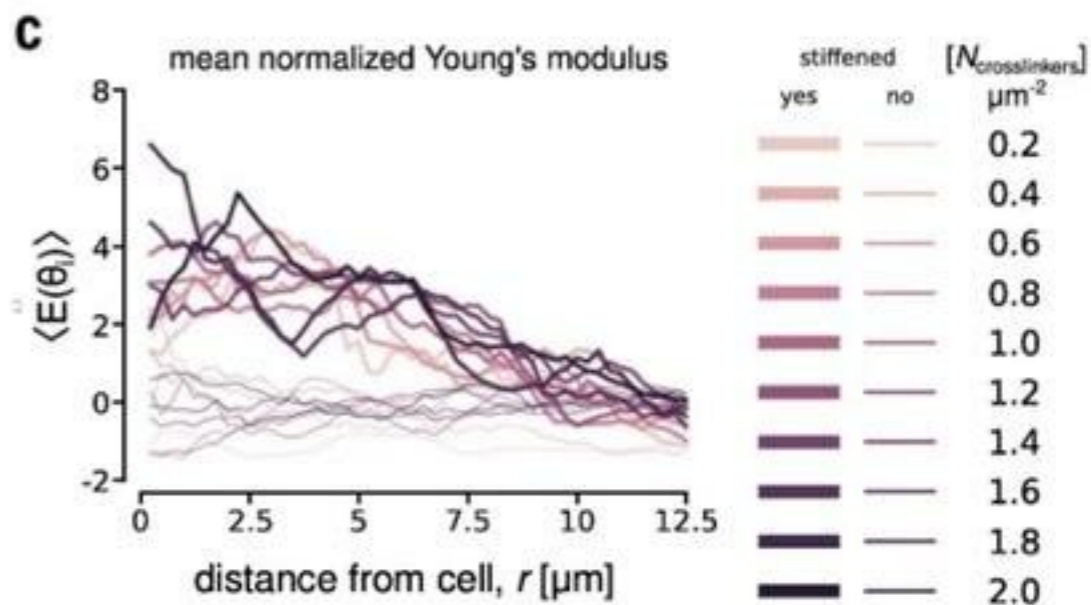
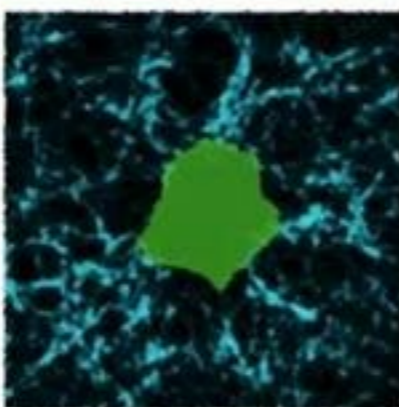
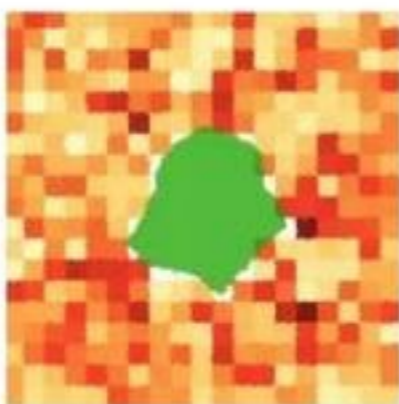
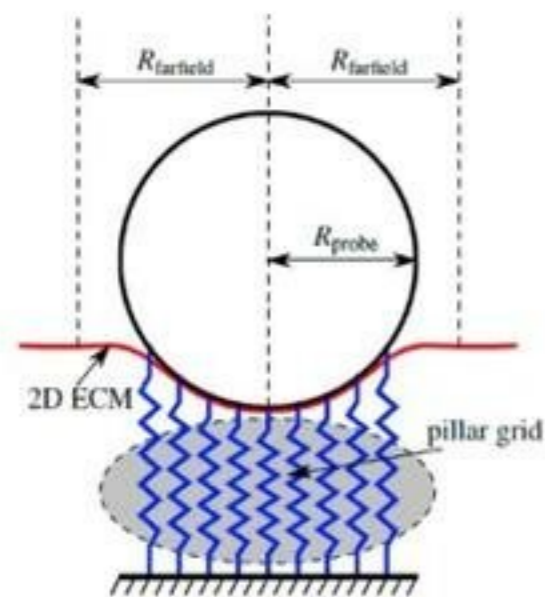
Experiment

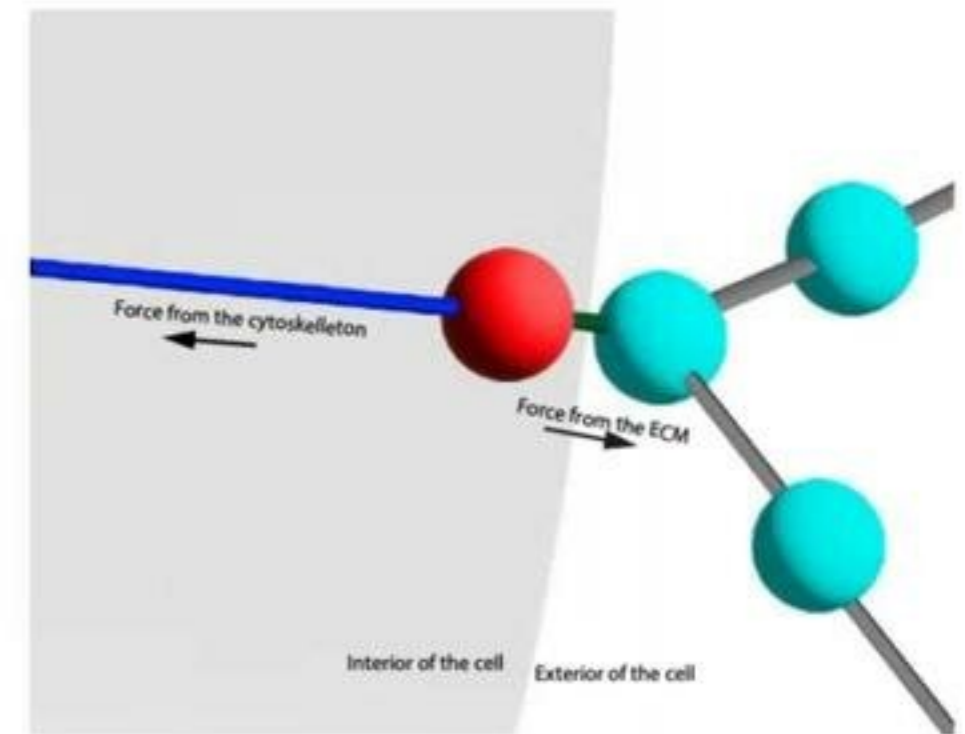
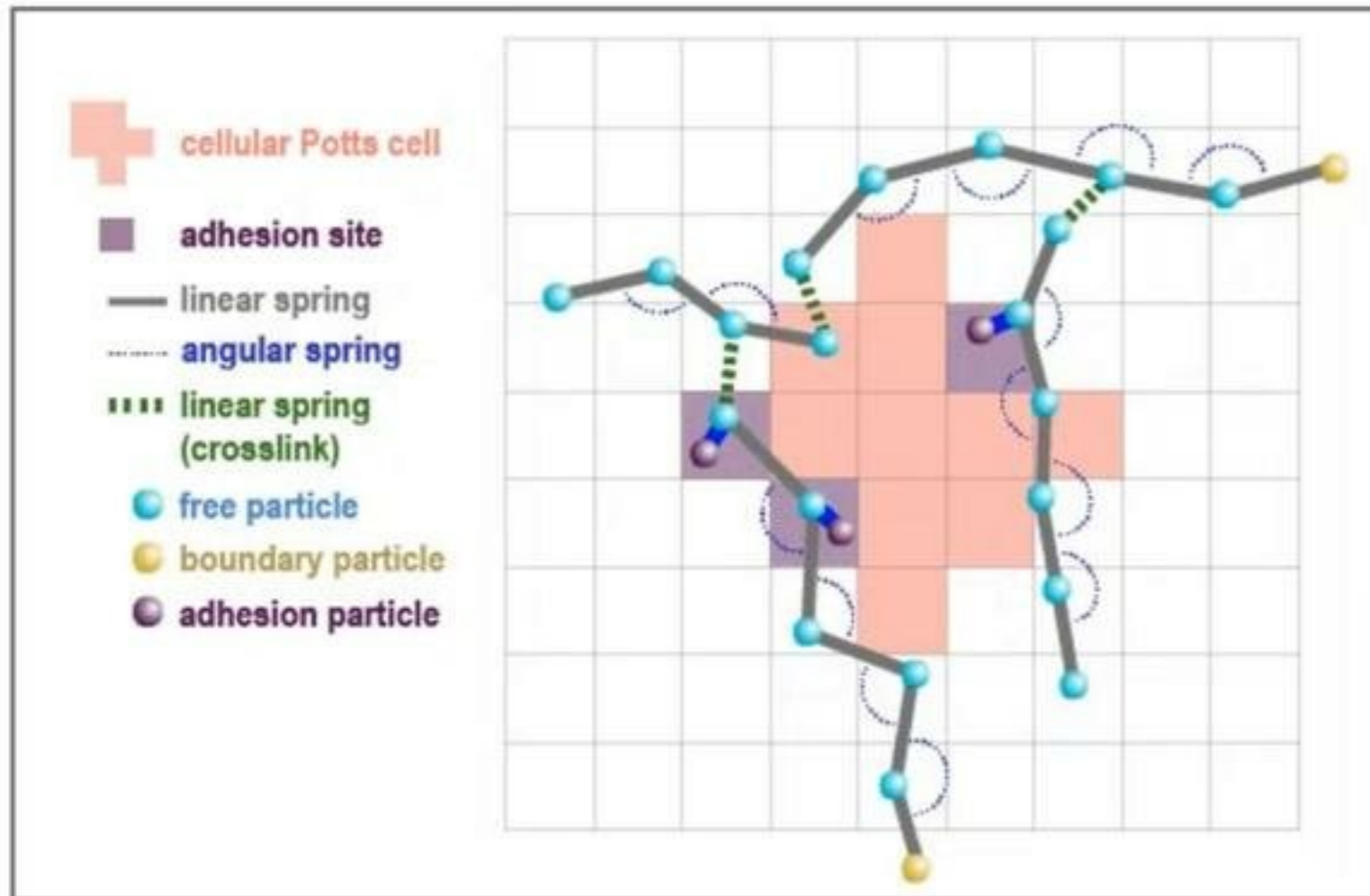


Van Helvert ... Friedl et al. (2016)
ACS Applied Materials & Interfaces



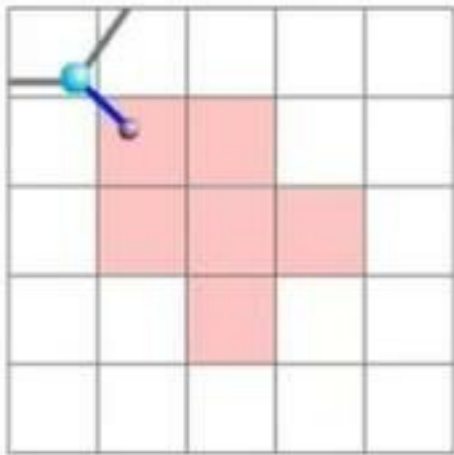
Simulation



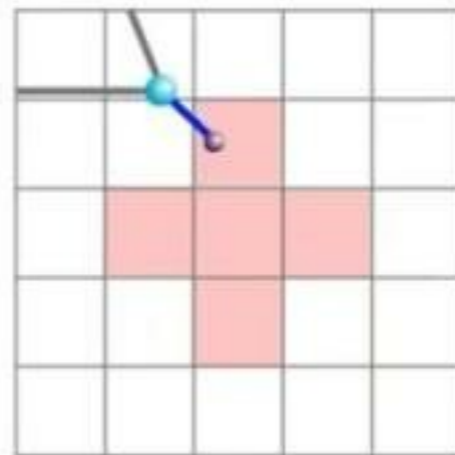




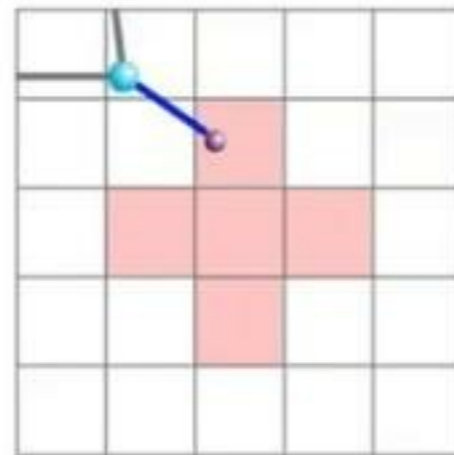
Cell movement is coupled to ECM at adhesions



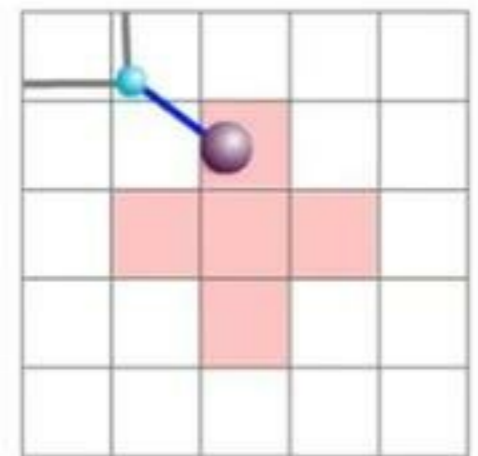
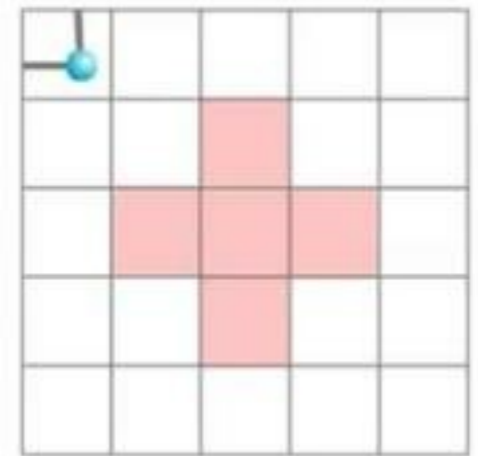
If part of the cell moves some ECM is taken with it



Tension between the cell and the ECM is measured (blue spring)



Based on tension and adhesions size the focal adhesion yields or grows

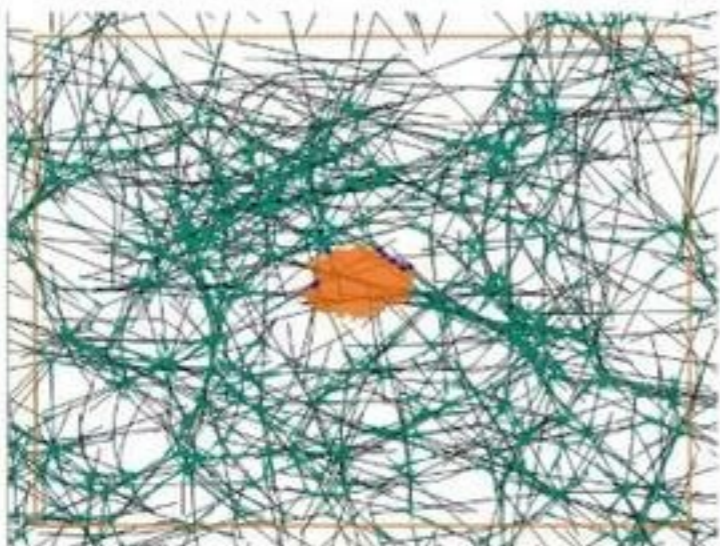
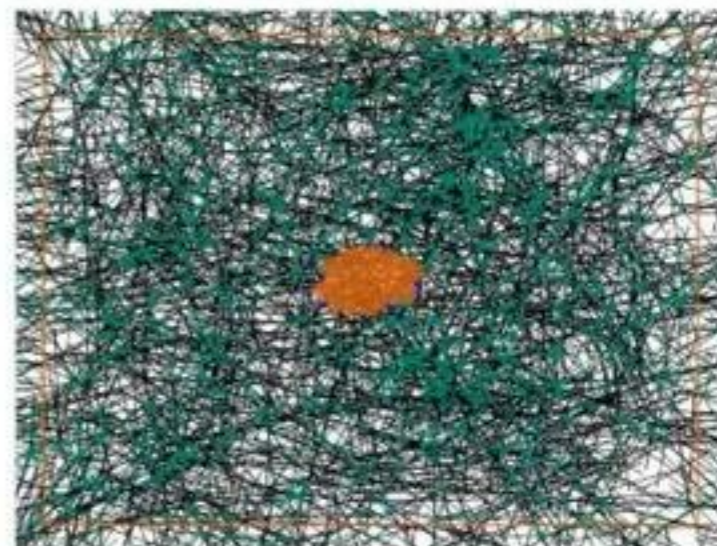
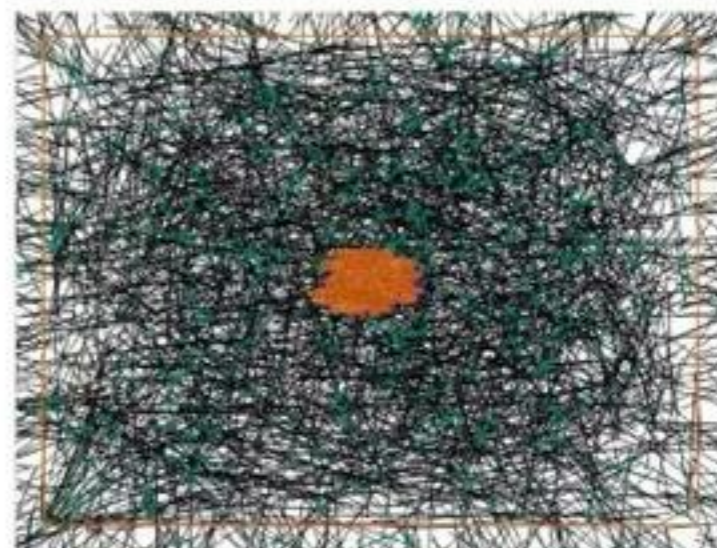
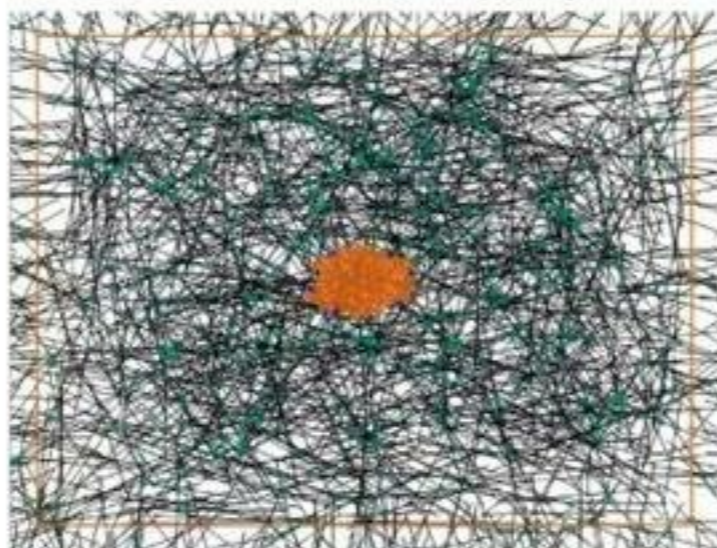
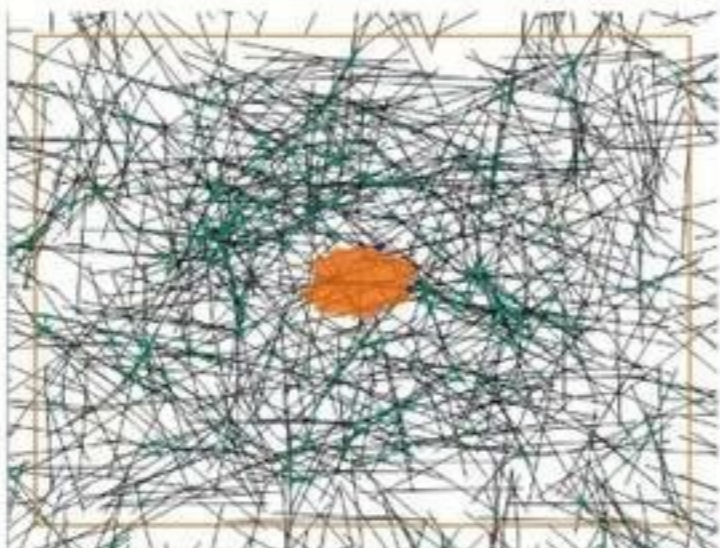




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Cross-linker Density

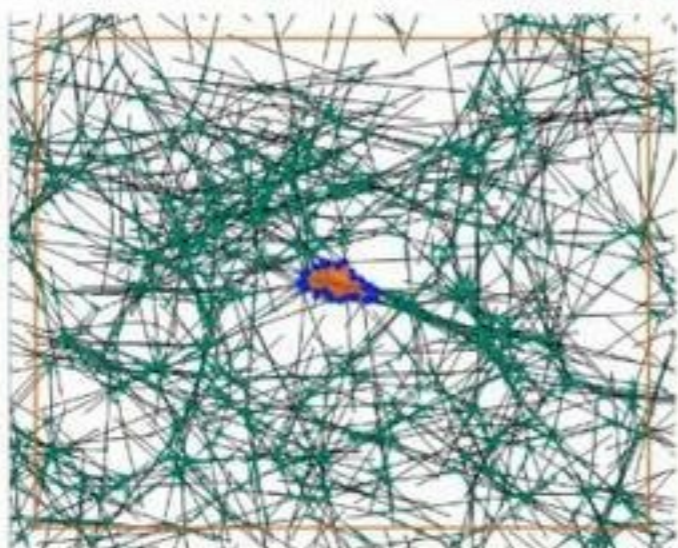
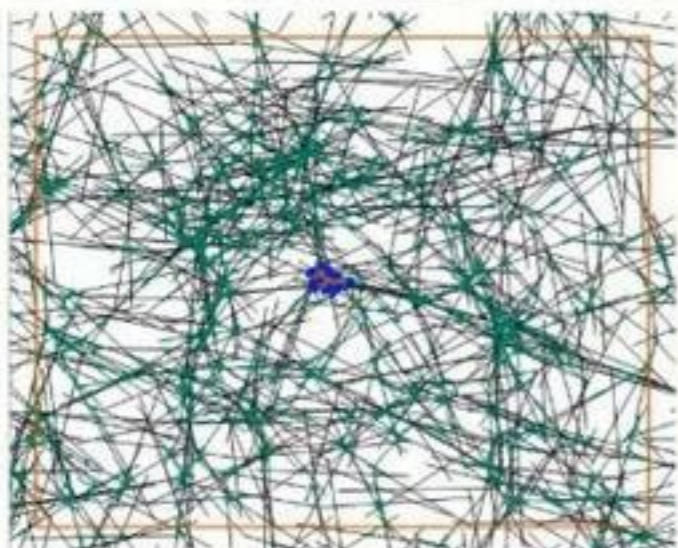
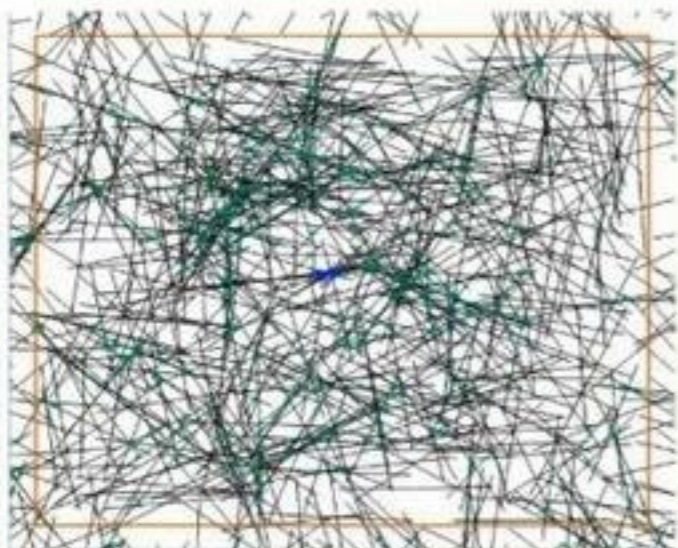
ECM Density



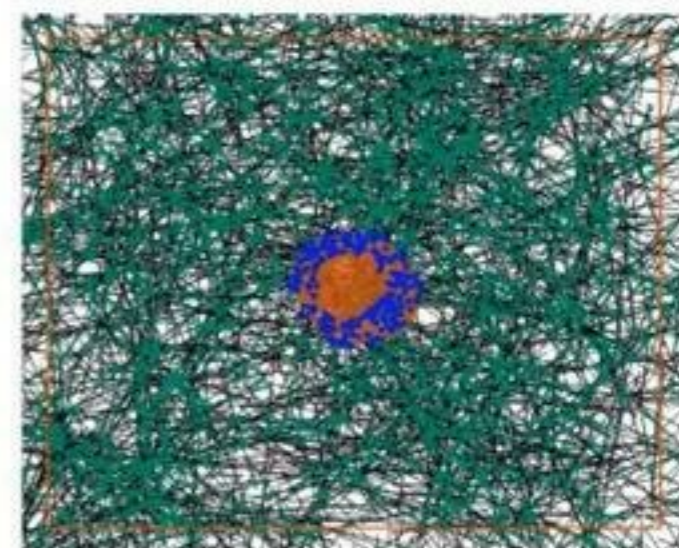
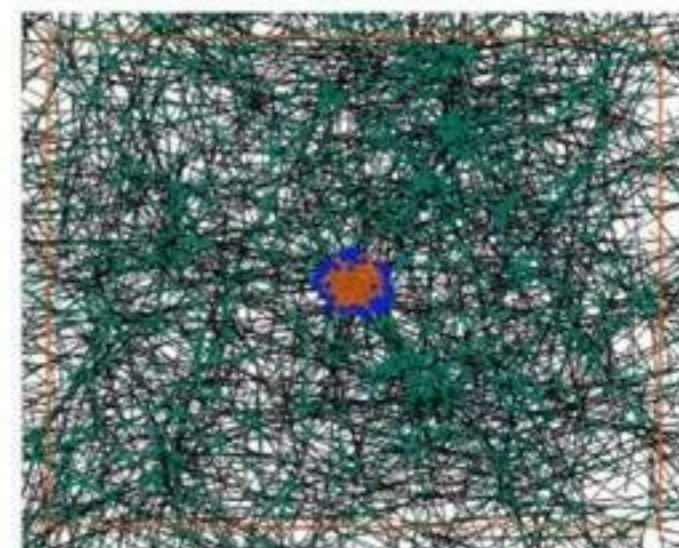
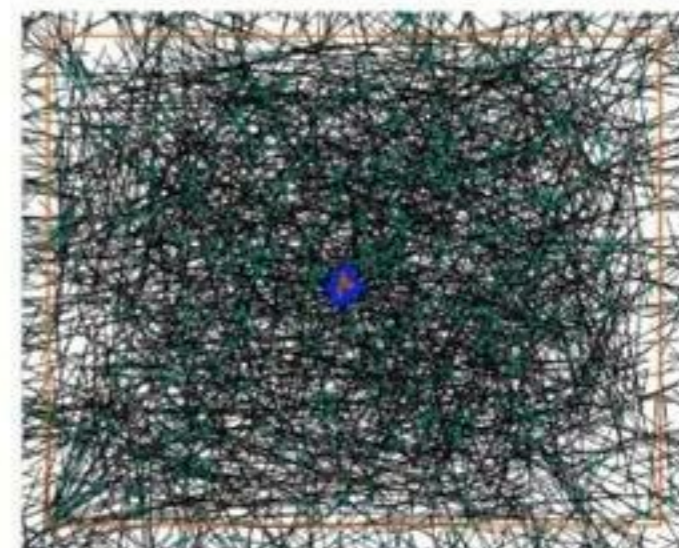
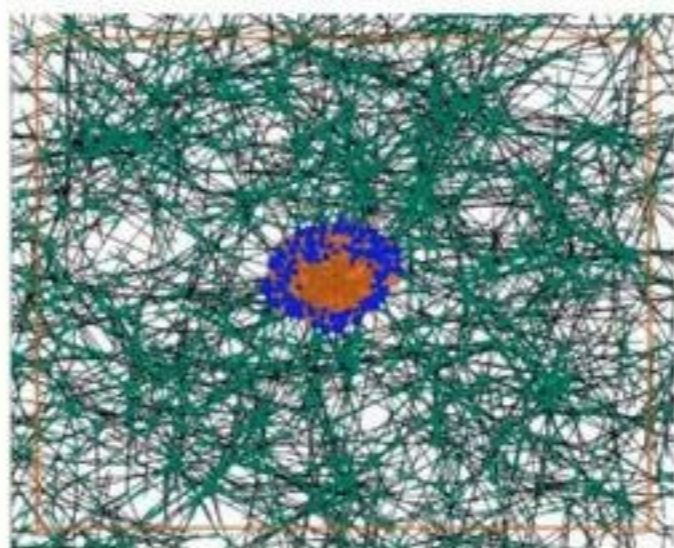
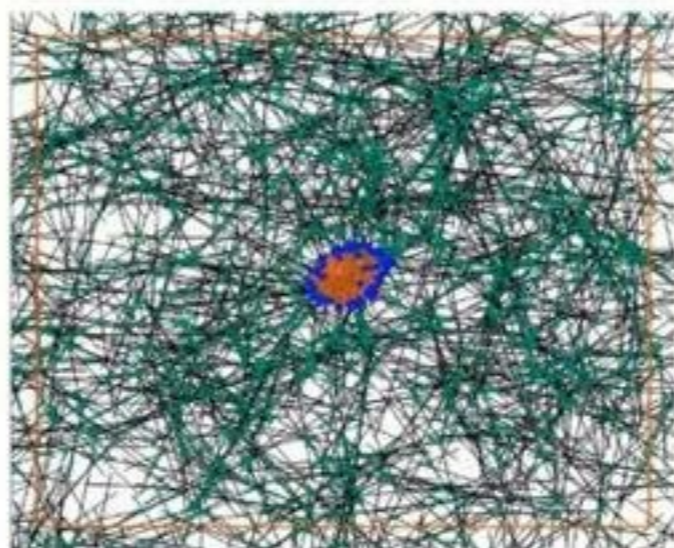
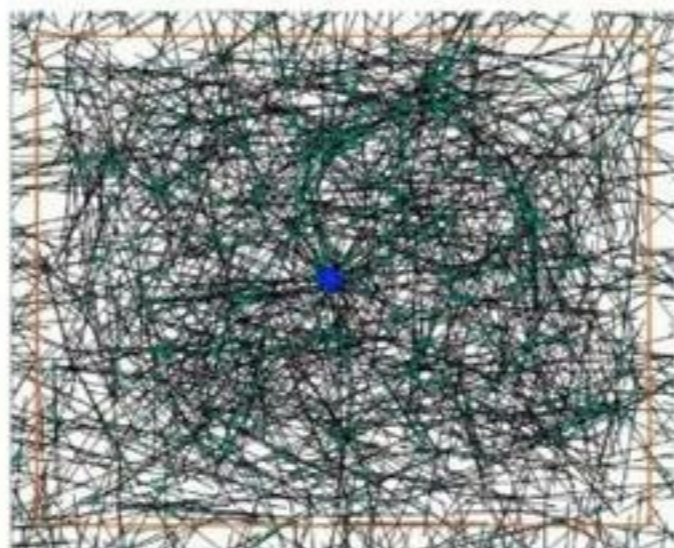


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Cross-linker Density



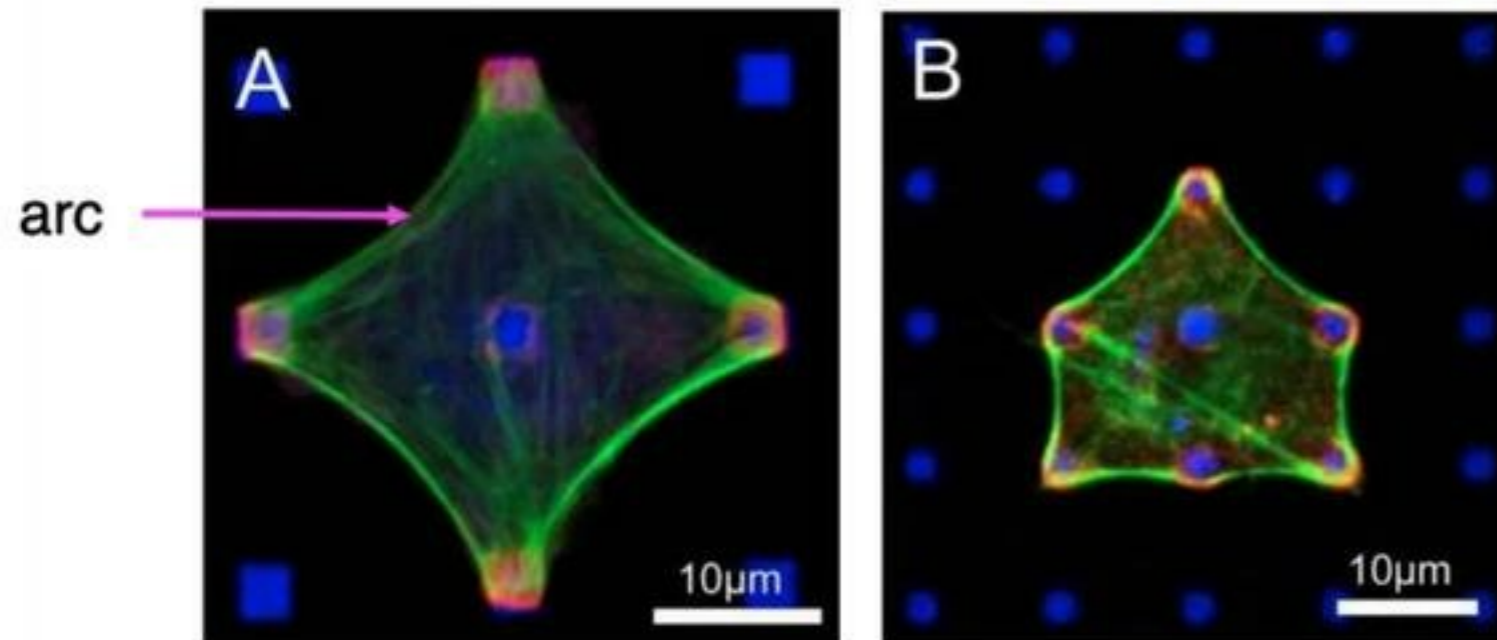
ECM Density



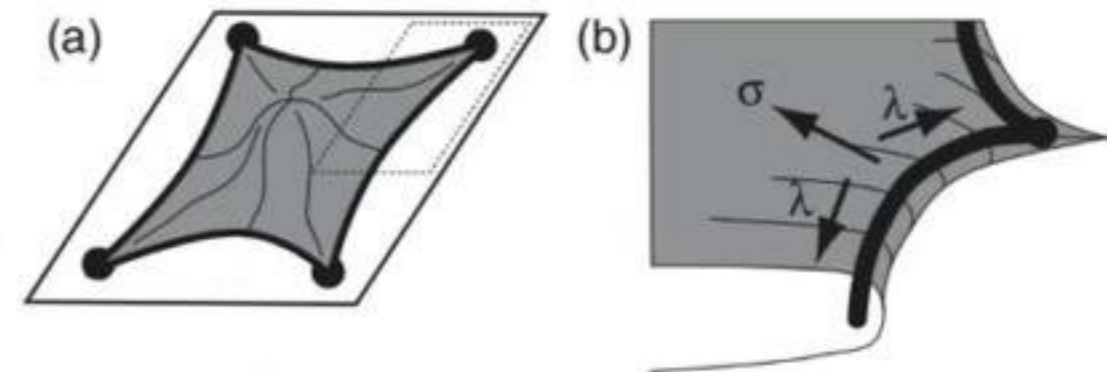


Effect cytoskeletal contractility on cell shape

- Cells adhering on patterned substrates



Bischofs et al. Biophys J 2008



Bischofs et al. PRL 2009

- What is the shape of the free hanging 'arcs'?



Cross-talk between cell shape and cytoskeletal organization

- **Approach:** let a coarse-grained model of the actin cytoskeleton control the CPM and *vice versa*

- Q-tensor describes actin orientation at each location

$$\hat{Q} = \begin{bmatrix} Q_{xx} & Q_{xy} \\ Q_{xy} & -Q_{xx} \end{bmatrix} = \frac{S}{2} \begin{bmatrix} \cos 2\theta_{SF} & \sin 2\theta_{SF} \\ \sin 2\theta_{SF} & -\cos 2\theta_{SF} \end{bmatrix}$$

- With $S = \sqrt{2 \text{tr} Q^2}$, the nematic order parameter (S=0 isotropic, S=1 fully aligned)

- Dynamics:

- tendency of actin fibers to **align with one another (K)** versus **alignment of fibers with cell boundary (W)**





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From **isotropy** to **anisotropy**

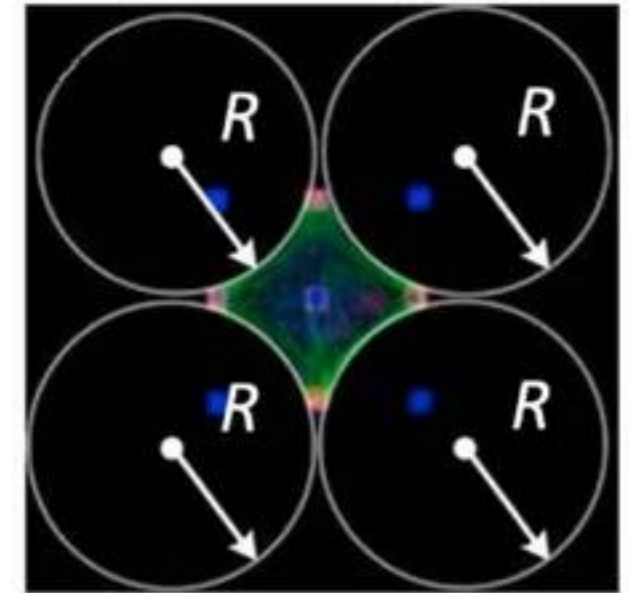
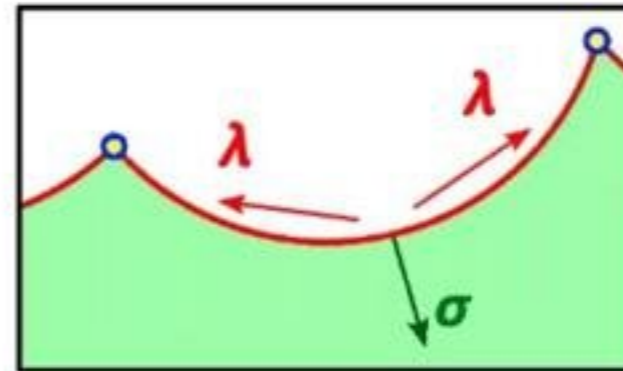
Is the model of
intracellular contractility correct?



Isotropic contraction: circular arcs

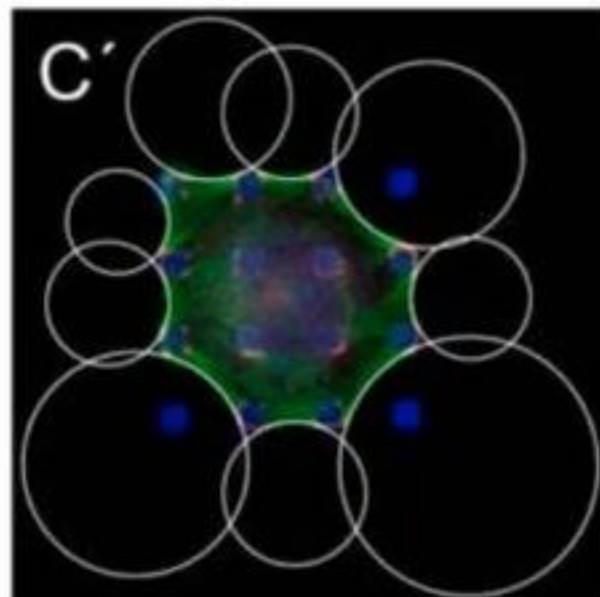
- Young-Laplace law predicts circular arcs
(Bar-Ziv et al. PNAS 1999)

- Minimize $H = \sigma A + \int \lambda(s) ds$
- Gives $R = \lambda/\sigma$

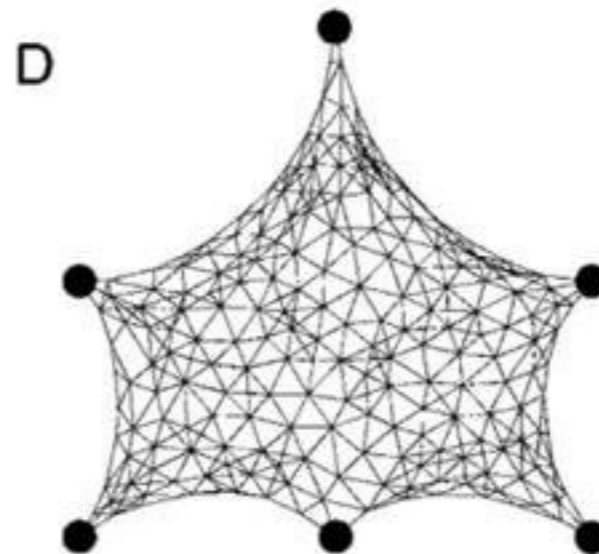


Bischofs et al. Biophys J 2008

- Cell bulk is elastic and cortex contracts actively:
 - Curvature depends on distance between adhesion points
(Bischofs et al. Biophys J 2008)



Bischofs et al. Biophys J 2008



$$R = l_c \left(\frac{2R}{\alpha d} \arcsin \left(\frac{d}{2R} \right) - 1 \right).$$



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Isotropic cell contraction in the CPM



Koen Schakenraad

- Cortex is elastic and cortex and cell bulk contract actively:

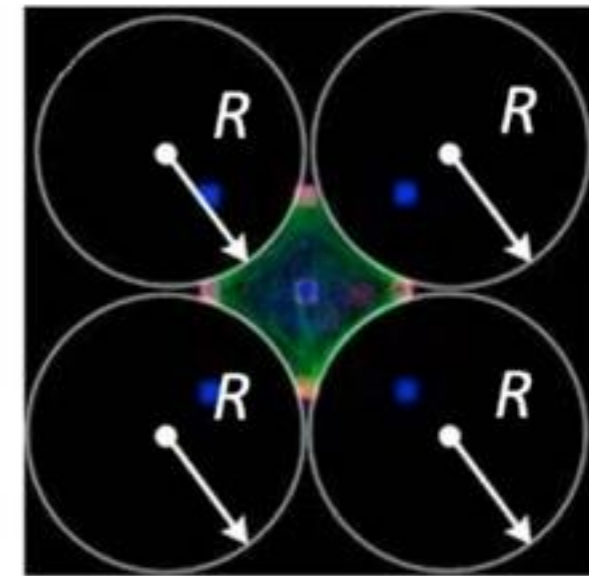
$$H = \sigma A + \lambda P - \frac{E_0}{A_{\text{ref}} + A_{\text{ad}}} A_{\text{ad}}$$

H = contraction + line tension - adhesion to patterned substrate

- Prediction:

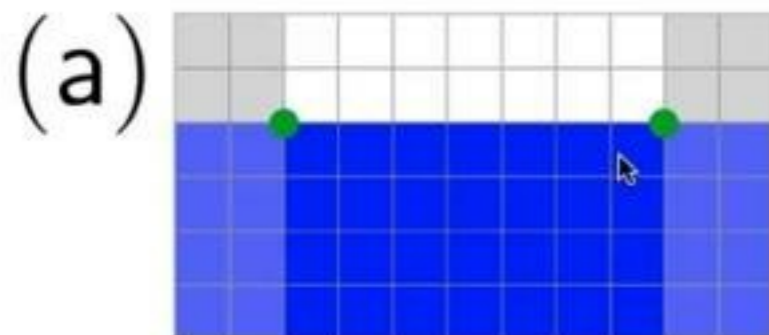
- Young-Laplace law: circular arcs between adhesion sites

$$R = \lambda / \sigma \quad \lambda = 500$$

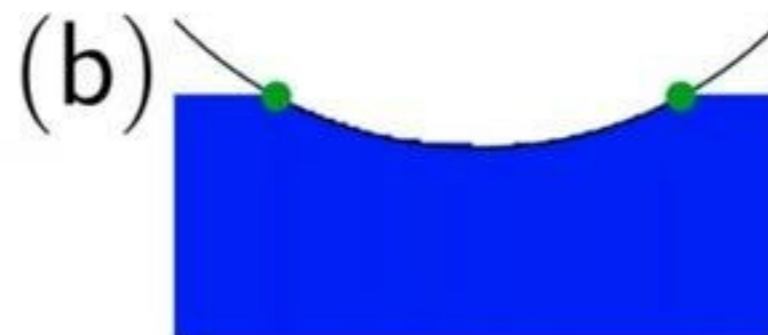


Bischofs et al. Biophys J 2008

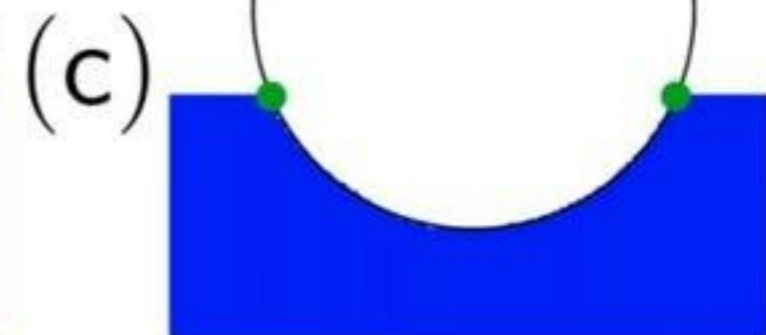
CPM predictions for isotropic cells match Young-Laplace law



Initial configuration



$\sigma = 10, R = 50, R_{\text{CPM}} = 54$



$\sigma = 5, R = 100, R_{\text{CPM}} = 105$

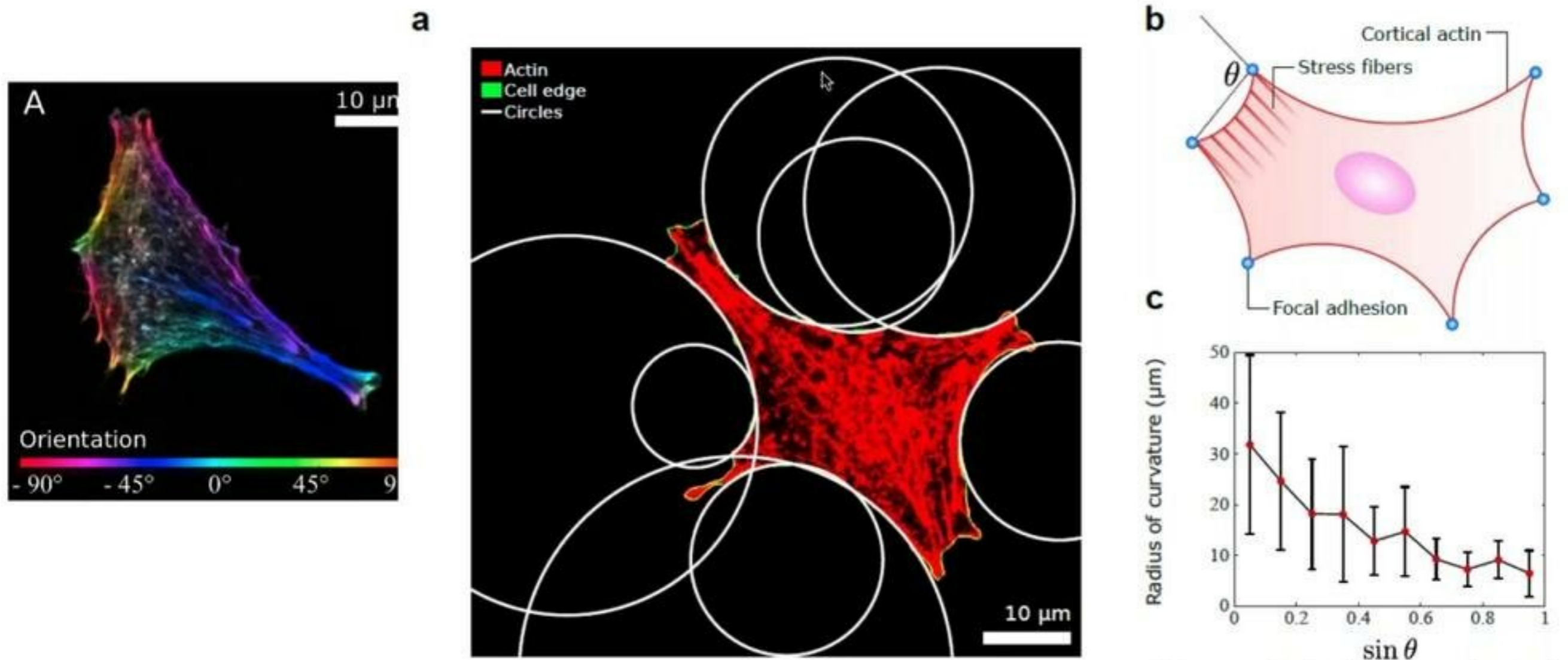
Schakenraad, Martorana, Bakker, Giomi, RM, in revision
bioRxiv, <https://doi.org/10.1101/2022.04.18.488715>



Anisotropic contraction

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- Curvature of cell edge depends on angle θ between stress fibers and lines connecting adhesion points



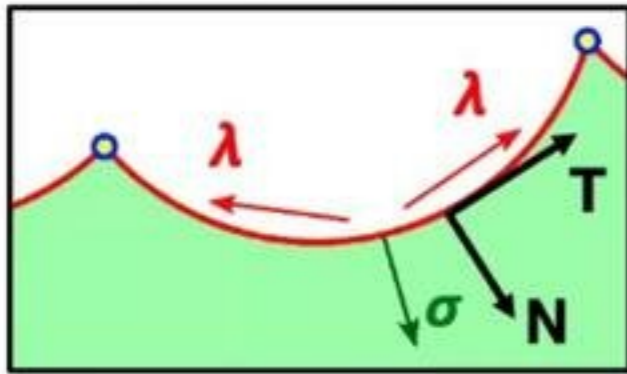
Pomp, Schakenraad et al.
Phys Rev Lett 2018



Anisotropic contraction: elliptic arcs

Isotropic case

$$\frac{d\lambda}{ds} \mathbf{T} + (\lambda\kappa + \sigma) \mathbf{N} = \mathbf{0}$$

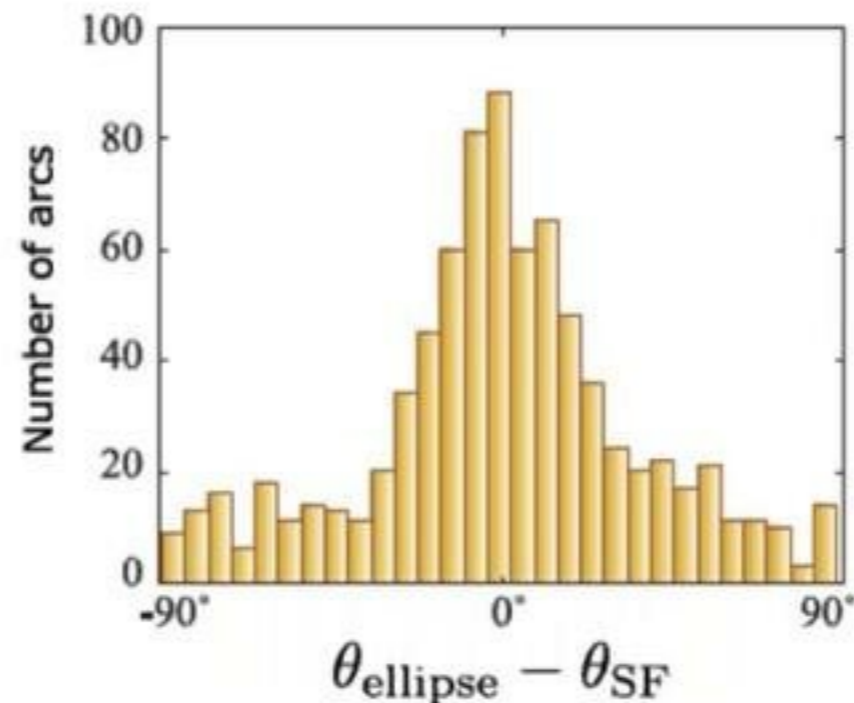
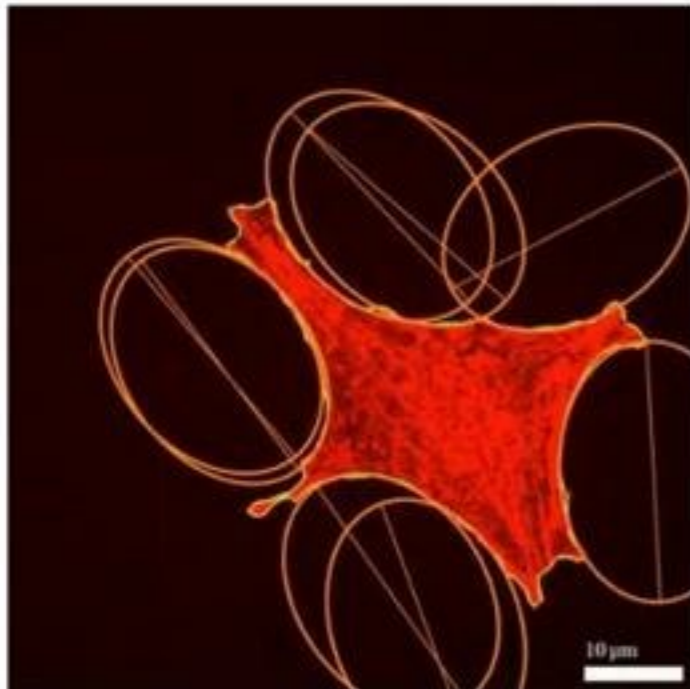
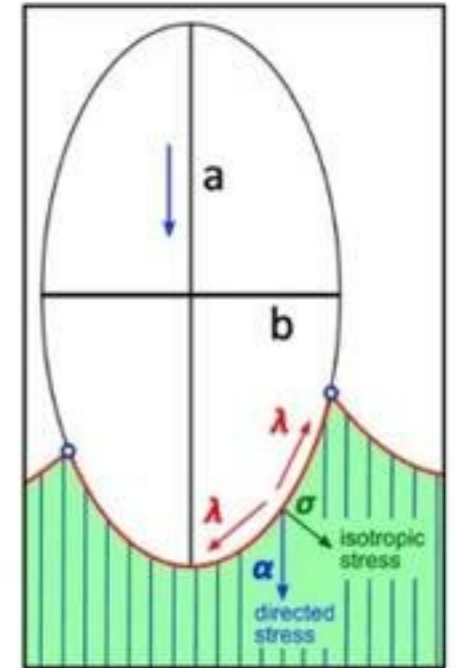


Anisotropic case

$$\frac{d\lambda}{ds} \mathbf{T} + (\lambda\kappa + \sigma) \mathbf{N} + \alpha(\mathbf{n} \cdot \mathbf{N}) \mathbf{n} = \mathbf{0}$$

- **Cell shape:** segment of an ellipse.
- **Long axis** aligns with stress fibers
- **Aspect ratio** given by ratio between isotropic (σ) and directed (α) forces

$$\frac{b^2}{a^2} = \frac{\sigma}{\sigma + \alpha}$$





Cross-talk between cell shape and cytoskeletal organization

- **Approach:** let a coarse-grained model of the actin cytoskeleton control the CPM and *vice versa*

- Q-tensor describes actin orientation at each location

$$\hat{Q} = \begin{bmatrix} Q_{xx} & Q_{xy} \\ Q_{xy} & -Q_{xx} \end{bmatrix} = \frac{S}{2} \begin{bmatrix} \cos 2\theta_{SF} & \sin 2\theta_{SF} \\ \sin 2\theta_{SF} & -\cos 2\theta_{SF} \end{bmatrix}$$

- With $S = \sqrt{2 \text{tr} Q^2}$, the nematic order parameter (S=0 isotropic, S=1 fully aligned)

- Dynamics:

- tendency of actin fibers to **align with one another (K)** versus **alignment of fibers with cell boundary (W)**





Anisotropic cell forces in the CPM

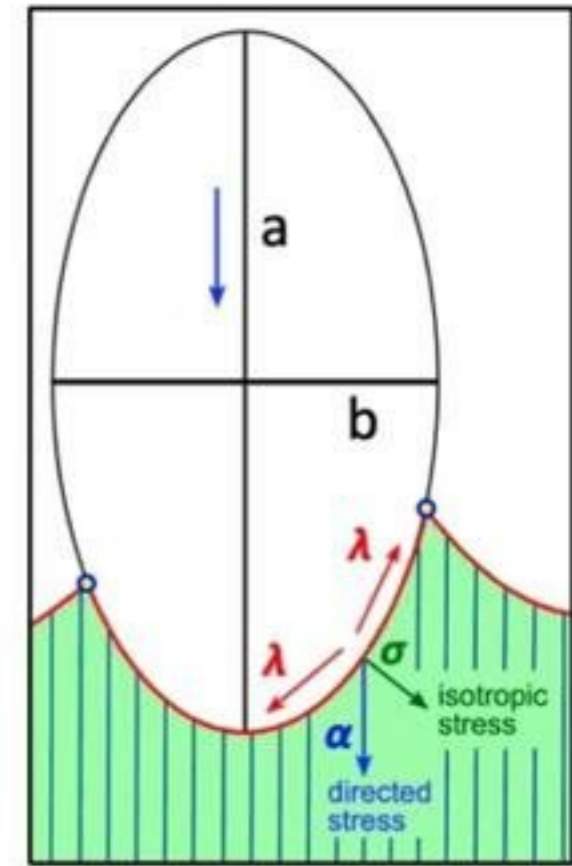
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$$\vec{f} = \frac{d\lambda}{ds} \mathbf{T} + (\lambda\kappa + \sigma)\vec{N} + \alpha S(\vec{n} \cdot \vec{N})\vec{n}$$

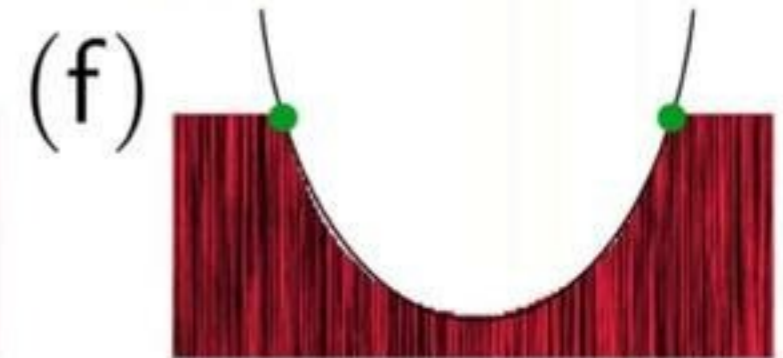
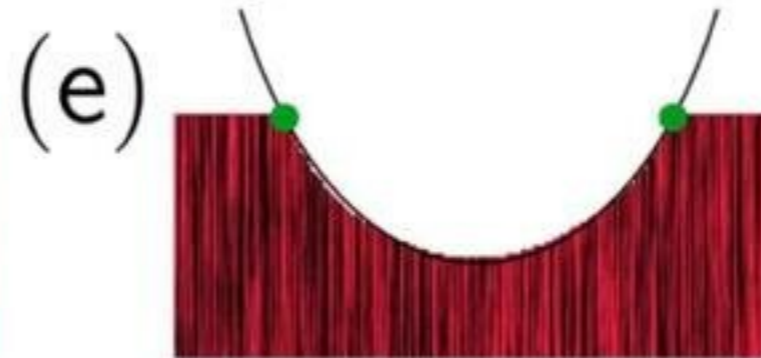
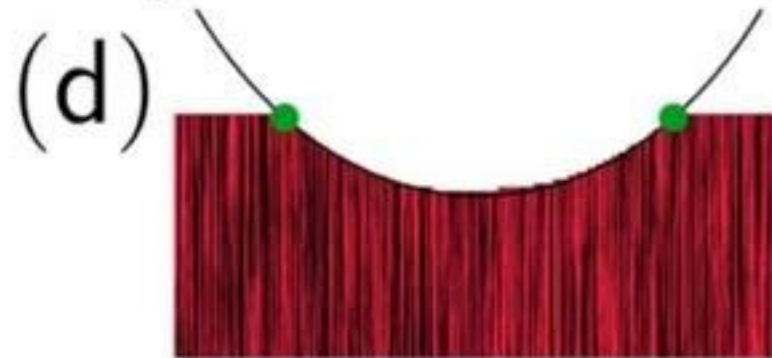
$$\Delta H = \lambda\Delta P + \sigma\Delta A + \Delta H_{\text{work}}$$

$$\Rightarrow \Delta H_{\text{work}} = \alpha S(\vec{n} \cdot \vec{N})^2 \Delta A$$

Additional force along actin fiber orientation



CPM predictions for isotropic cells:



Semi-major axis

Theory: 120 l.u.

120 l.u.

100 l.u.

Simulation: 134 l.u.

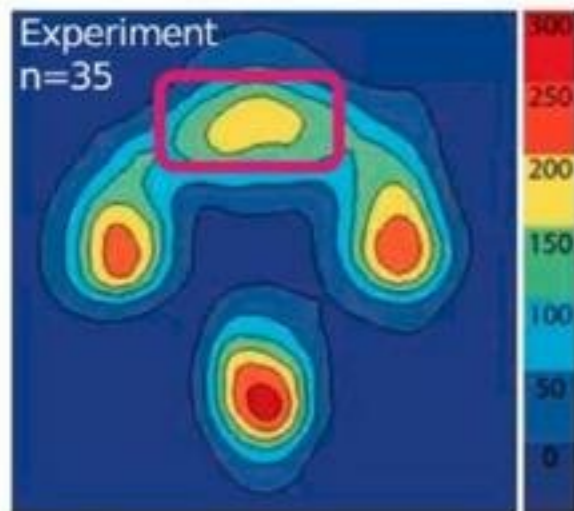
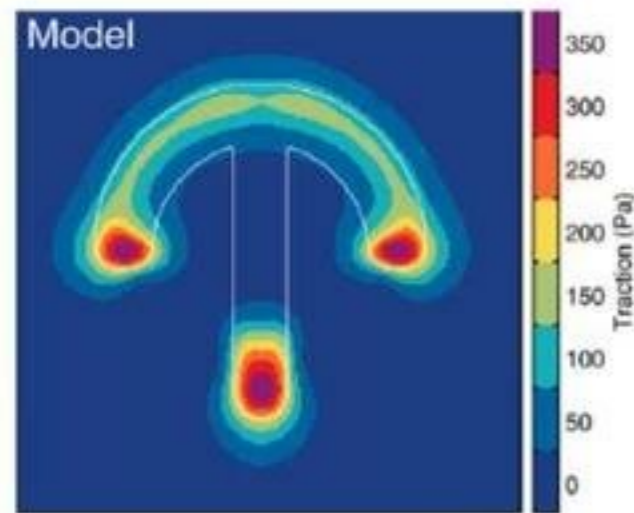
118 l.u.

98 l.u.



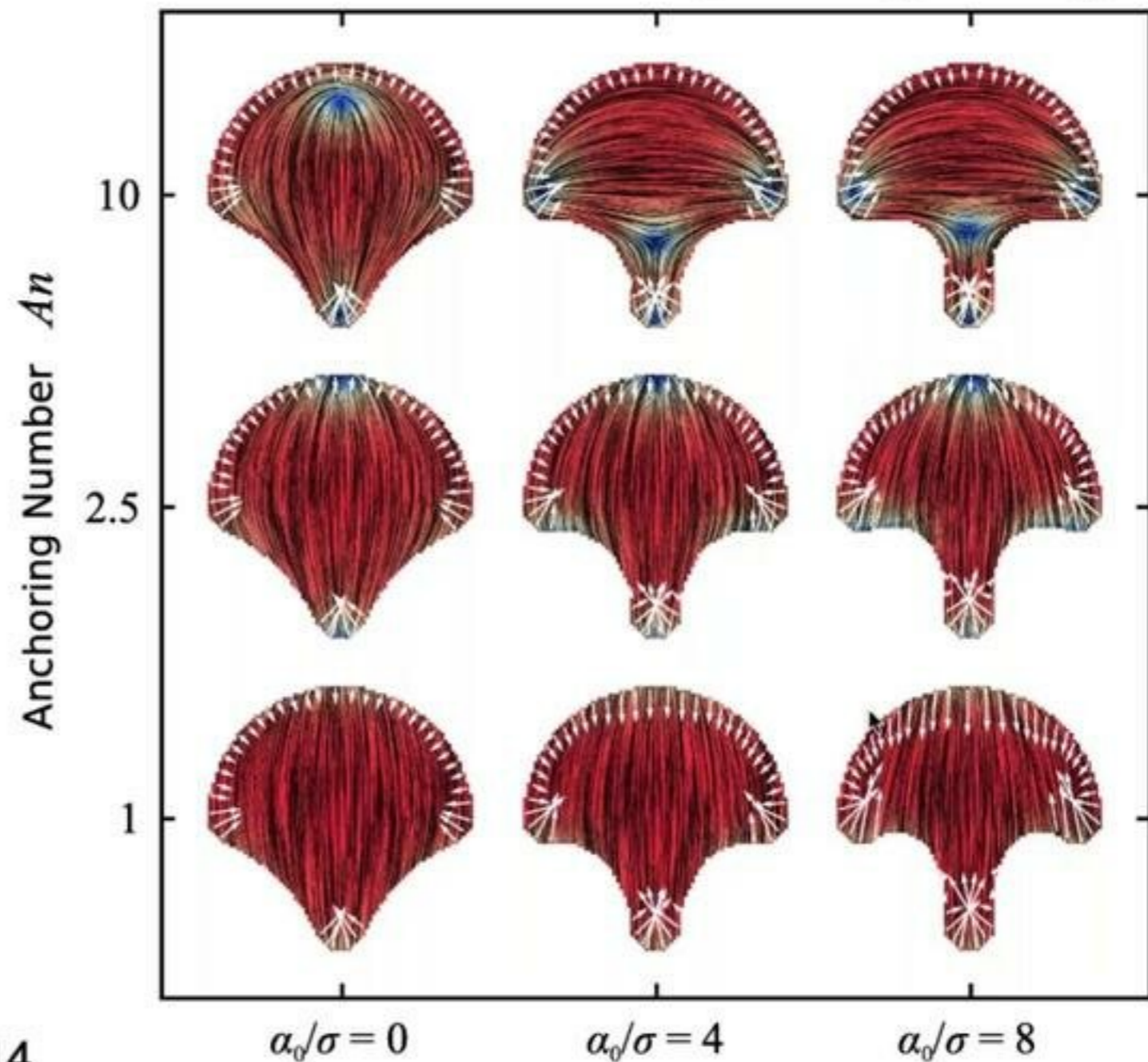
Anisotropic cell forces in the CPM

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Albert and Schwarz, Biophys J 2014

Order Parameter S

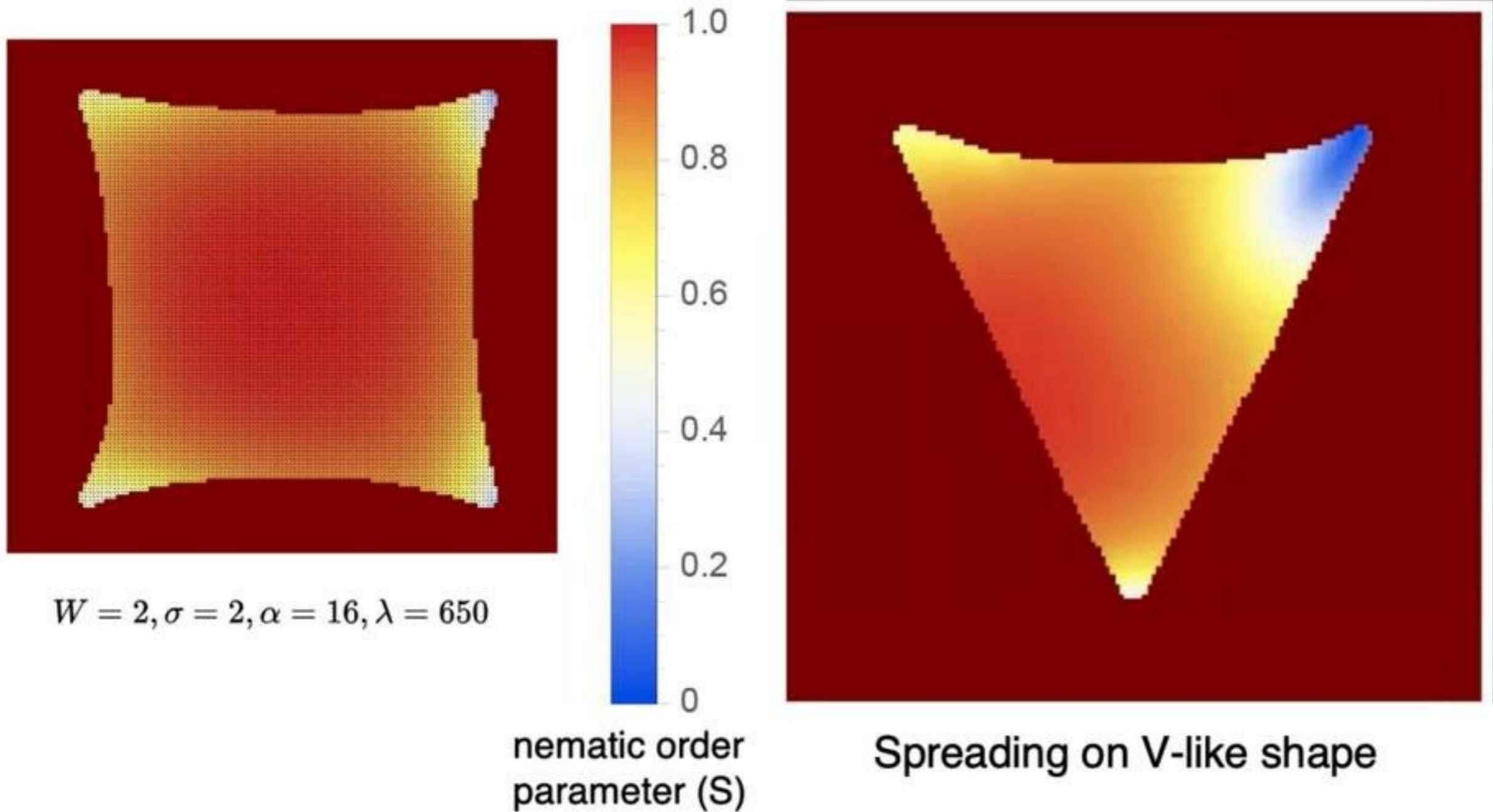


Schakenraad, Martorana, Bakker, Giomi, RM, in revision
bioRxiv, <https://doi.org/10.1101/2022.04.18.488715>



Cell and cytoskeleton cross-talk

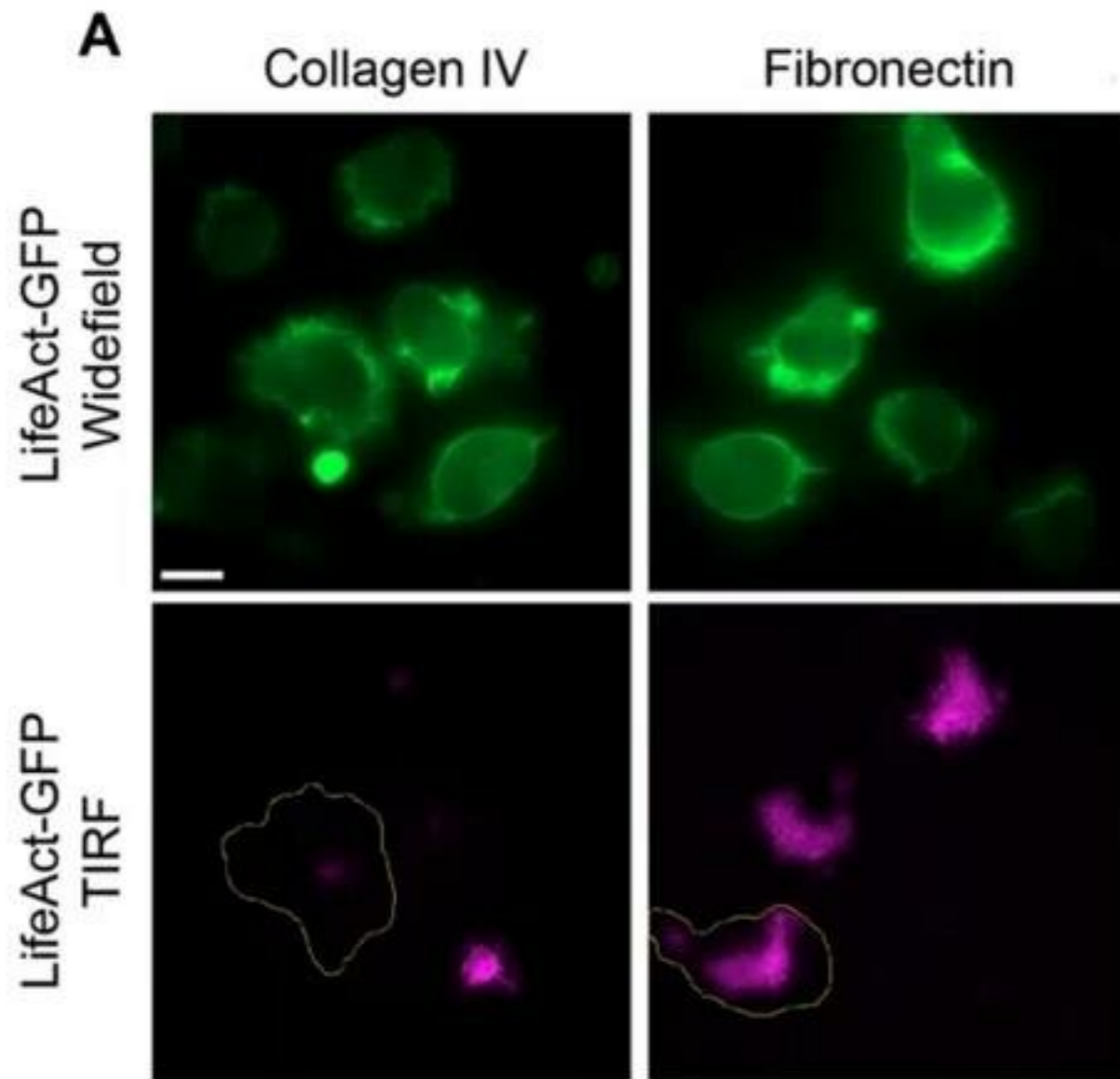
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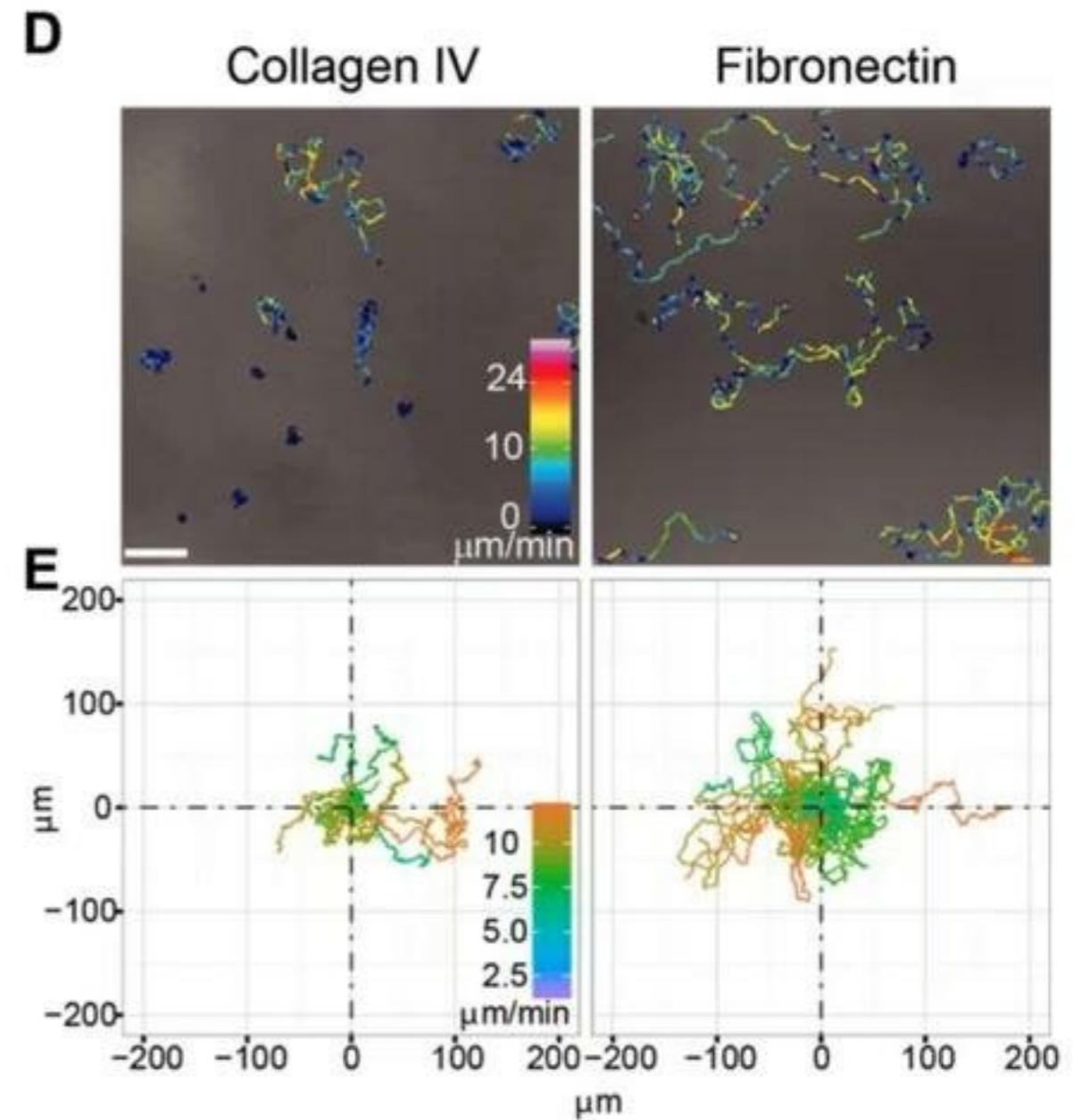


ECM affects B-cell migration

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B lymphocytes
(human JY cell line)



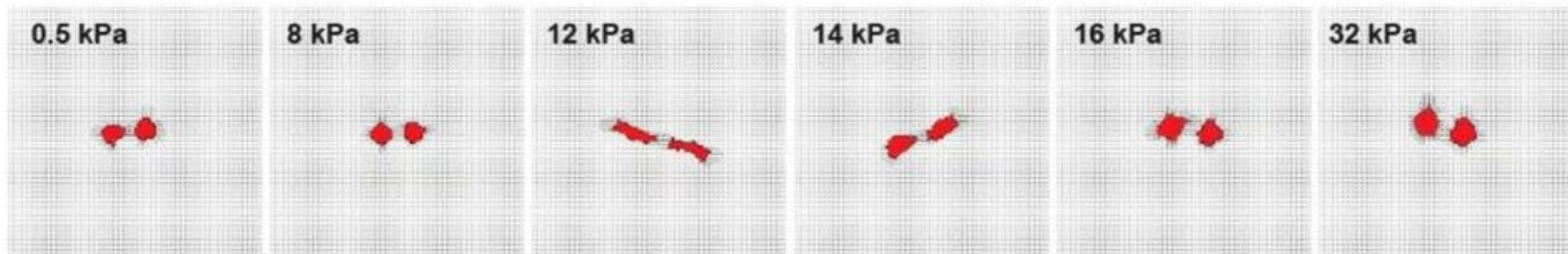
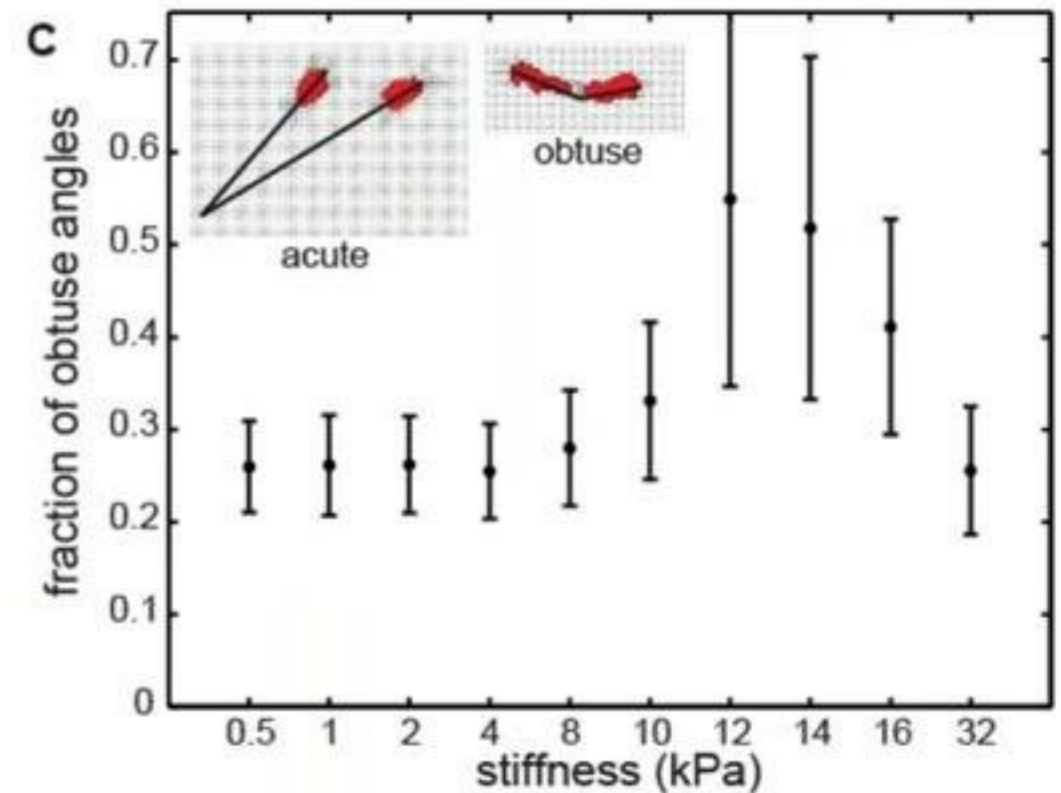


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Simplified model: Cell-substrate reciprocity partly explains stiffness-dependent cell-cell interactions

Video S2 - cell pairs

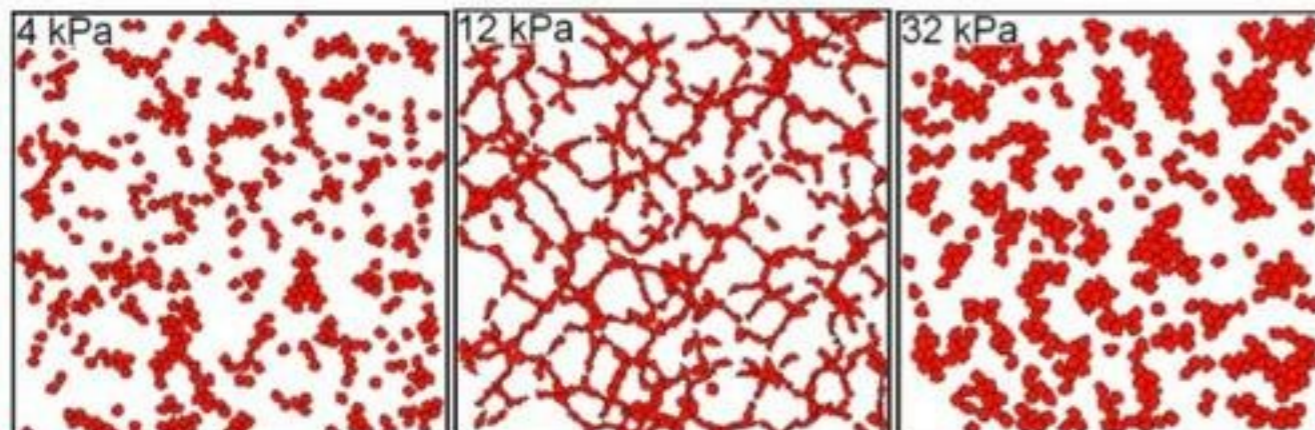
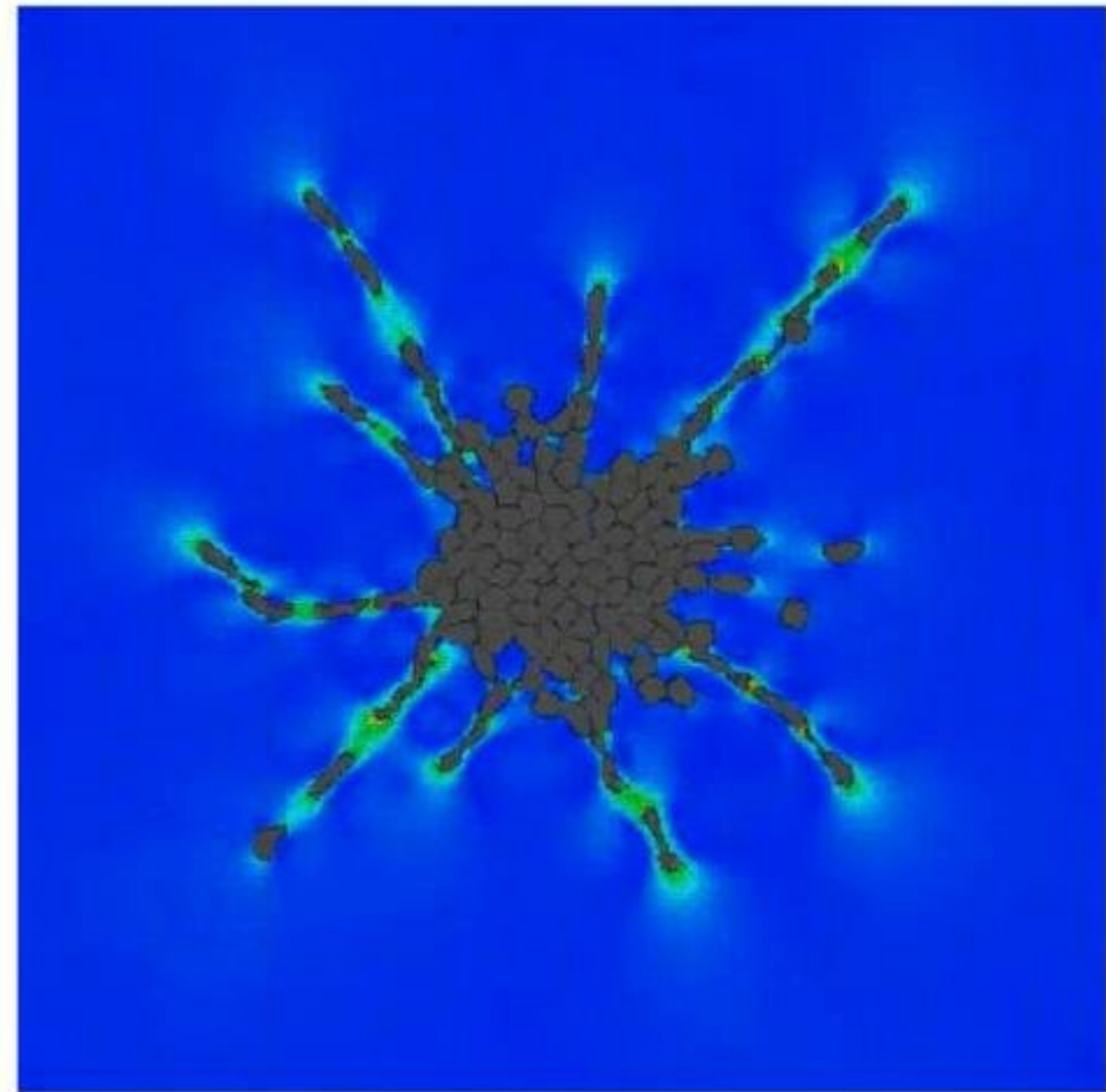
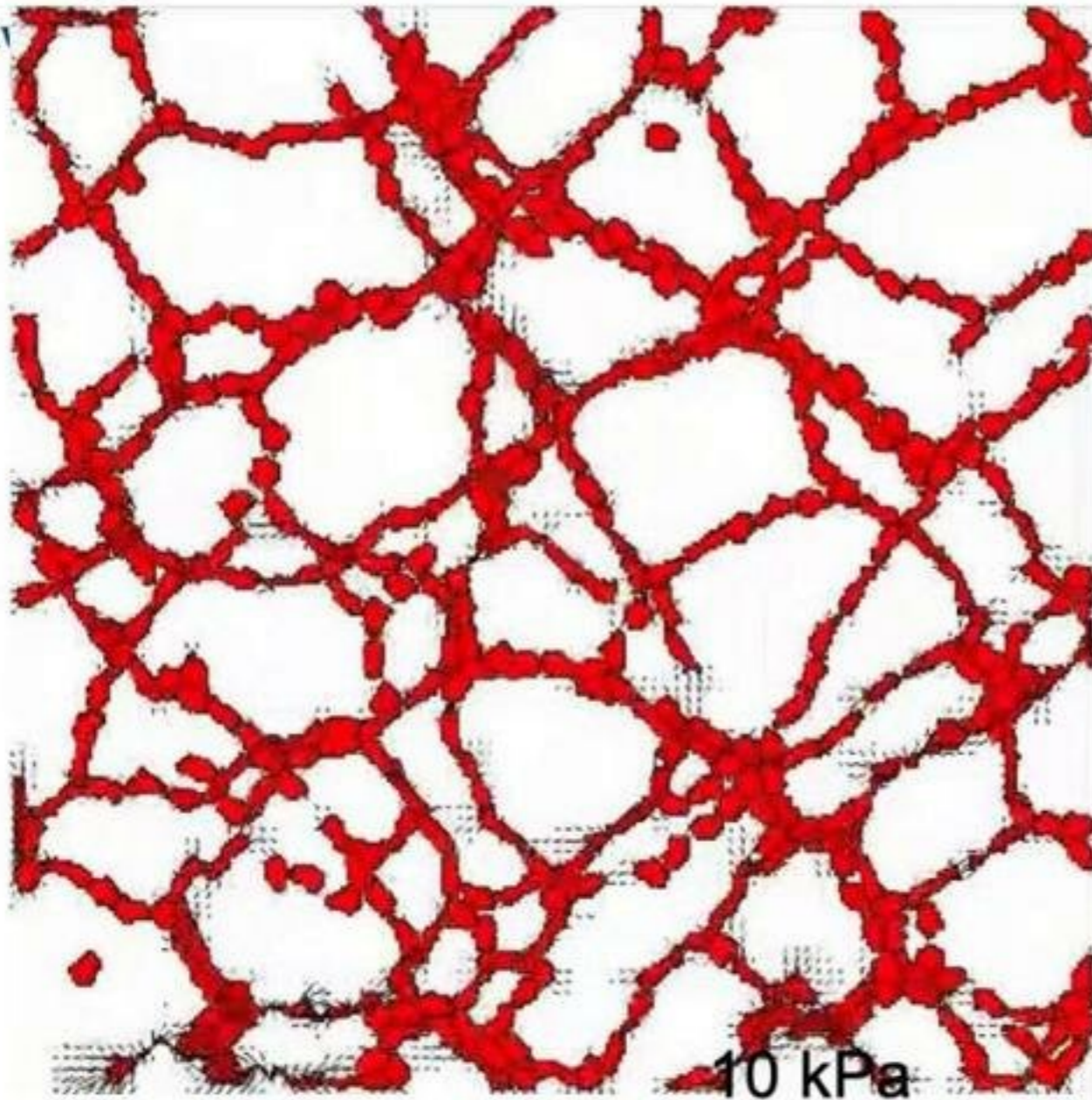
Van Oers, Rens, LaValley, Reinhart-King, and Merks
PLoS Comp Biol 2014





Collective cell behavior

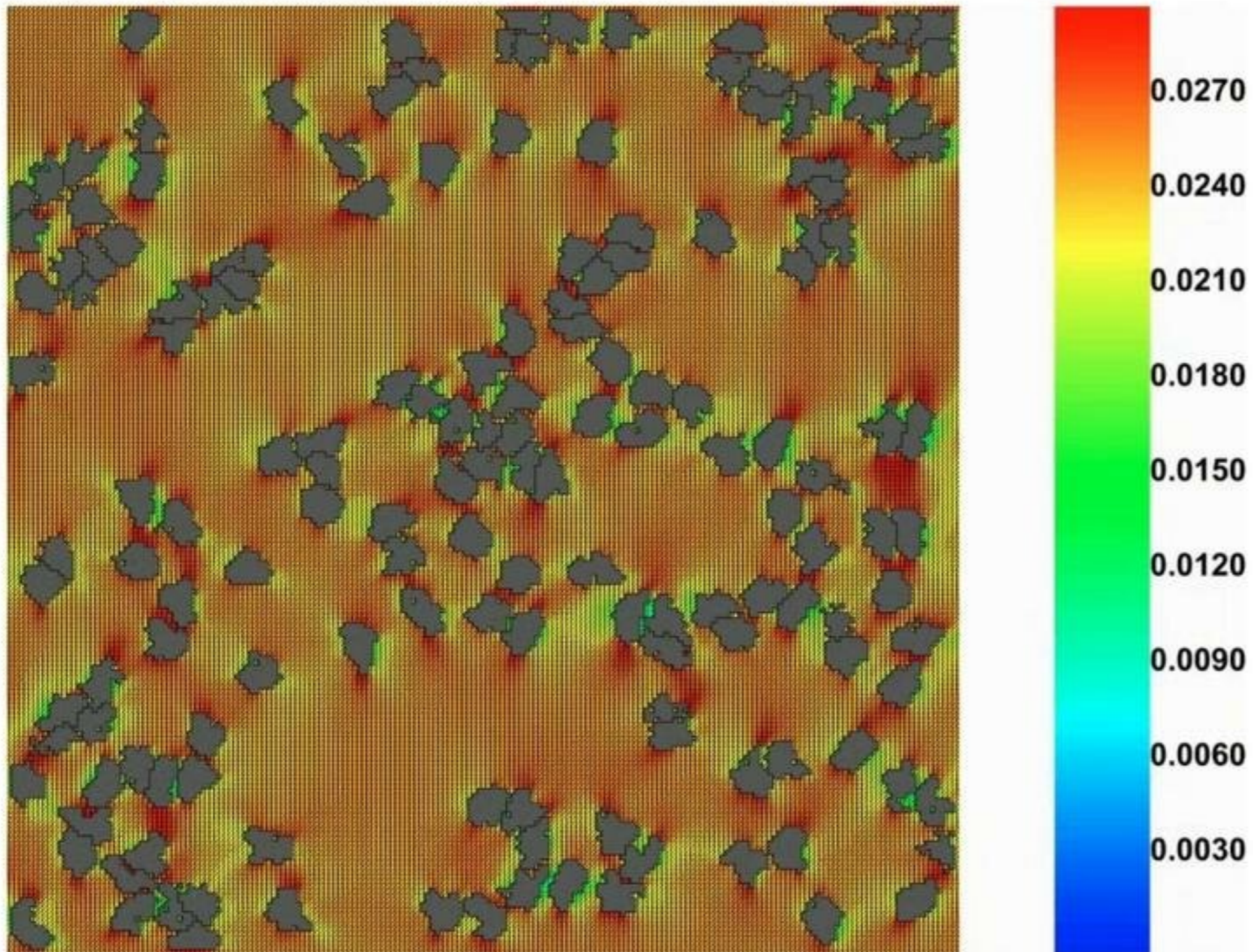
Univ





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... but only if cells exert forces on matrix



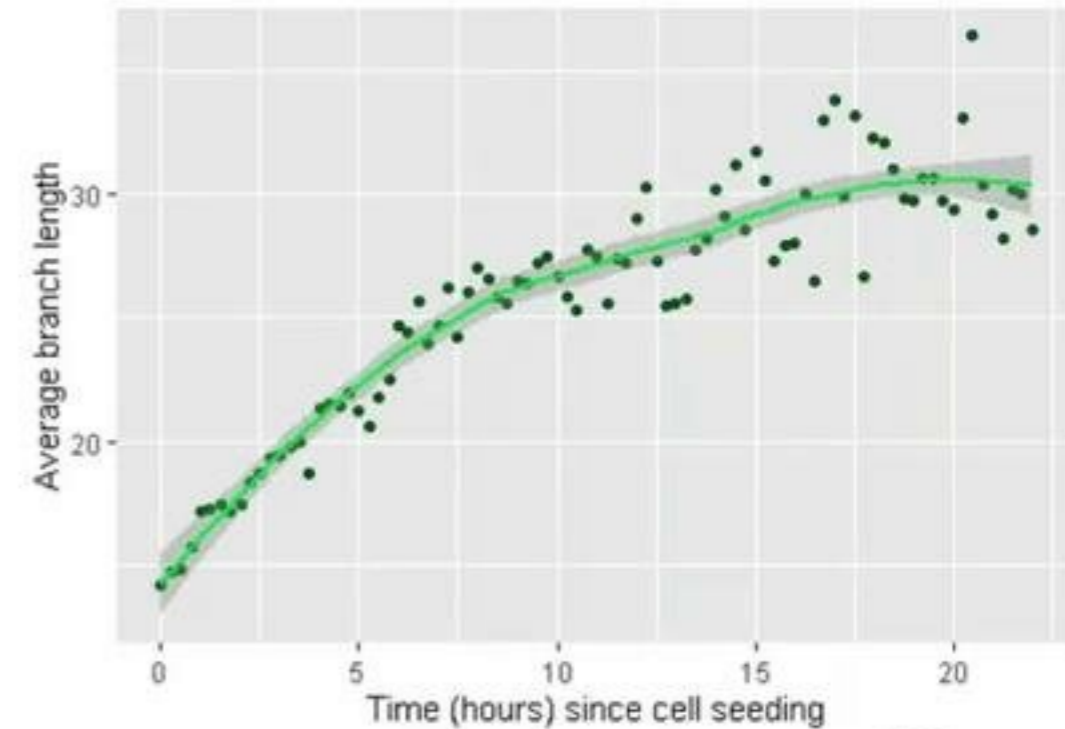
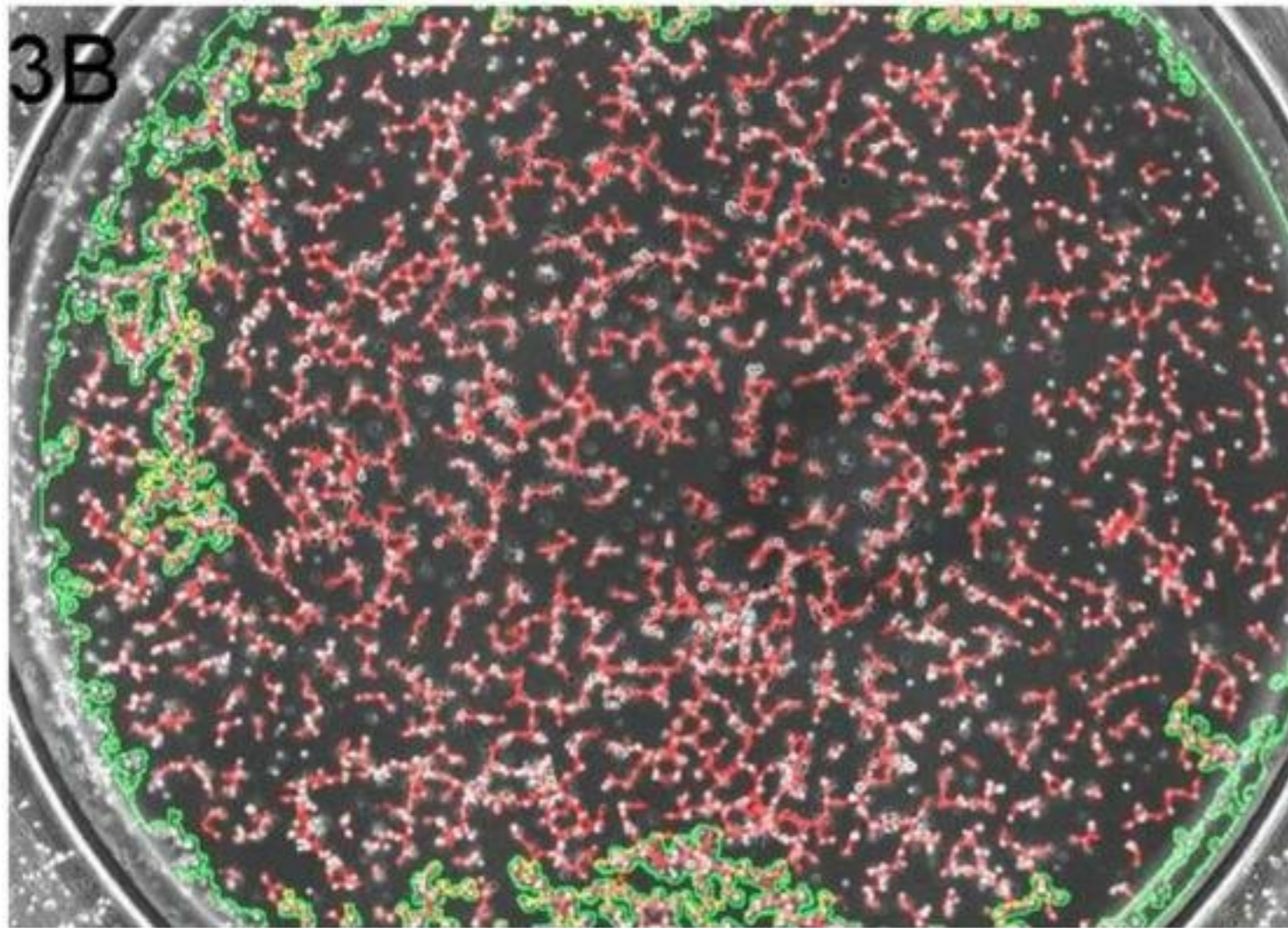


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Automated image analysis



Tessa Vergroesen

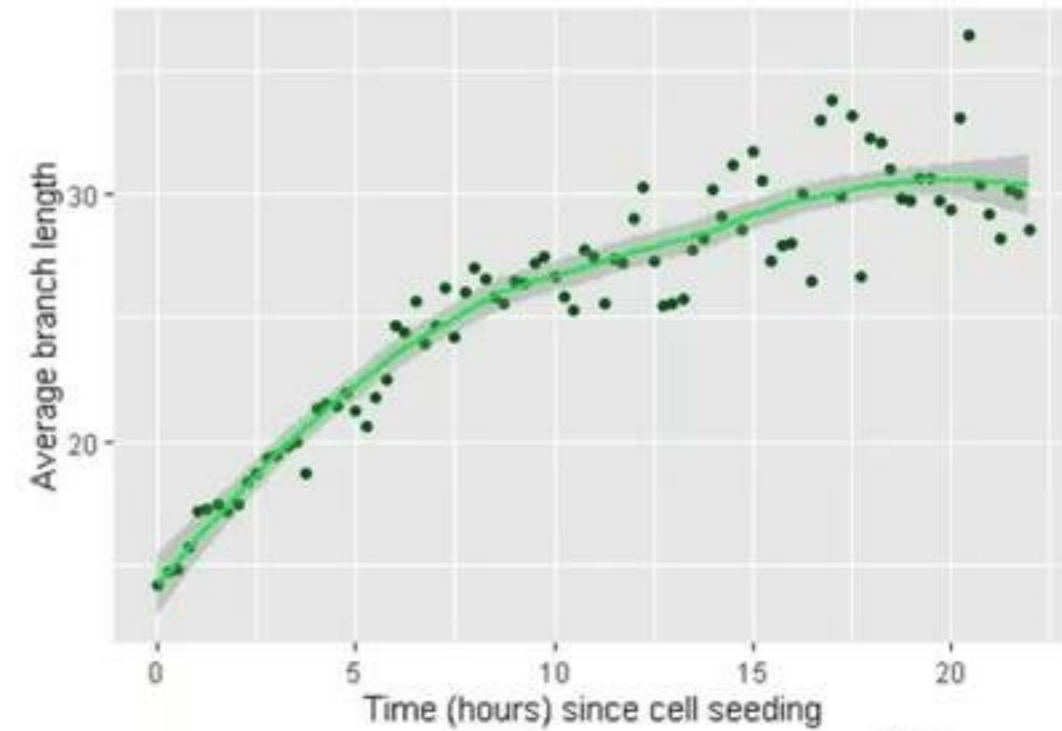
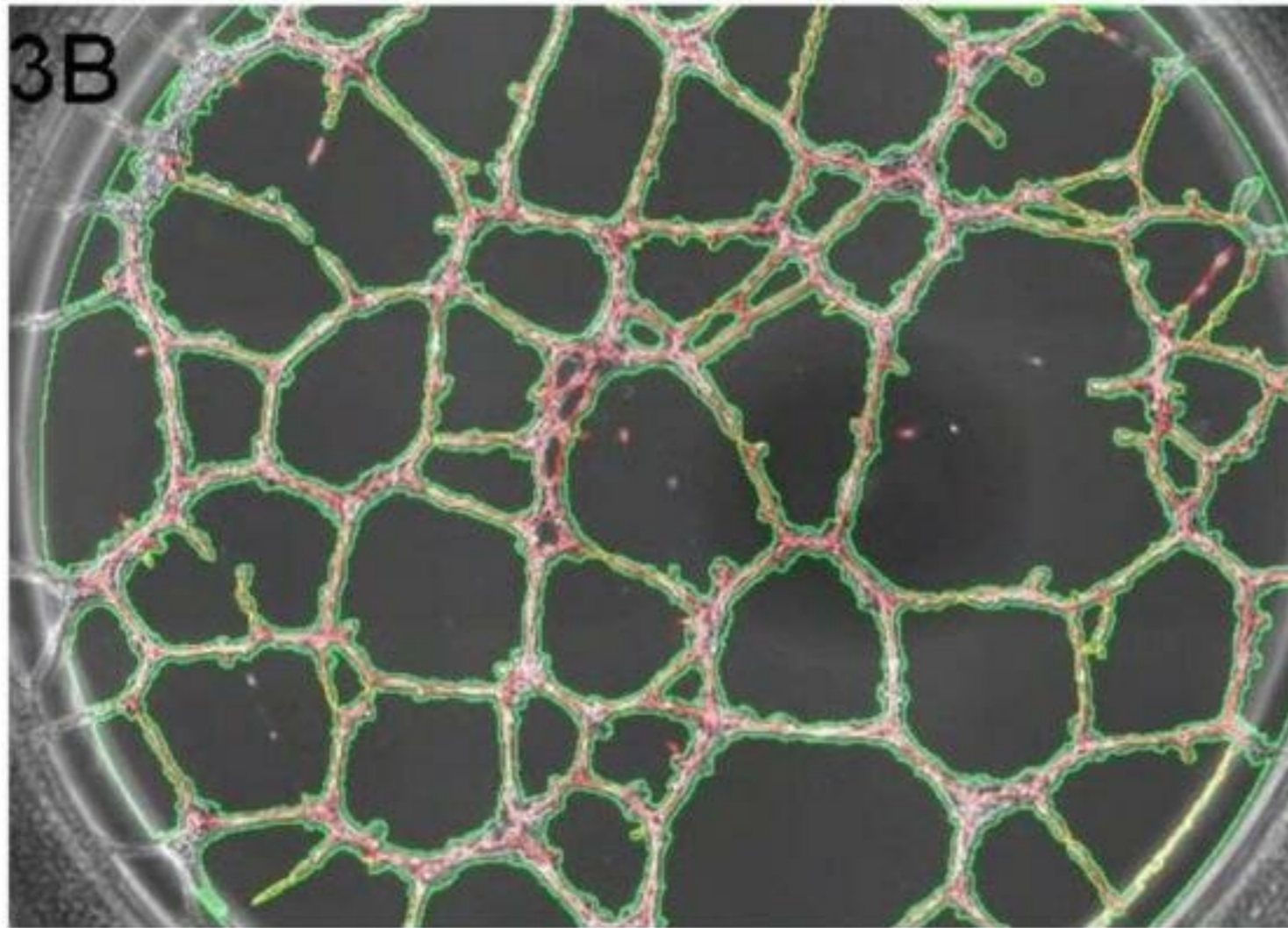




Automated image analysis



Tessa Vergroesen





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Acknowledgments



Not on the picture:

- *Enrico Sandro Colizzi*
- *Koen Schakenraad*

Collaborators:

Leiden University:

- *Luca Giomi*
- *Eric Danen*

Cornell University:

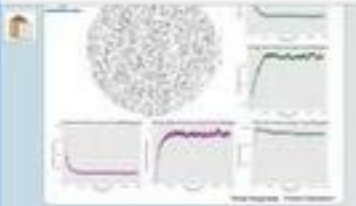
- *Danielle LaValley*
- *Cynthia Reinhart-King*

Funding:

NWO Vidi, NWO Vici, NWO ENW-XL
Netherlands Genomics Initiative



Netherlands Organisation for Scientific Research



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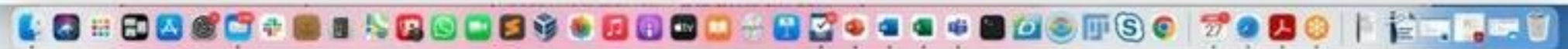
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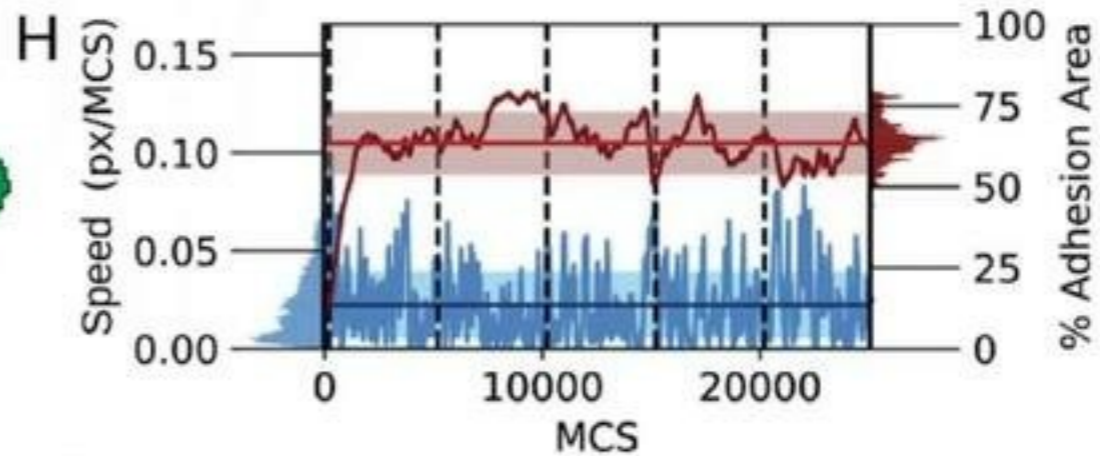
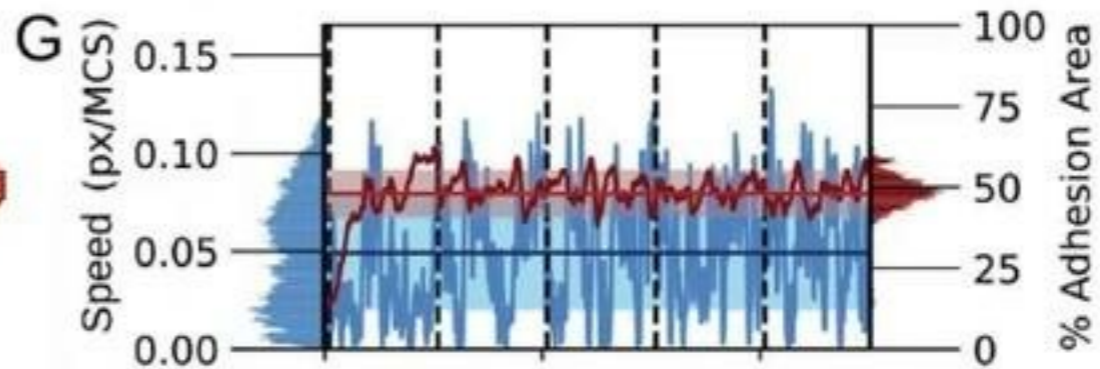
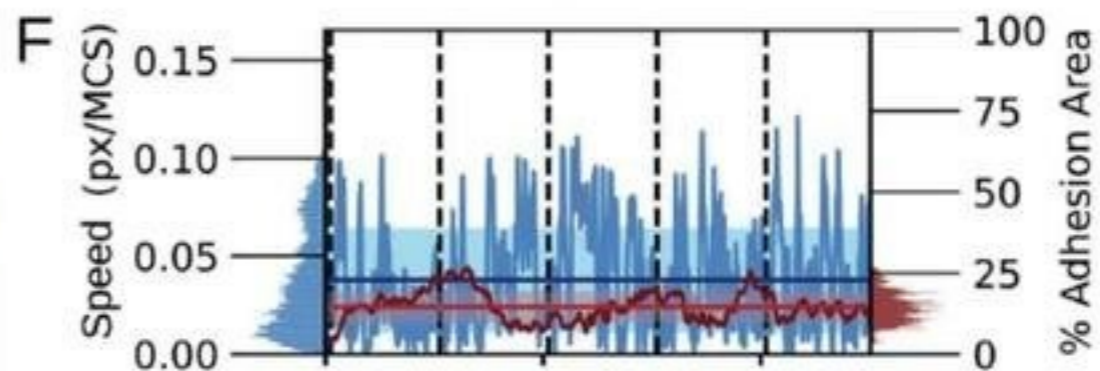
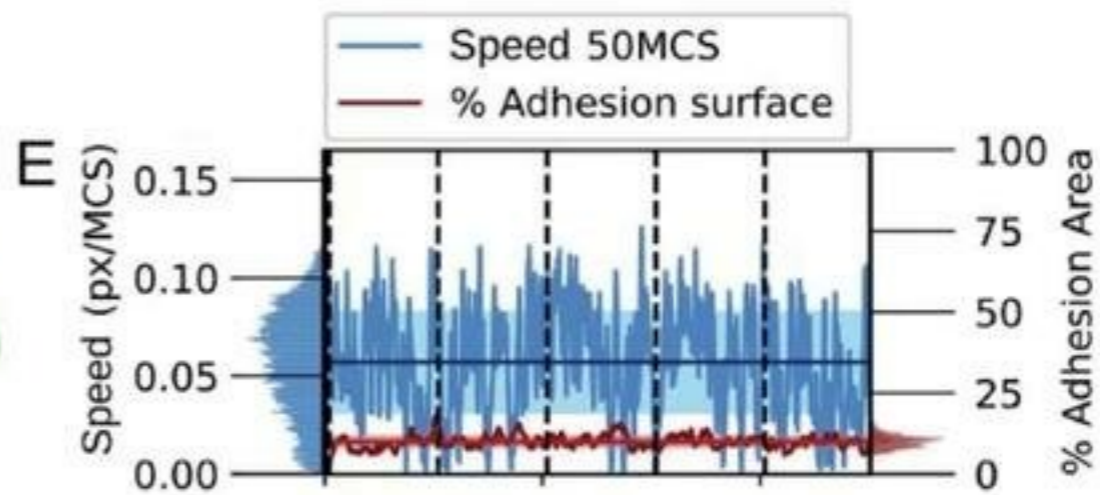
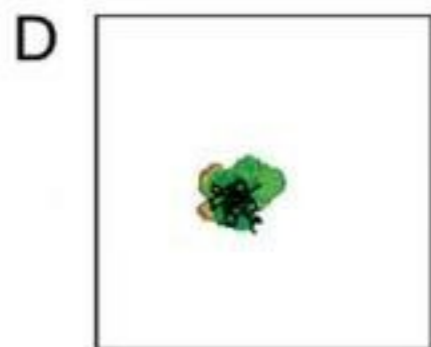
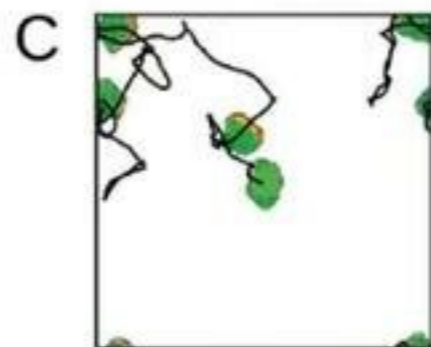
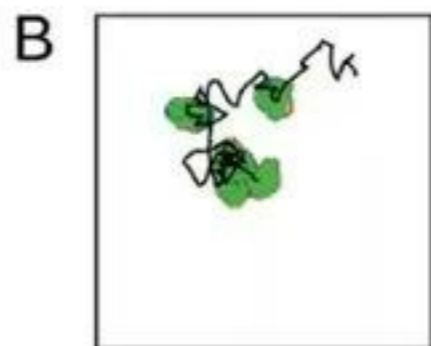
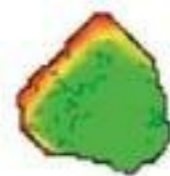
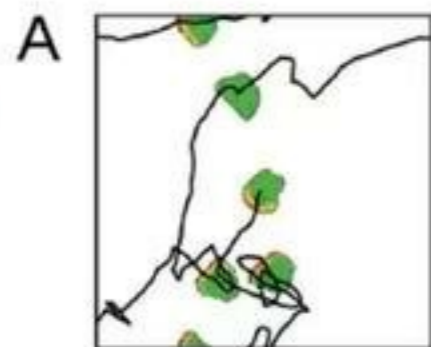


Klik om notities toe te voegen





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Growth rate of adhesions



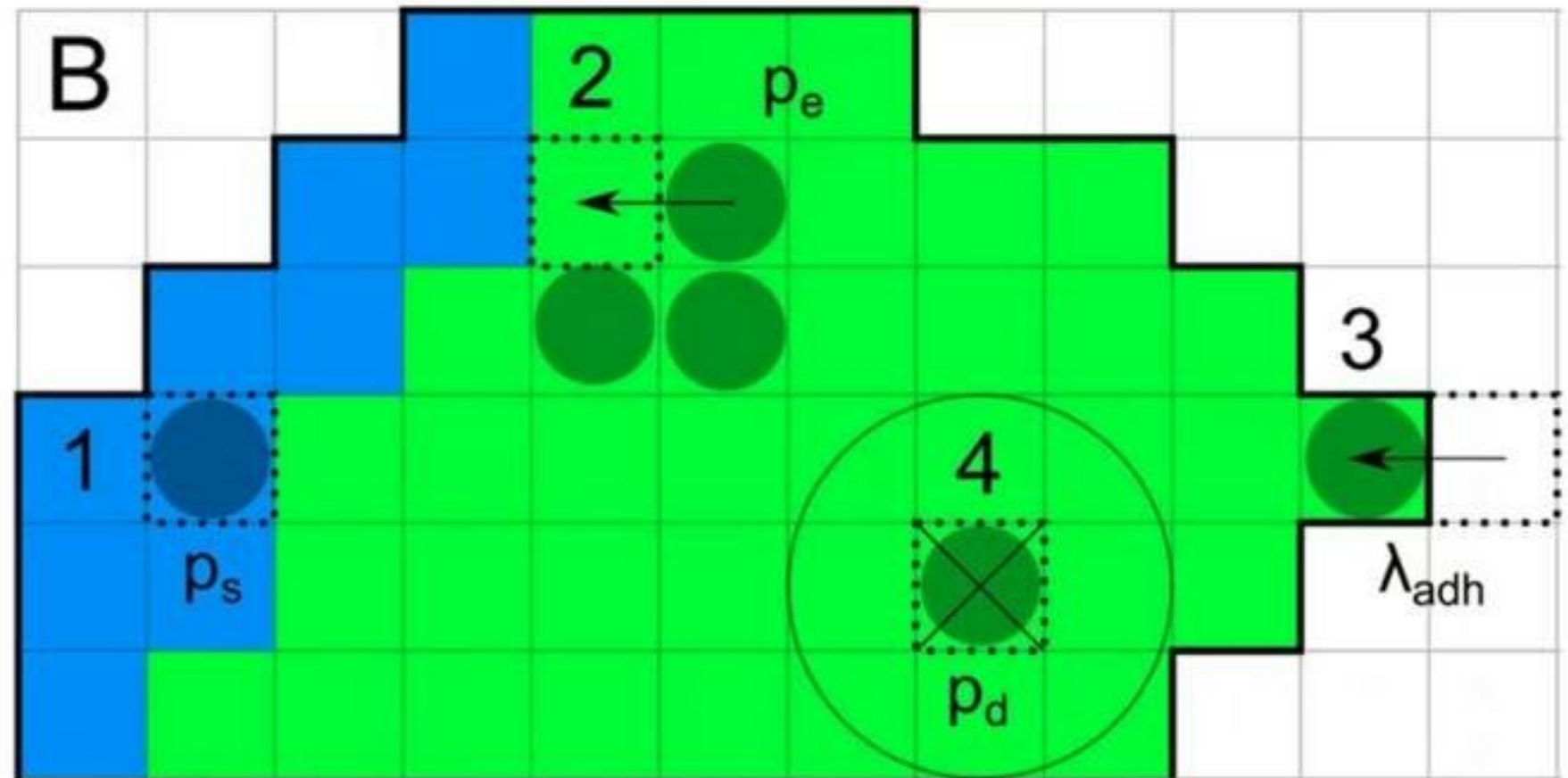
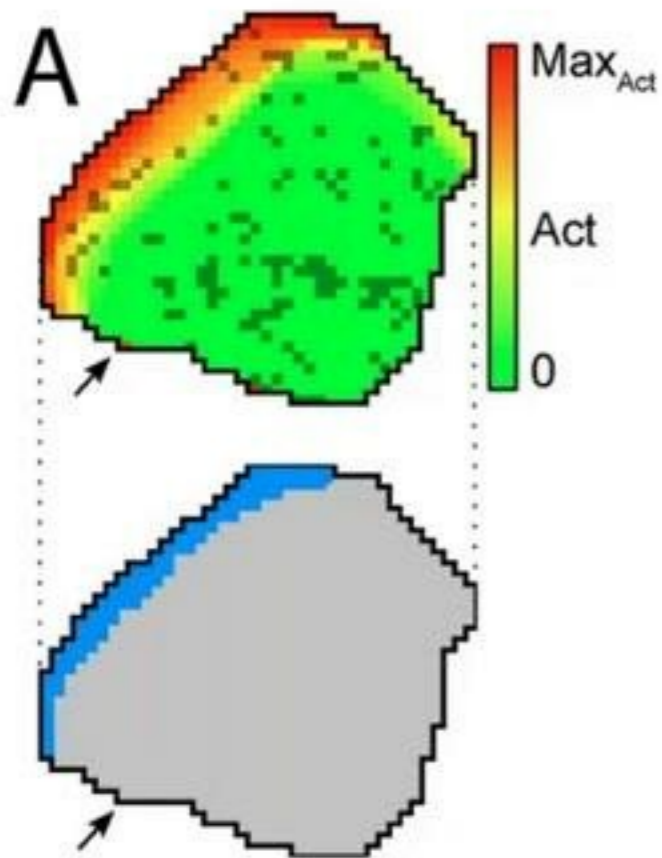


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How do such differences arise? Hypothesis: **cell-substrate adhesion**

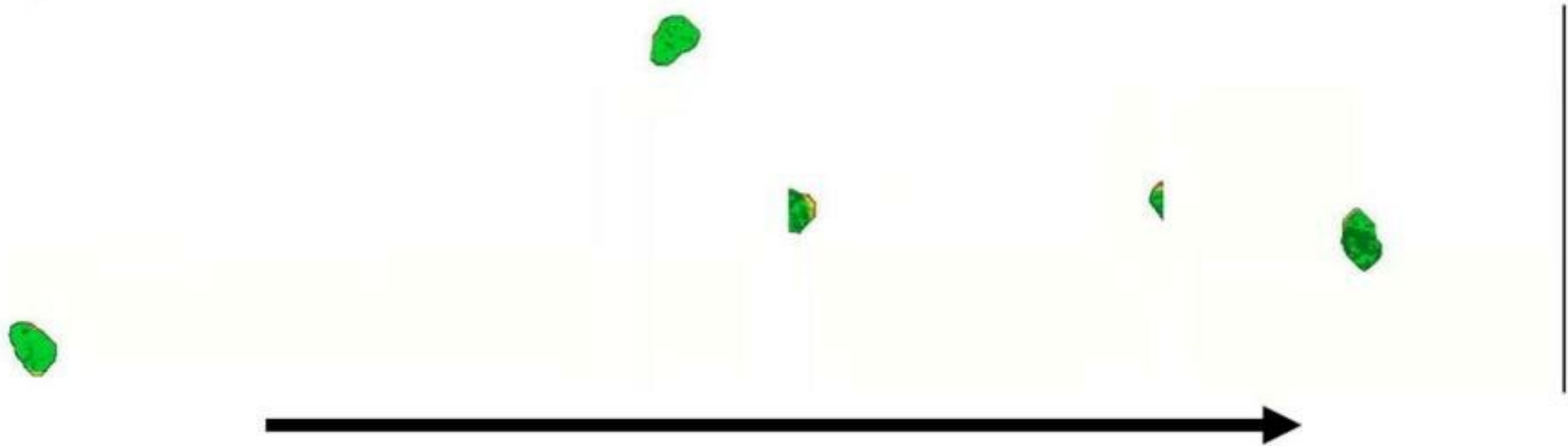


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Growth rate of adhesions

Merks-CECAM2023-plenary

Start Invoegen Tekenen Ontwerpen Overgangen Animaties Diavoorstelling Controleren Beeld MathType Opnemen Acrobat

Tekenen Gum Lassoselectie Pen toevoegen Tekenen met trackpad

73

74 Multicellular Models

75 Evolution of Collective Cell Behavior

76 Cells use cell adhesion, persistence and motility, and stromal cells

Klik om notities toe te voegen

Dia 73 van 98 Nederlands (standaard) Toegankelijkheid: onderzoeken

Notities Opmerkingen 77%

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Standard model (Niculescu et al. P Comput Biol. 2015)

Extended model

Persistence

Total adhesion area

Van Steijn et al., PLOS Computational Biology, 2022

Interactive model Artistoo by Inge Wortel

Leonie van Steijn

Documenten

2-18

PDF-documenten

Spreadsheets

Andere

Schermafbeelding en

Example images folie

export_2023-3-9

export_2023-2-28

